

CBCT with Single-View Temporal Resolution

Marc Kachelrieß

German Cancer Research Center (DKFZ)

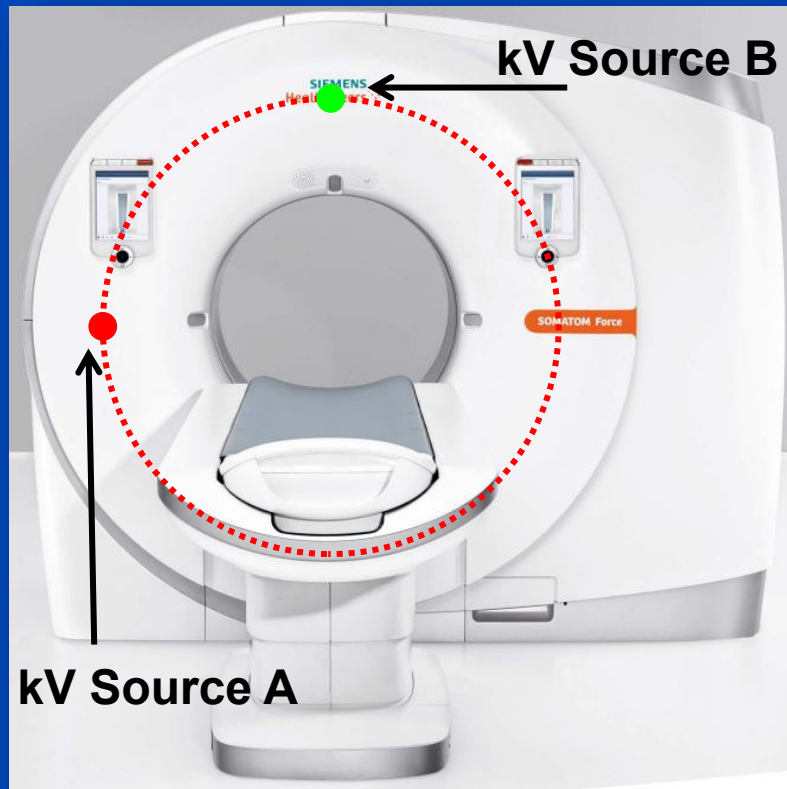
Heidelberg, Germany

www.dkfz.de/ct

BRIEF GENERAL INTRODUCTION

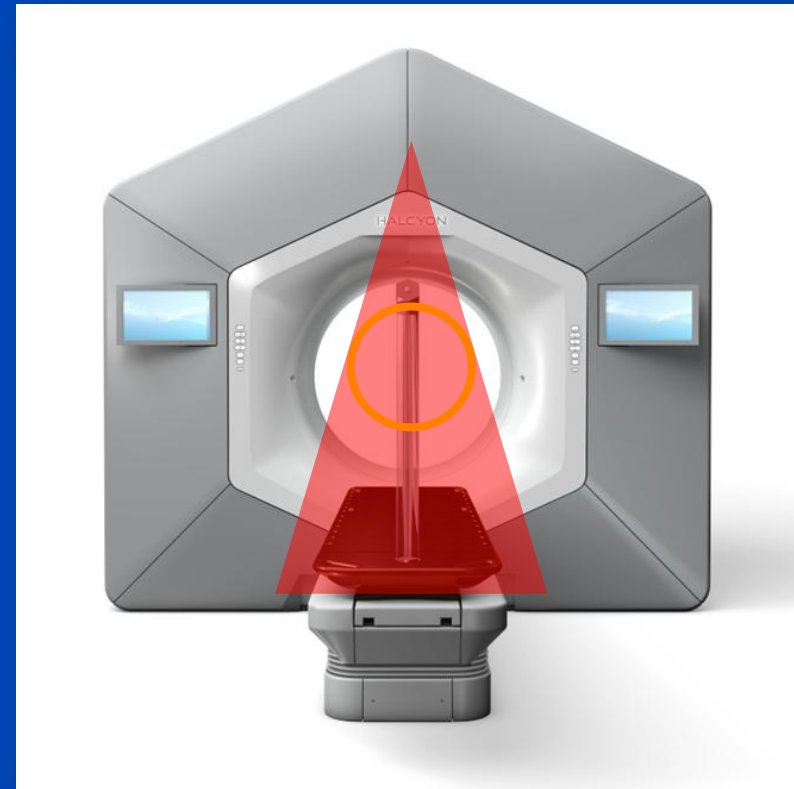
CT vs. CBCT

Clinical CT



Rotation time T_{rot} : down to 0.23 s

CBCT in IGRT



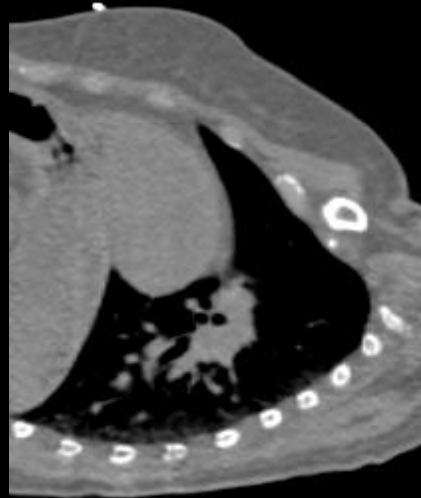
Rotation time T_{rot} : ~ 10 s

Temporal resolution: $0.5 \times T_{\text{rot}}$ (single source), $0.25 \times T_{\text{rot}}$ (dual source)

Faster, Equal or Slower Gantry Rotation than Motion Cycle – Which is Best for Cyclic 4D?

- **Much faster 😊**
 - Always good, since motion is (nearly) frozen.
 - Requires fast scanners with very high tube power and very high detector frame rates.
 - Not possible in CBCT.
- **Much slower 😞**
 - Allows for gating, if motion is quasi-periodic.
 - Gating results in sparseness artifacts (sparse angular sampling).
 - The slower the better: more motion cycles mean less pronounced sparseness artifacts.
- **Close to equal 😐**
 - For each view angle the patient is seen in a different motion state.
 - Weird artifacts may occur.
- **Exception**
 - Single breath-hold scan, if scan is fast enough (e.g. less than 10 s).
 - However, organ motion can no longer be resolved.

Much Faster: 4D CT



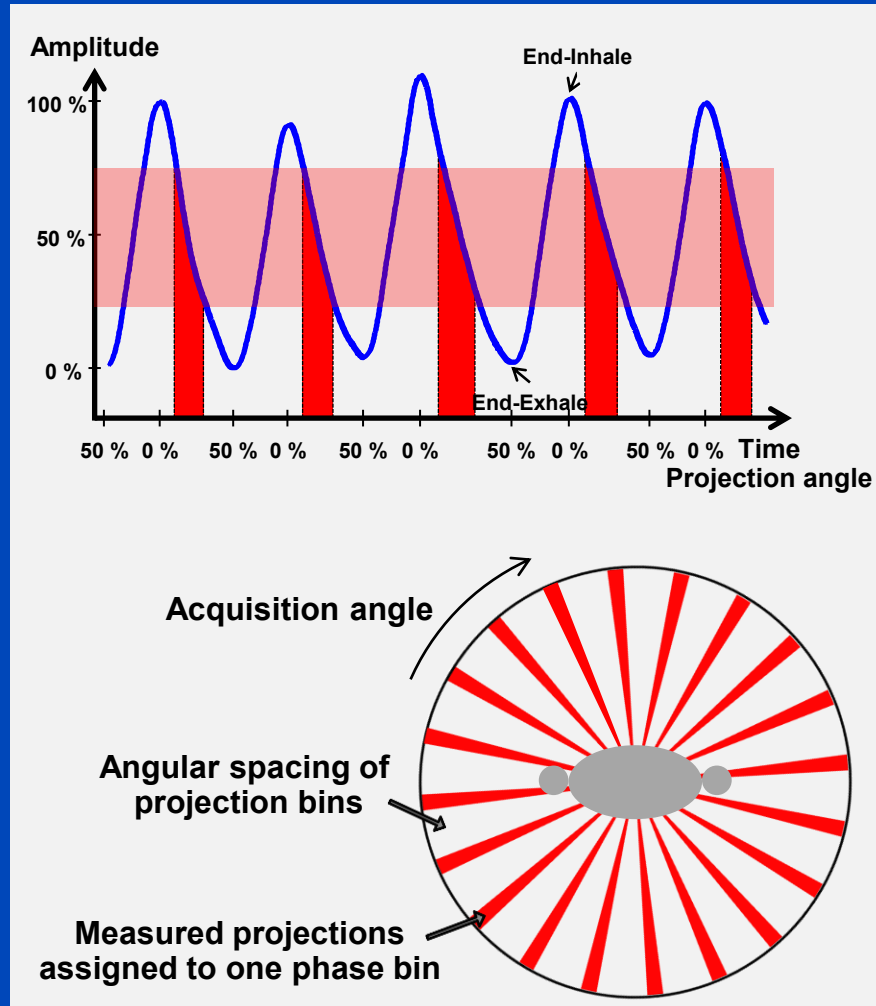
Patient 1



Patient 2

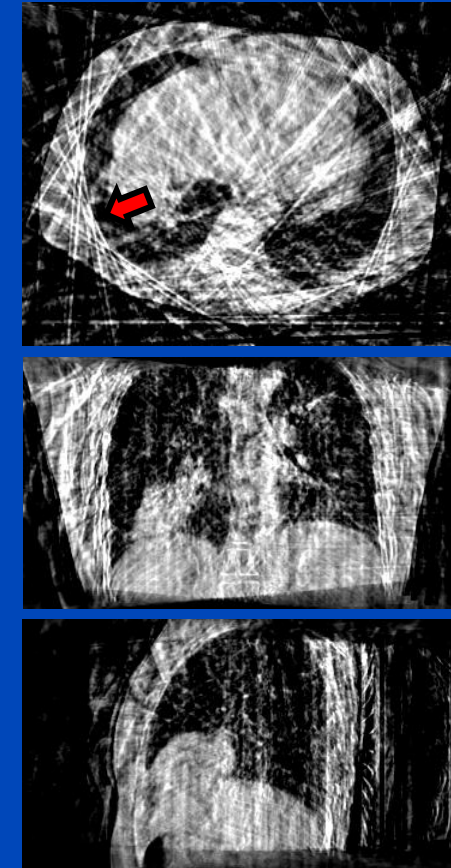
C = 0 HU, W = 1000 HU

Much Slower: 4D CBCT Scan

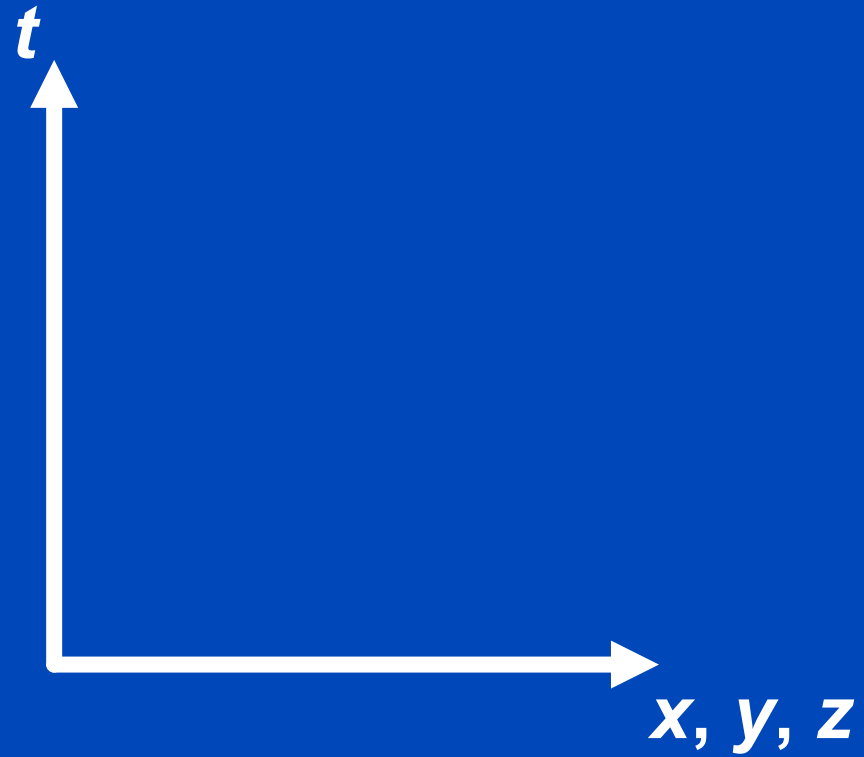


Without gating (3D): Motion artifacts

With gating (4D):
Sparse-view artifacts



What is 4D?



What is 4D?

Cyclic 4D

Assumes periodic motion

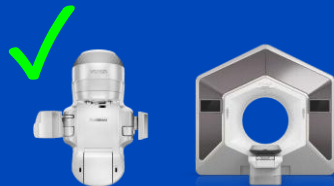
Needs breathing signal

Today's 4D CT and 4D CBCT

~ 500 ms temp. res.

~ 10 time points

Only before treatment



True 4D

Any kind of motion

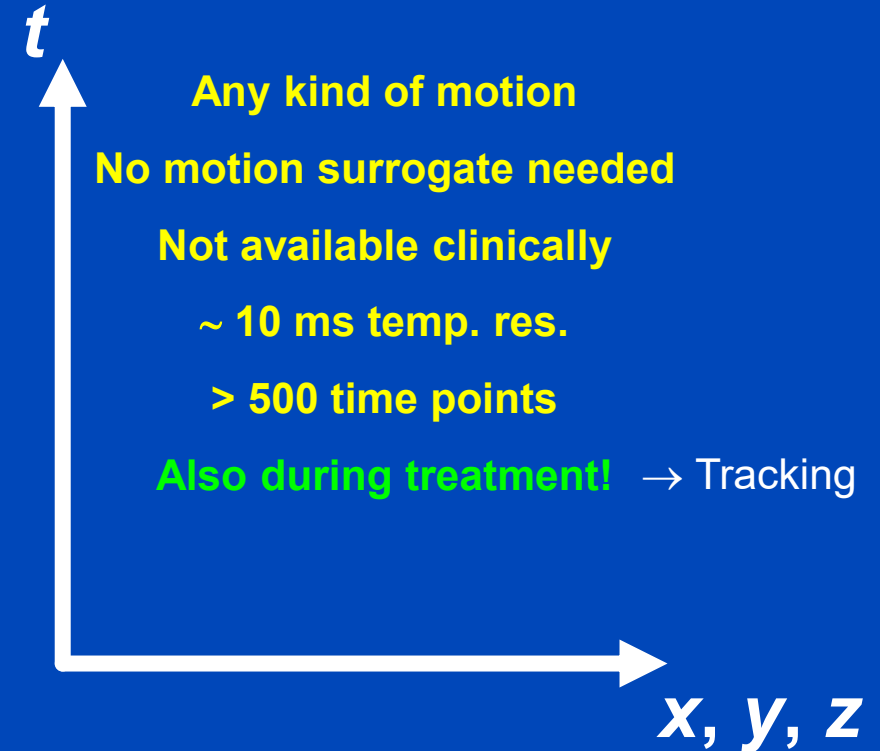
No motion surrogate needed

Not available clinically

~ 10 ms temp. res.

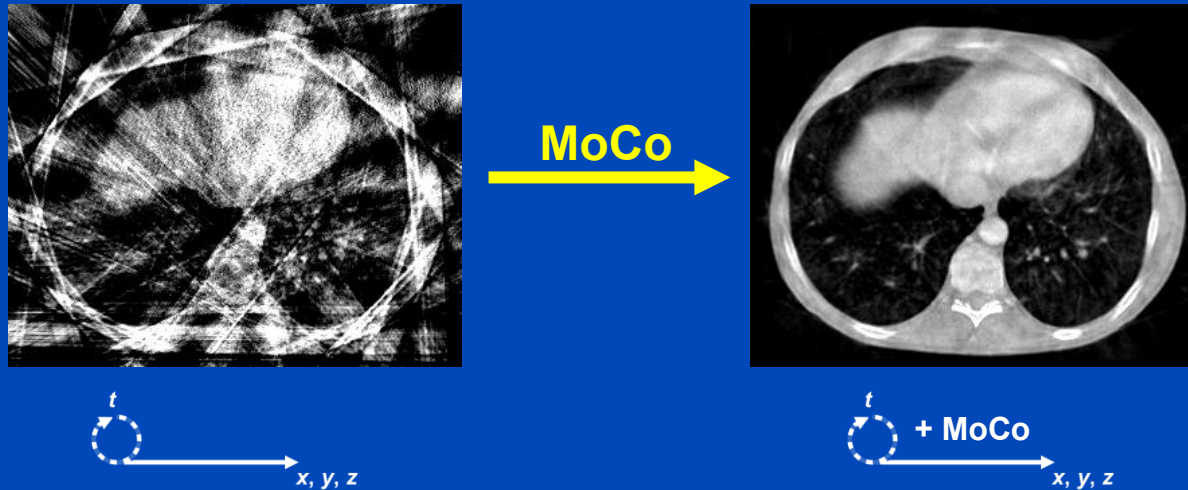
> 500 time points

Also during treatment! → Tracking



→ this presentation

Motion Compensation (MoCo) Let the Voxels Move!



State-of-the-art

CYCLIC 4D

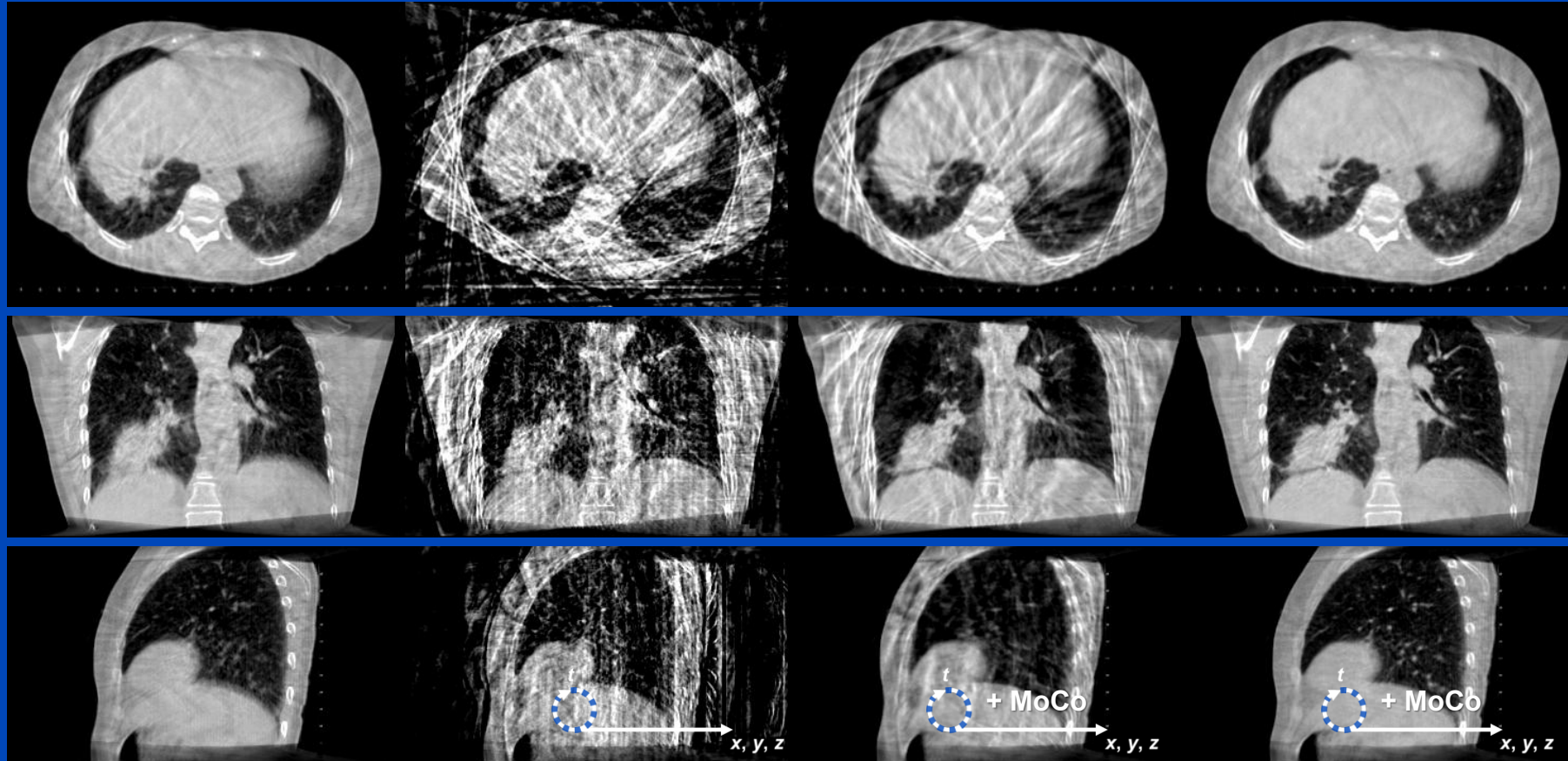
4D – University of Erlangen (2011 – 2014)

3D CBCT
Standard

4D gated CBCT
Conventional
Phase-Correlated

sMoCo
Standard Motion
Compensation

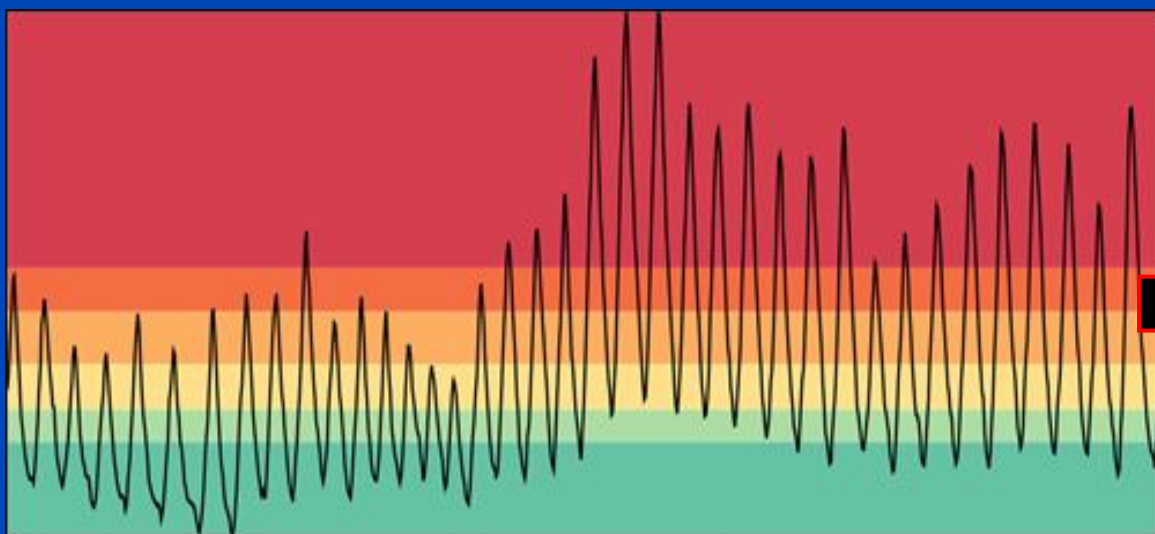
acMoCo
Artifact Model-Based
Motion Compensation



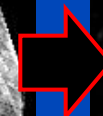
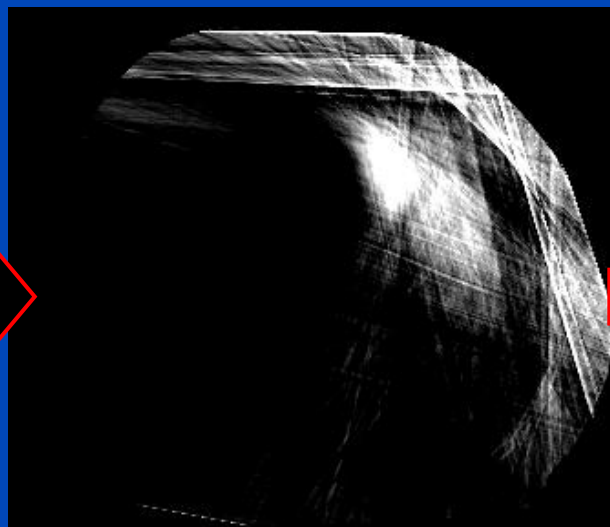
- sMoCo:** Li, Koong, and Xing, "Enhanced 4D cone-beam CT with inter-phase motion model," Med. Phys. 51(9), 3688–3695, 2007.
- cMoCo:** Brehm, Paysan, Oelhafen, Kunz, and Kachelrieß, "Self-adapting cyclic registration for motion-compensated cone-beam CT in image-guided radiation therapy," Med. Phys. 39(12):7603-7618, 2012.
- acMoCo:** Brehm, Paysan, Oelhafen, and Kachelrieß, "Artifact-resistant motion estimation with a patient-specific artifact model for motion-compensated cone-beam CT" Med. Phys. 40(10):101913, 2013.

1 min shifted detector CBCT scan with about 12 respiratory cycles, displayed with 30 rpm.
Patient data provided by Memorial Sloan-Kettering Cancer Center, New York, NY. $C = -200$ HU, $W = 1400$ HU

Gating Fails on Irregular Breathing!



Gating = bad



Gating + MoCo = still bad



Future
TRUE 4D

RESEARCH ARTICLE

MEDICAL PHYSICS

Deep learning-based cone-beam CT motion compensation with single-view temporal resolution (Deep SAMoCo)

Joscha Maier¹ | Stefan Sawall^{1,2} | Marcel Arheit³ | Pascal Paysan³ |
Marc Kachelrieß^{1,2}

¹Division of X-Ray Imaging and Computed Tomography, German Cancer Research Center (DKFZ), Heidelberg, Germany

²Medical Faculty Heidelberg, Heidelberg University, Heidelberg, Germany

³Varian Medical Systems Imaging Laboratory, GmbH, Baden-Daettwil, Switzerland

Correspondence

Marc Kachelrieß, Division of X-Ray Imaging and Computed Tomography, German Cancer Research Center (DKFZ), Heidelberg, Germany.
Email: marc.kachelriess@dkfz.de

Abstract

Background: Cone-beam CT (CBCT) scans that are affected by motion often require motion compensation to reduce artifacts or to reconstruct 4D (3D+time) representations of the patient. To do so, most existing strategies rely on some sort of gating strategy that sorts the acquired projections into motion bins. Subsequently, these bins can be reconstructed individually before further post-processing may be applied to improve image quality. While this concept is useful for periodic motion patterns, it fails in case of non-periodic motion as observed, for example, in irregularly breathing patients.

Purpose: To address this issue and to increase temporal resolution, we propose the deep single angle-based motion compensation (SAMoCo).

Methods: To avoid gating, and therefore its downsides, the deep SAMoCo trains

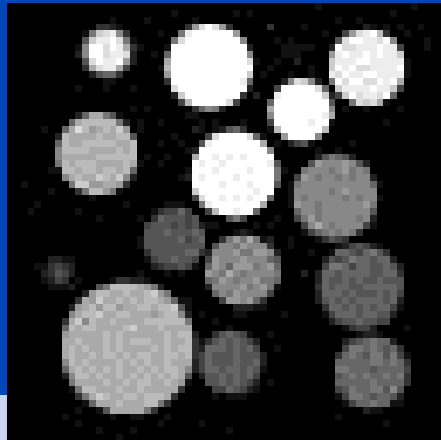
Deep SAMoCo = True 4D



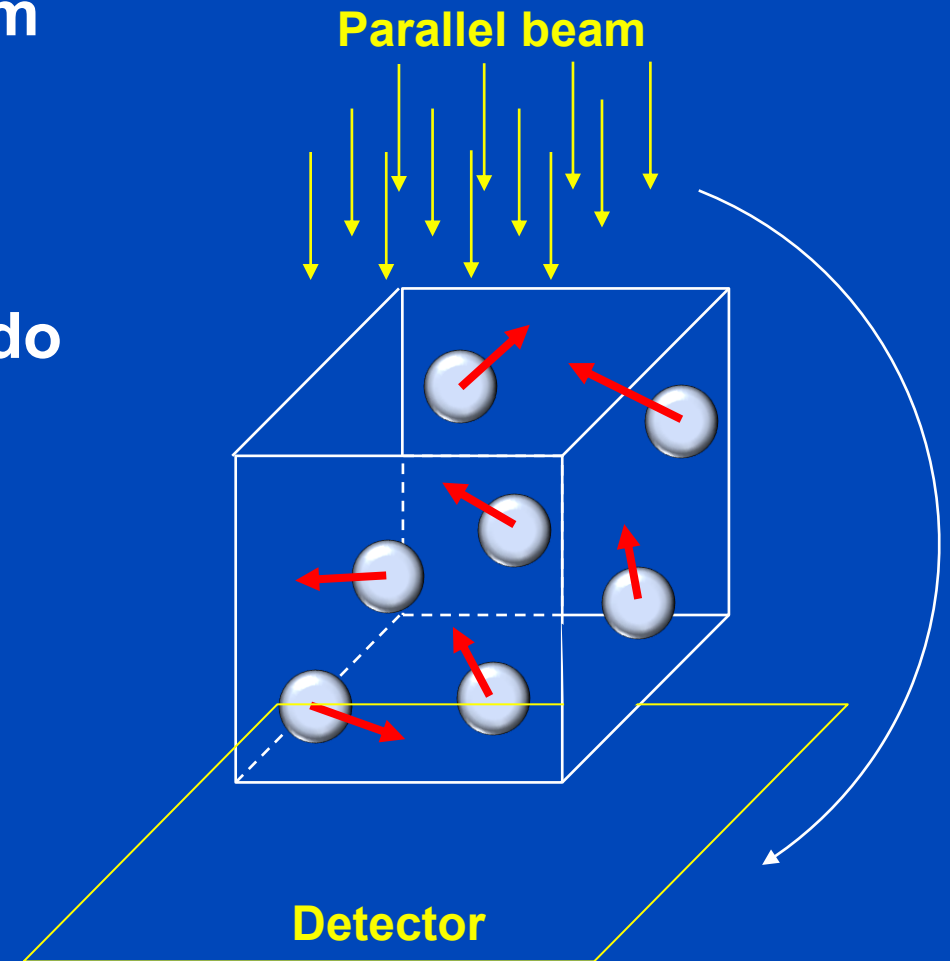
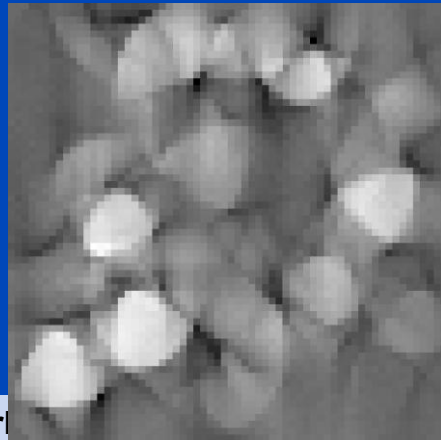
Bouncing Spheres

- Spheres with random velocity and random density in a box.
- Elastic collisions with other spheres and walls are elastic.
- 180° scan (180 projections) using a pseudo parallel-beam geometry.
- FDK reconstruction ($64 \times 64 \times 32$) of single views $\rightarrow$ 180 PARs.

Slice of prior volume



3D reconstruction



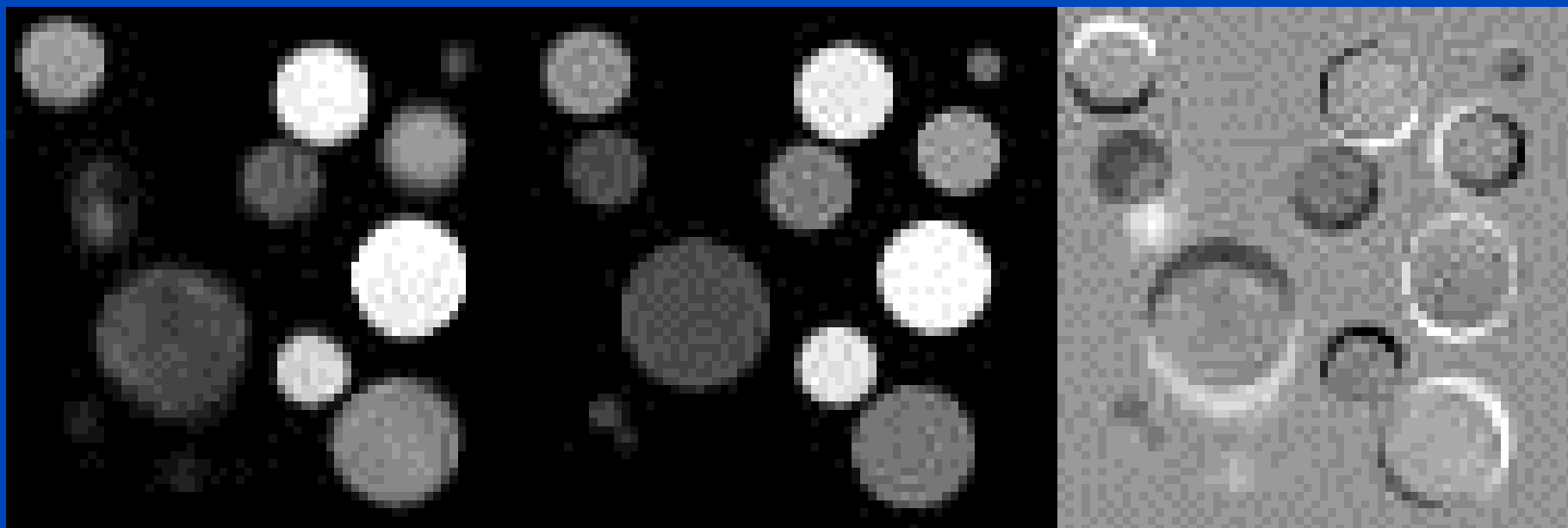
Results

Spheres

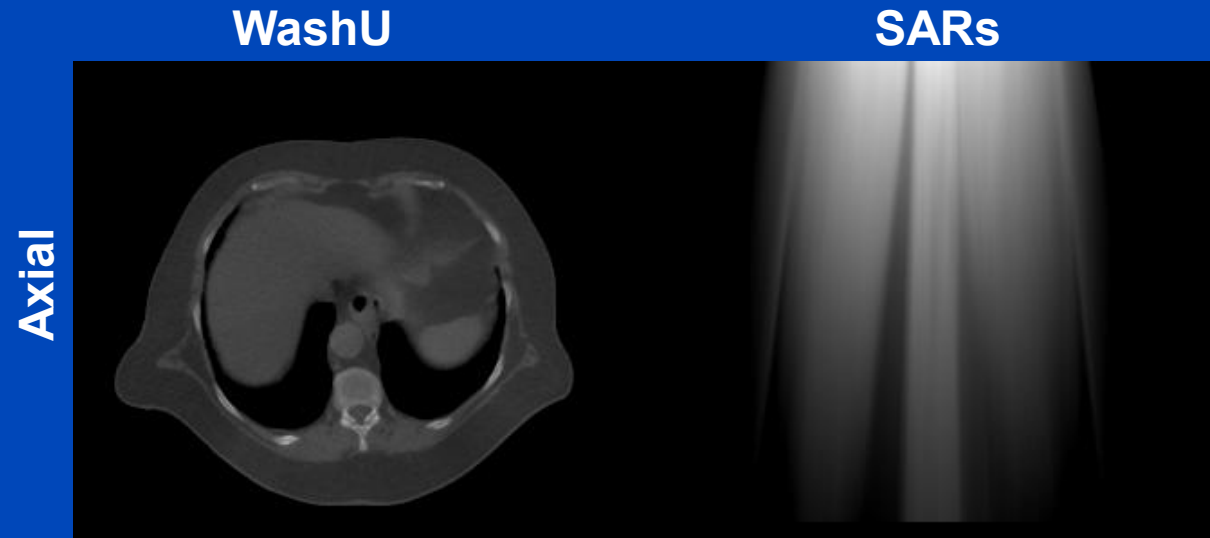
Prediction

Ground truth

Difference



Single Angle Reconstructions (SARs)



84 4D CT scans (no artifacts, high temporal resolution)

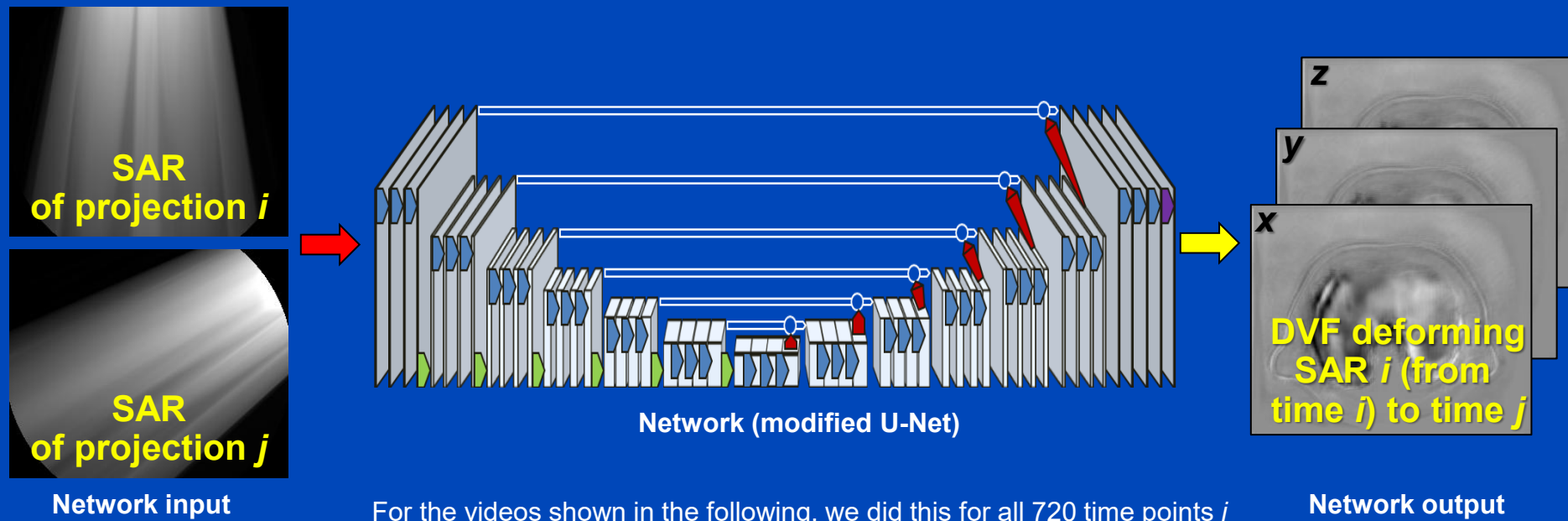
- 10 respiratory phases each (WashU/Colorado dataset)
- 10·10 combinations of phase *A* and *B* possible (including $A=B$)
- 84·10·10 displacement vector fields (DVF) known
- 720 CBCT projections¹ simulated for each CT scan (each phase)
- $84 \cdot 10 \cdot 720 \cdot 10 \cdot 720 = 6.5$ billion projection pairs with known DVF

¹The actual projection numbers are between 420 and 900 and depend on the scan mode.

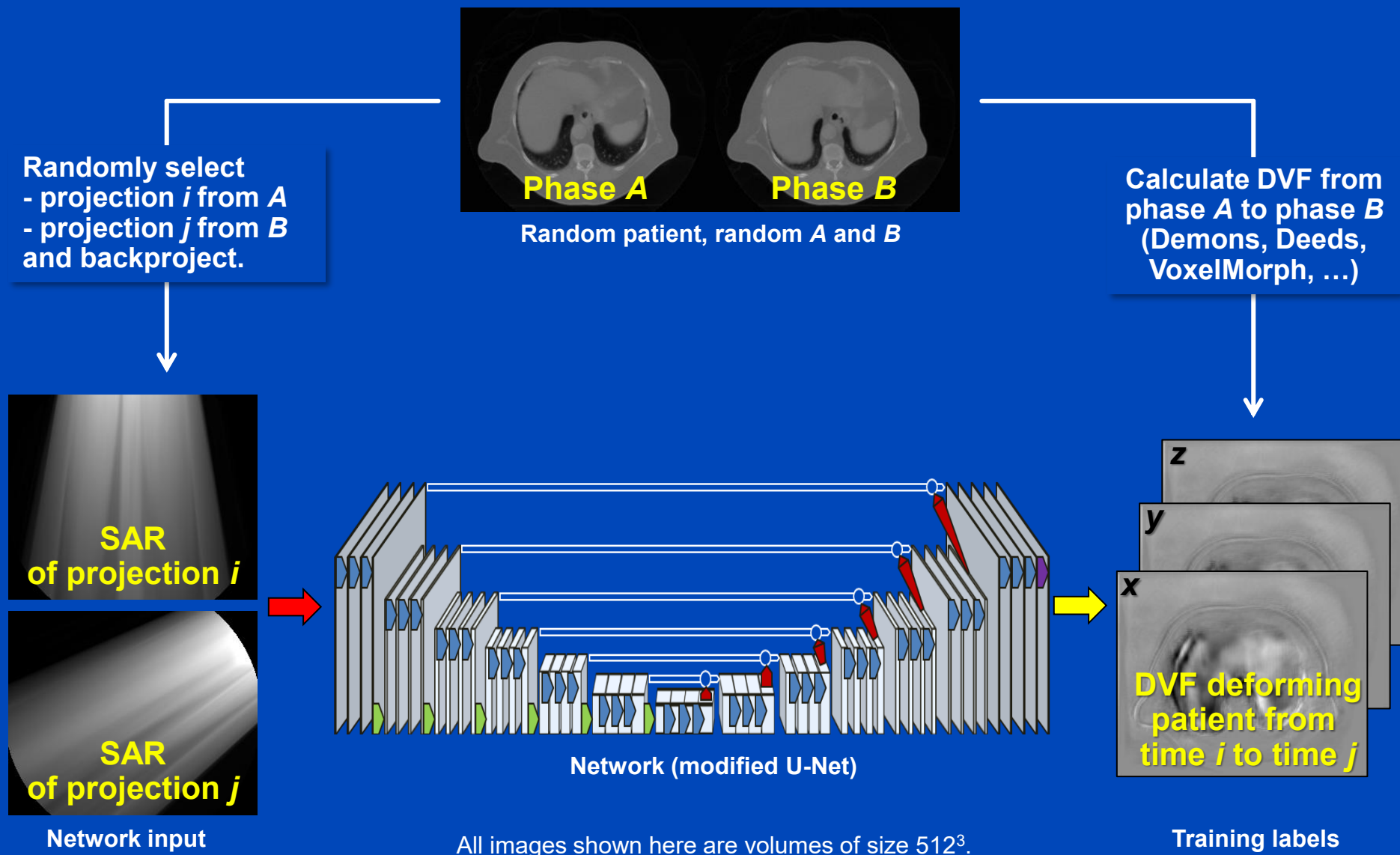
Inference Workflow of Deep SAMoCo

- For a new patient
 - decide for the desired time point j , e.g. the one from 1 millisecond ago
 - for all $i \neq j$ get the DVFs pointing from i to j from the neural network
 - deform SARs for all $i \neq j$ into time point j
 - add all the volumes

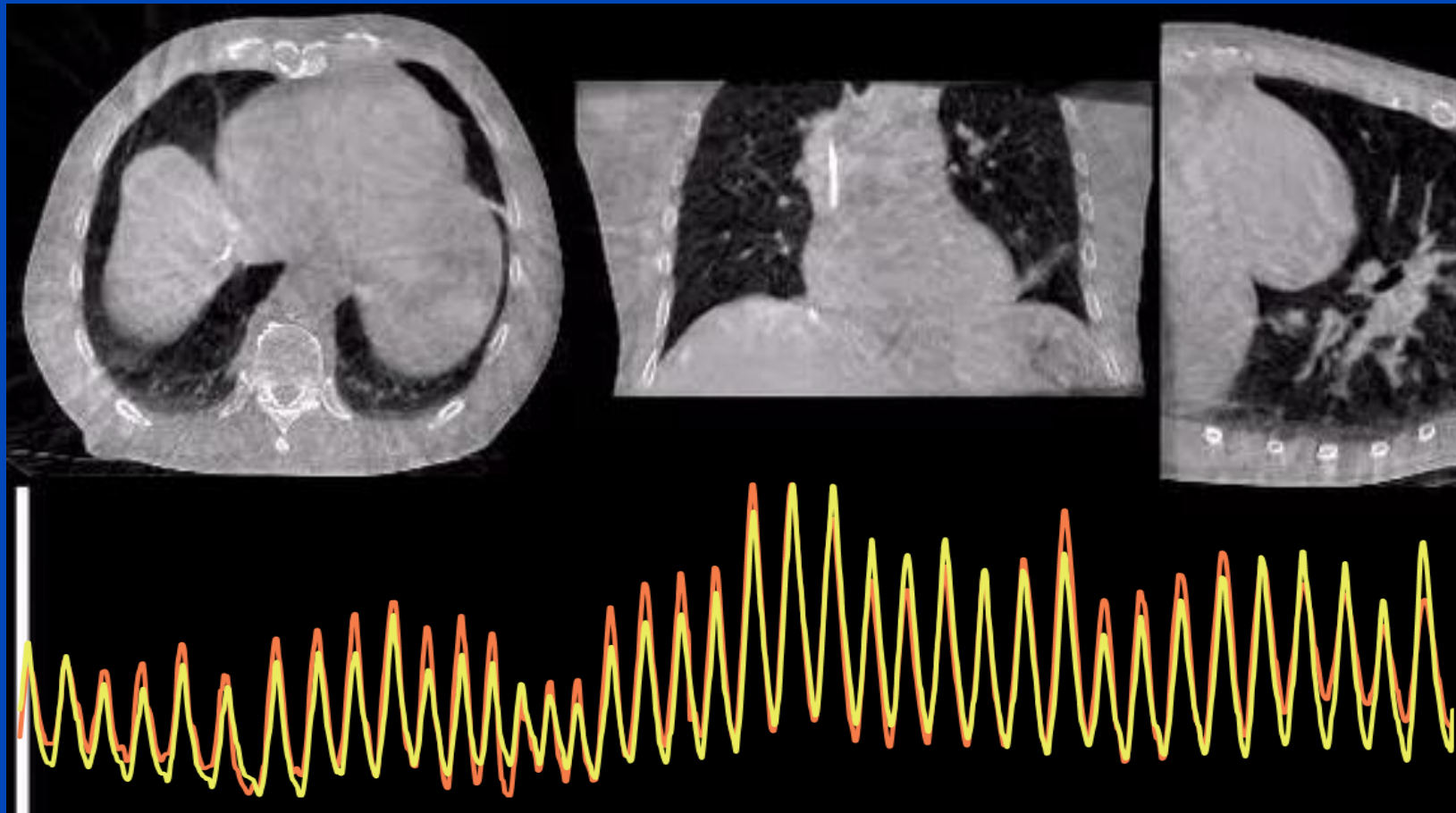
For all $i \neq j$ do



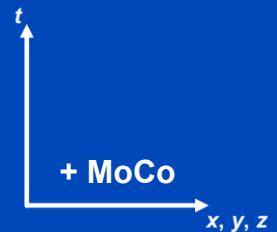
Training Workflow of Deep SAMoCo



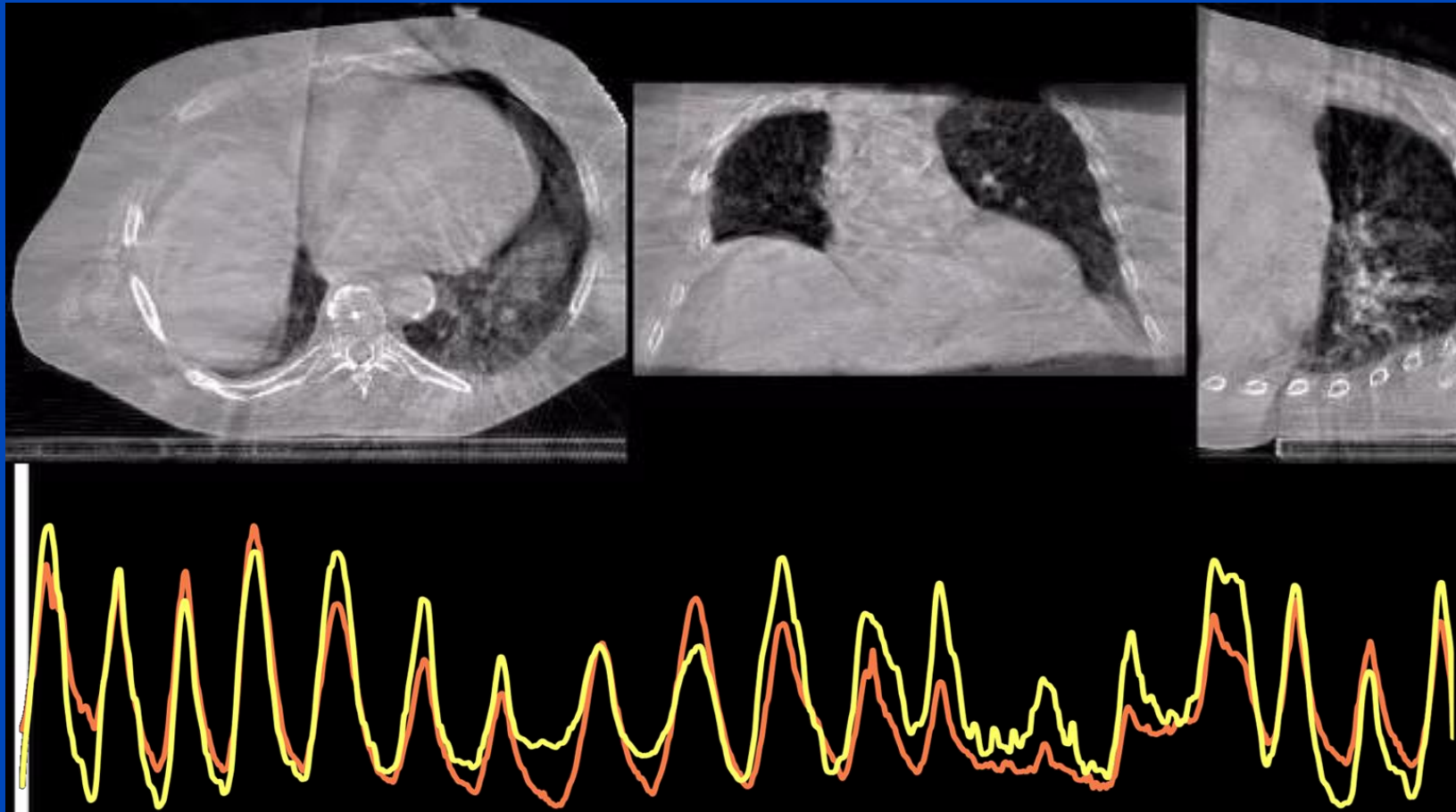
VUMC_4DThorax



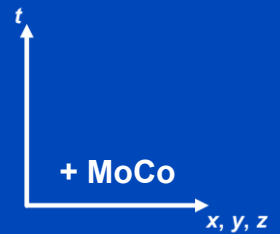
Red: RPM signal (external signal – not used for recon)
Yellow: Diaphragm motion (intrinsic signal – from PAMoCo recon)



MSK 1



Red: RPM signal (external signal – not used for recon)
Yellow: Diaphragm motion (intrinsic signal – from PAMoCo recon)



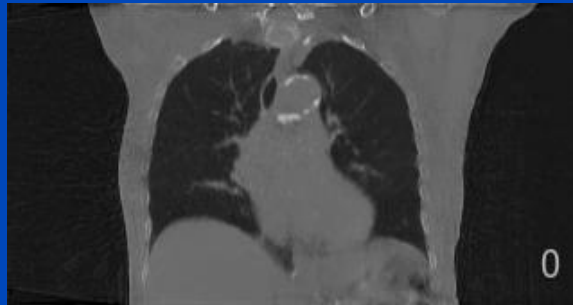
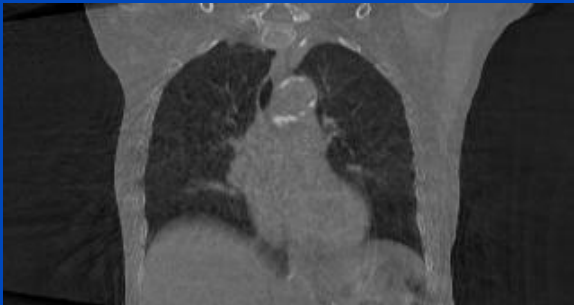
Hypersight Patient Example

60 s Scan

FDK recon (3D)



SAMoCo recon (true 4D)



60 s, 200° short scan, 867 projections, MA_53_Lung_60s.
Displayed are 434 time points with 140 ms increment at 10 fps.

6 s Scan

FDK recon (3D)

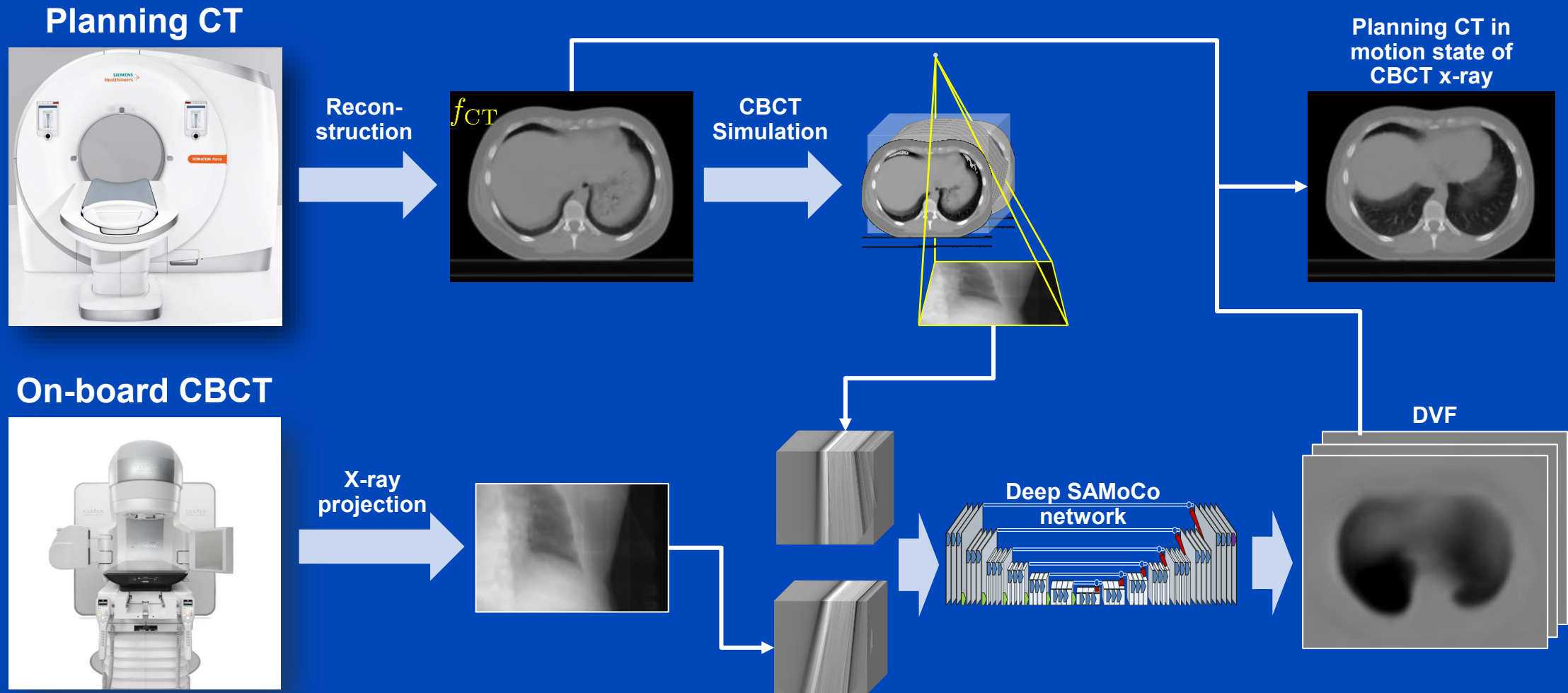


SAMoCo recon (true 4D)

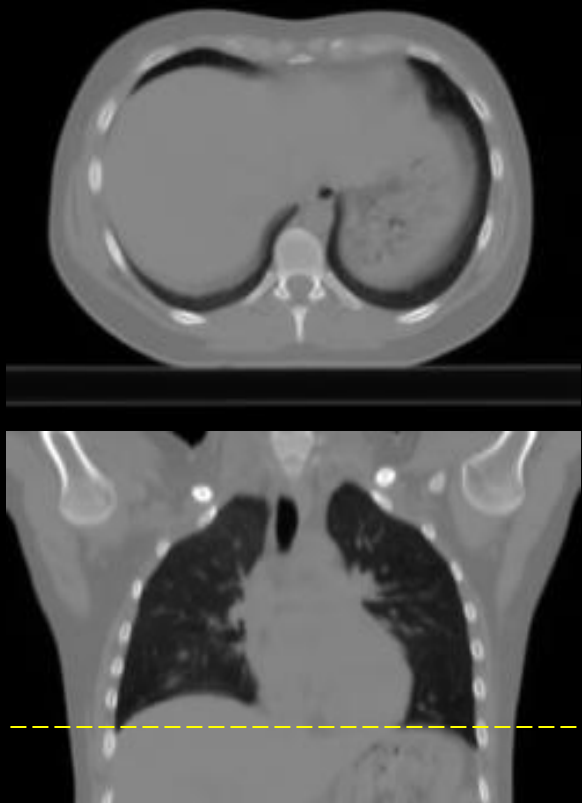


6 s, 200° short scan, 406 projections, MA_53_Lung_BH_6s
Displayed are 41 time points with 140 ms increment at 10 fps.

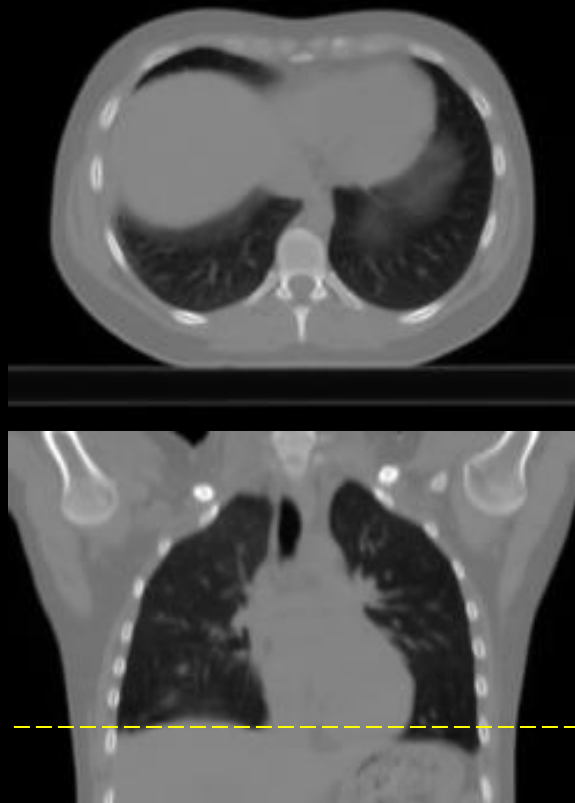
Experiment: Deform Planning CT



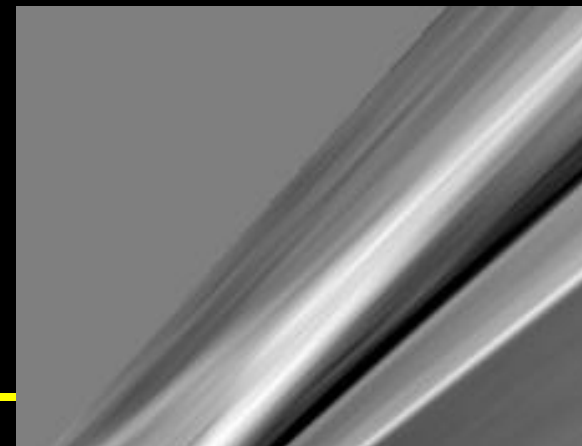
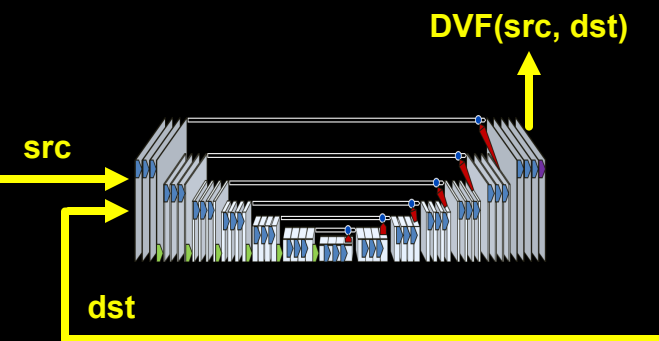
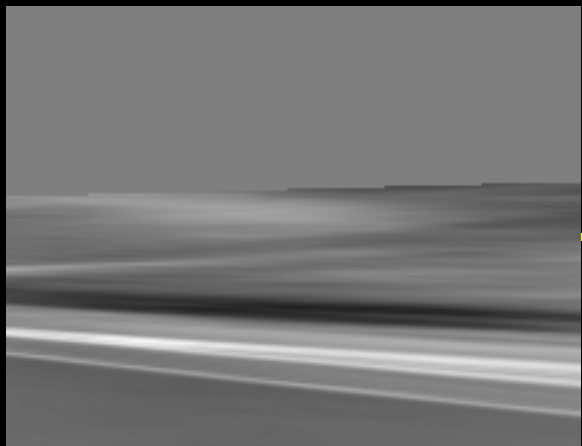
Planning CT
at source time t_{src}

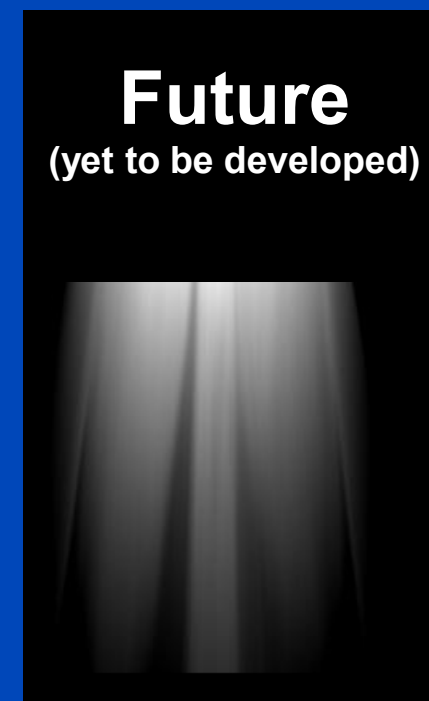
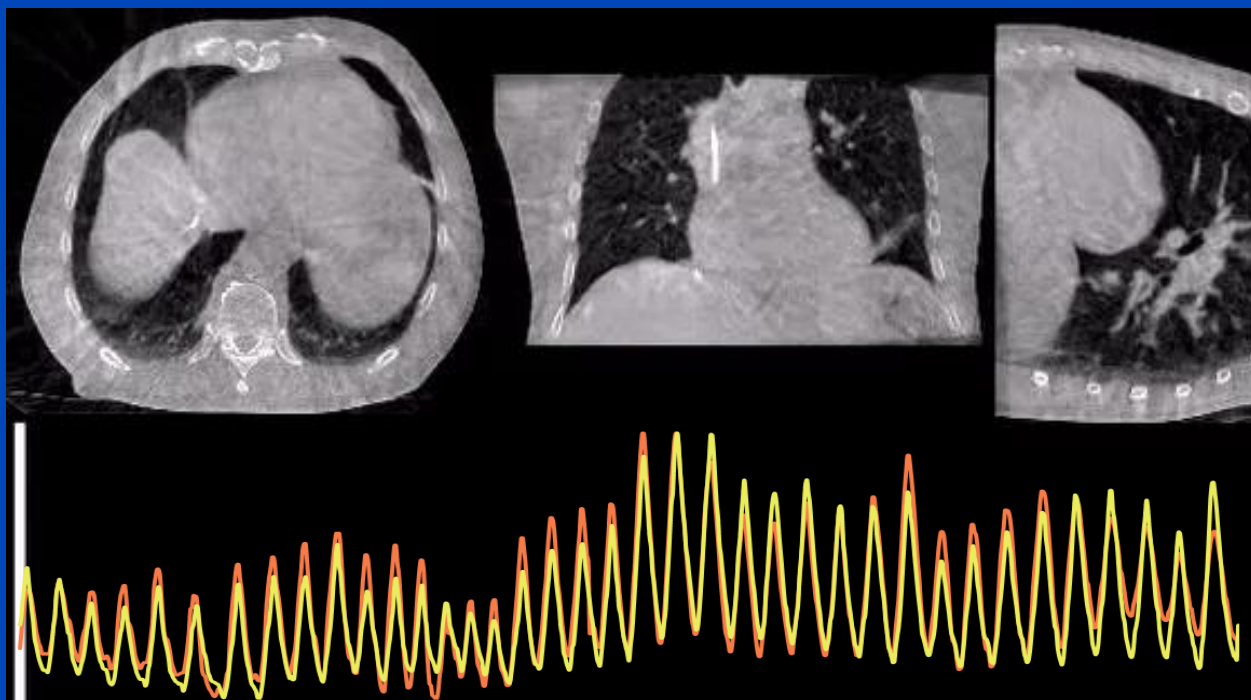


Planning CT deformed
to destination time t_{dst}

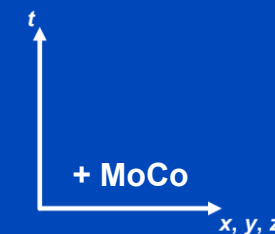


CBCT SAMoCo
for destination time t_{dst}



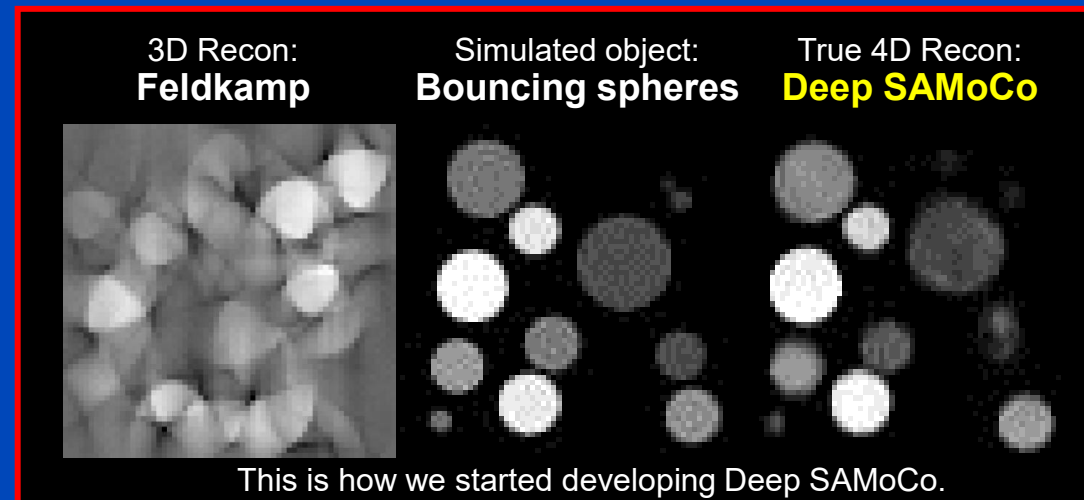


Imaging ($t < 0$) Treatment ($t > 0$)



Conclusions and Outlook

- Conventional 4D (cyclic 4D) collapses time onto a periodic phase.
- Deep SAMoCo 4D (true 4D) reconstructs time as a true dimension.
 - Motion does not need to be periodic.
 - Rotation speed does not matter.
- Deep SAMoCo allows to track structures in 3D, given x-ray images during treatment.
 - However: Single view x-ray data during treatment currently not available to us.



Thank You!

This presentation will soon be available at www.dkfz.de/ct.

Job opportunities through marc.kachelriess@dkfz.de or through DKFZ's international PhD or Postdoctoral Fellowship programs.

Parts of the reconstruction software were provided by RayConStruct® GmbH, Nürnberg, Germany.