

Living at the K-Edge: Is it Iodine Forever?

Marc Kachelrieß

German Cancer Research Center (DKFZ)

Heidelberg, Germany

www.dkfz.de/ct



DEUTSCHES
KREBSFORSCHUNGSZENTRUM
IN DER HELMHOLTZ-GEMEINSCHAFT

Disclaimer

- This talk is about physics.
- This talk is not about chemistry.
- Contrast agent in this talk refers to the atom that generates the contrast and not to the molecule into which the atom is integrated.
- Other atoms in such molecules typically are H, C, N, O and have atomic numbers as 1, 6, 7, and 8 and thus are x-ray interaction-wise not much different from water or soft tissue.
- Contrast is generated by high Z materials, and by high densities.

Can CT do Molecular Imaging?

- To obtain an enhancement of 100 HU, in the order of 10^{19} atoms iodine (or gadolinium) per mL are required.¹
- A human cell approximately occupies a sphere of 25 μm diameter.
- Thus, in the order of 10^{11} iodine (or gadolinium) need to be populated within or on the surface of a cell.

- The answer is: No 😞

- Why not?
 - PET requires only about 10^8 tracer atoms per mL and thus about 1 per cell².
 - PET tracer atoms shout “We are here!”.
 - CT iodine atoms are quiet and need to be probed by an x-ray photon.
 - There are not more than 10^5 x-ray photons probing a mm^2 . Many iodine atoms are needed to increase the likelihood of having some of the x-ray photons hit an iodine atom.

¹About $2.3 \cdot 10^{22}$ iodine atoms fit into a mL and make about 128 kHU. Scaling linearly down to 100 HU yields about $1.8 \cdot 10^{19}$ iodine atoms per mL.

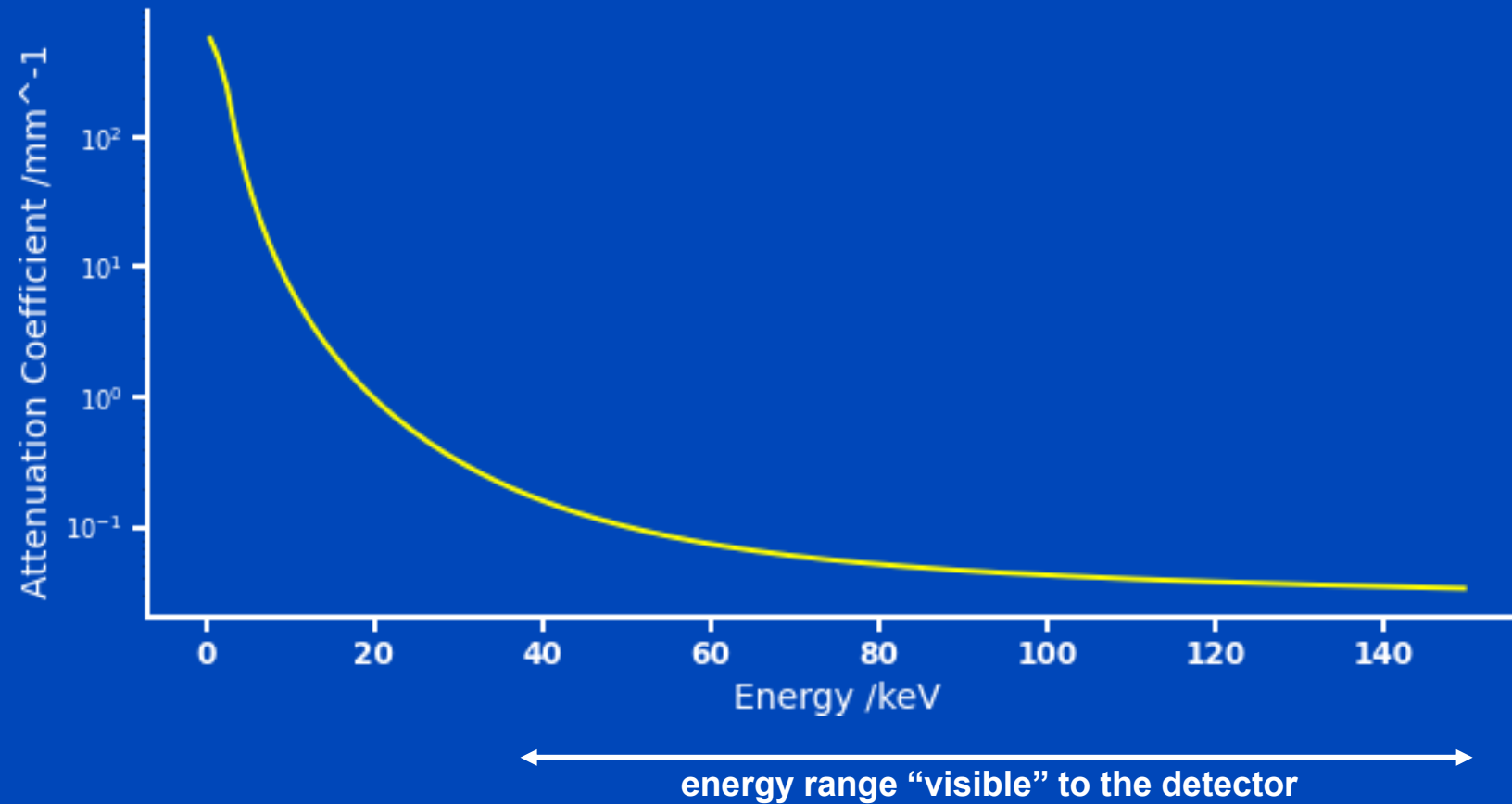
²C.S. Levin. New Imaging Technologies to Enhance the Molecular Sensitivity of Positron Emission Tomography. IEEE Proc., vol. 96(3):439-467, 2008.

Element	Z	K-edge	HVL	HVL×ρ	Hygros.	Cost (2025)	Machinability		
Silicon	14	1.8 keV	13.213 mm	3.08 g/cm ²	Low	1.70 \$/kg	Moderate	} Used or proposed as prefilter	
Calcium	20	4.0 keV	11.862 mm	2.05 g/cm ²	High	2.28 \$/kg	Low		
Copper	29	9.0 keV	1.001 mm	0.89 g/cm ²	Low	6.00 \$/kg	High		
Silver	47	25.5 keV	0.251 mm	0.26 g/cm ²	Low	521.00 \$/kg	High		
Cadmium	48	26.7 keV	0.293 mm	0.25 g/cm ²	Low	4.10 \$/kg	Low		
Tin	50	29.2 keV	0.315 mm	0.23 g/cm ²	Low	18.70 \$/kg	High		
Iodine	53	33.2 keV	0.404 mm	0.20 g/cm ²	Moderate	35.00 \$/kg	Low		} K-edges quite low to discriminate Ca and CA.
Barium	56	37.4 keV	0.505 mm	0.18 g/cm ²	High	0.26 \$/kg	Low		
Cerium	58	40.4 keV	0.239 mm	0.16 g/cm ²	Moderate	4.64 \$/kg	Moderate		
Gadolinium	64	50.2 keV	0.169 mm	0.13 g/cm ²	Moderate	28.60 \$/kg	Moderate		
Holmium	67	55.6 keV	0.164 mm	0.14 g/cm ²	Moderate	57.10 \$/kg	Moderate	} K-edges covered by most kV	
Ytterbium	70	61.3 keV	0.190 mm	0.13 g/cm ²	Moderate	17.10 \$/kg	Moderate		
Hafnium	72	65.4 keV	0.098 mm	0.13 g/cm ²	Low	900.00 \$/kg	Moderate		
Tantalum	73	67.4 keV	0.079 mm	0.13 g/cm ²	Low	305.00 \$/kg	Low		
Tungsten	74	69.5 keV	0.071 mm	0.14 g/cm ²	Low	35.30 \$/kg	Low		
Gold	79	80.7 keV	0.076 mm	0.15 g/cm ²	Low	44800.00 \$/kg	Moderate		
Bismuth	83	90.5 keV	0.170 mm	0.16 g/cm ²	Low	6.61 \$/kg	Moderate		

HVLs are calculated for the 120 kV Tucker spectrum with intrinsic + 32 cm water prefiltration as seen for a 1.6 mm CdTe sensor above 20 keV.

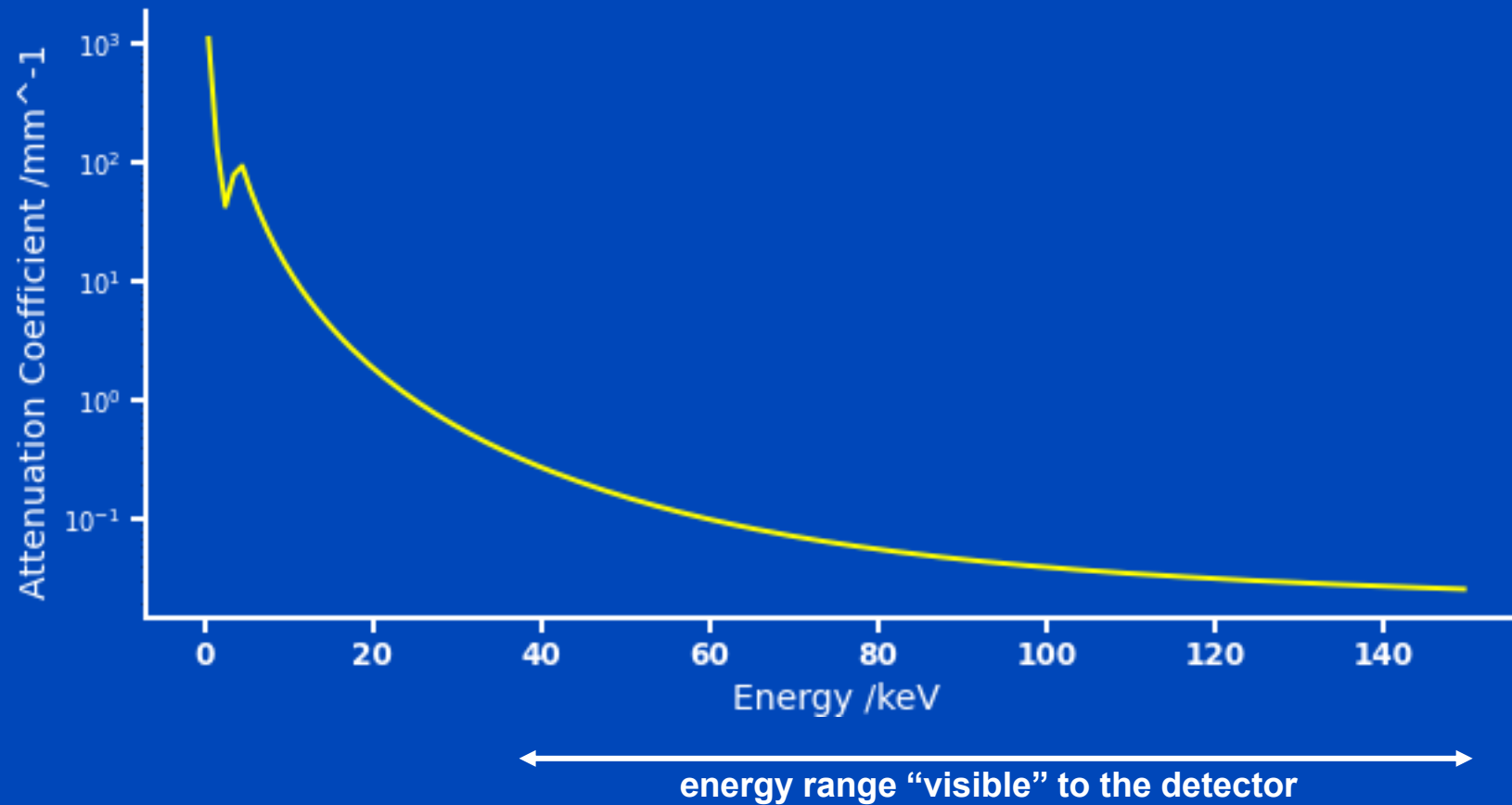
Attenuation Coefficients

Attenuation coefficient of silicon



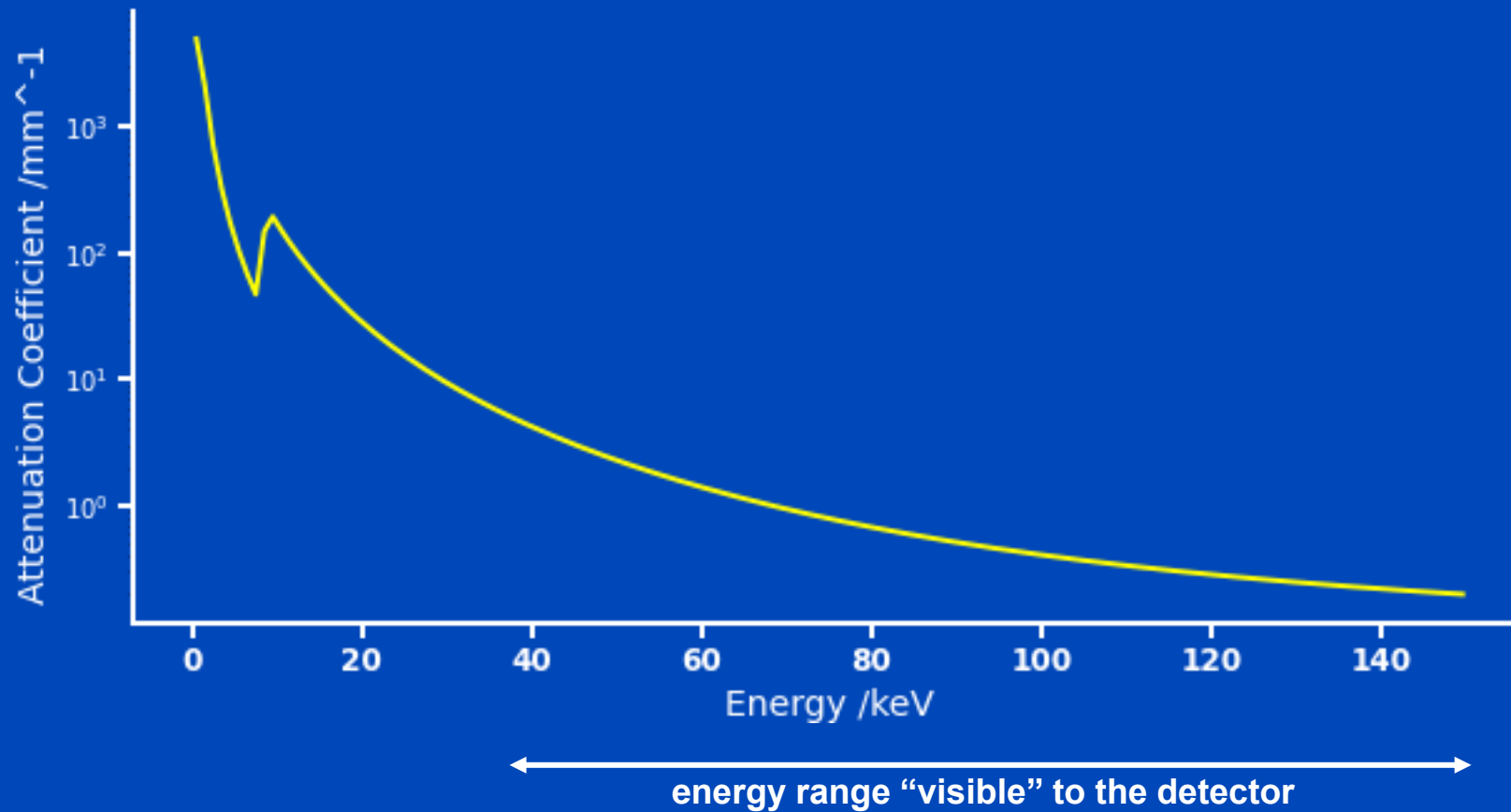
Attenuation Coefficients

Attenuation coefficient of calcium



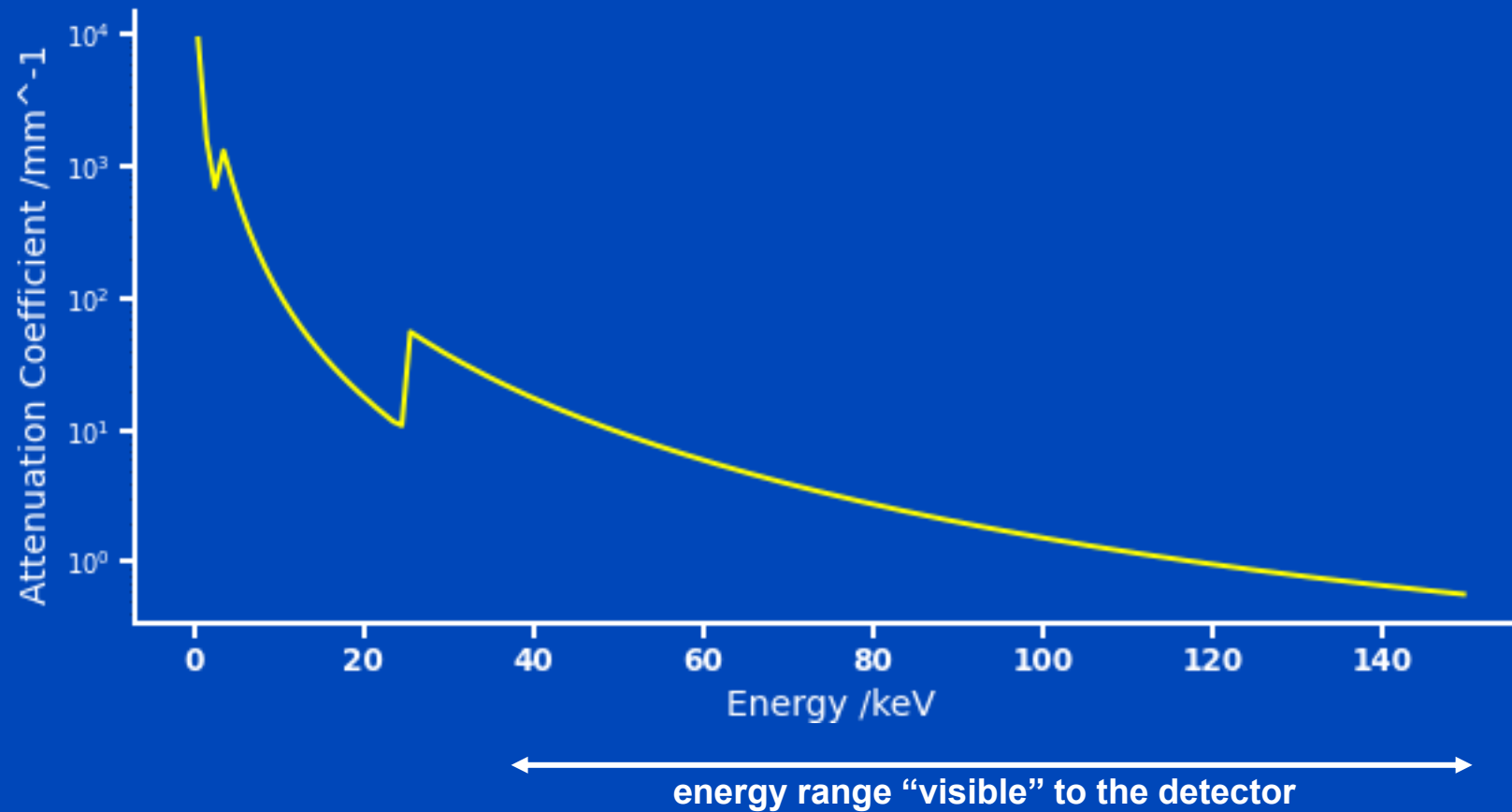
Attenuation Coefficients

Attenuation coefficient of copper



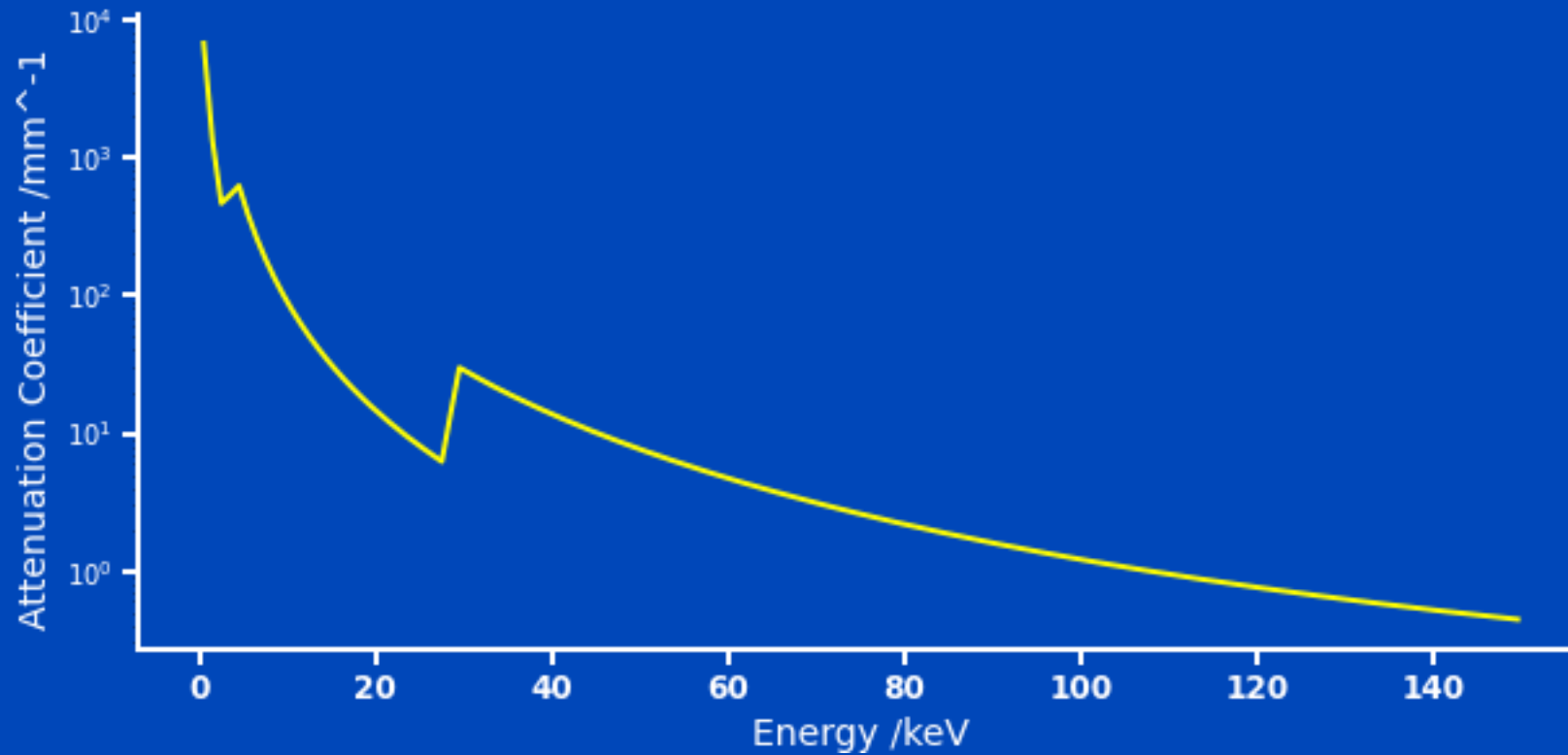
Attenuation Coefficients

Attenuation coefficient of silver



Attenuation Coefficients

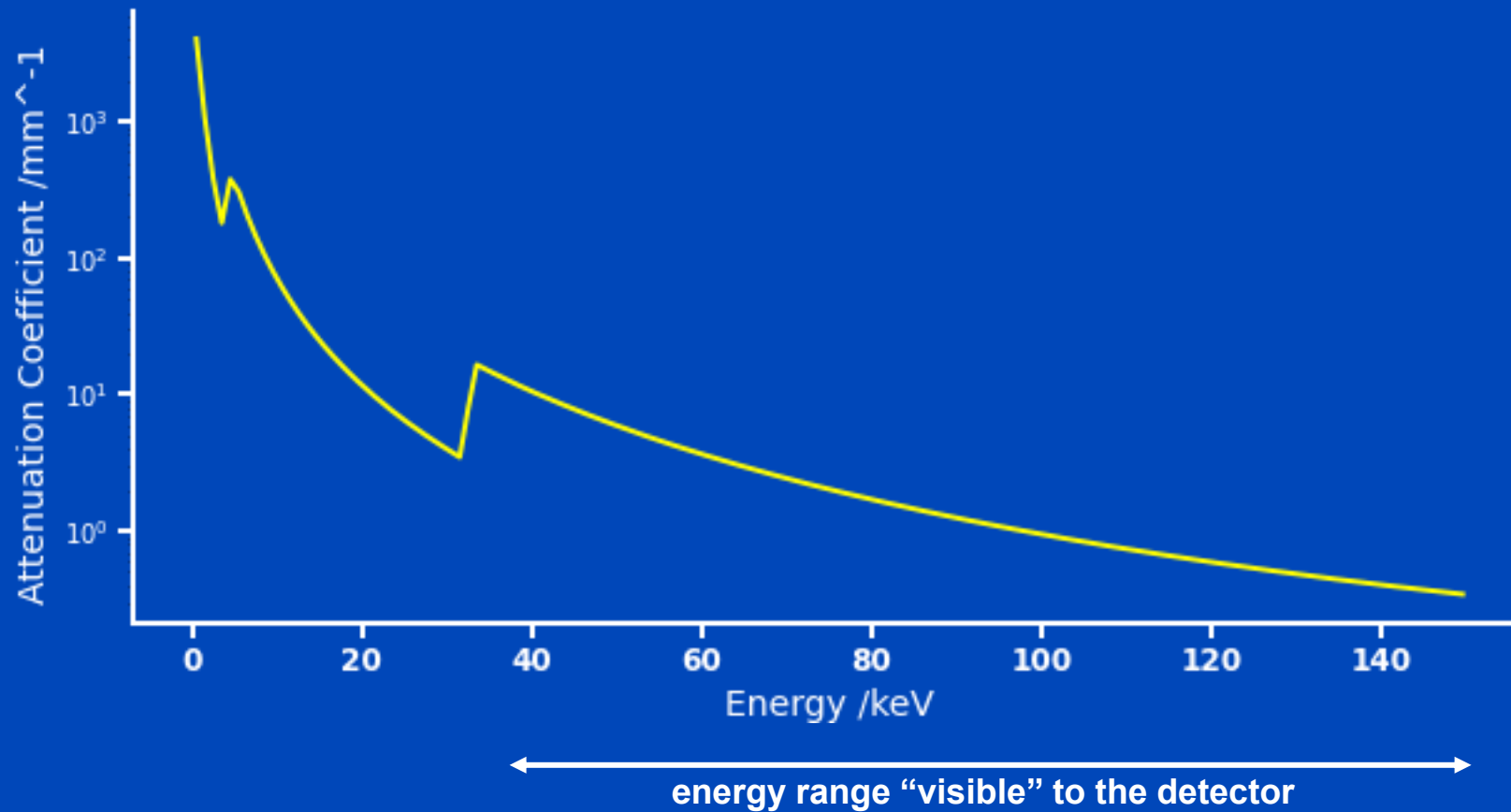
Attenuation coefficient of tin



← energy range “visible” to the detector →

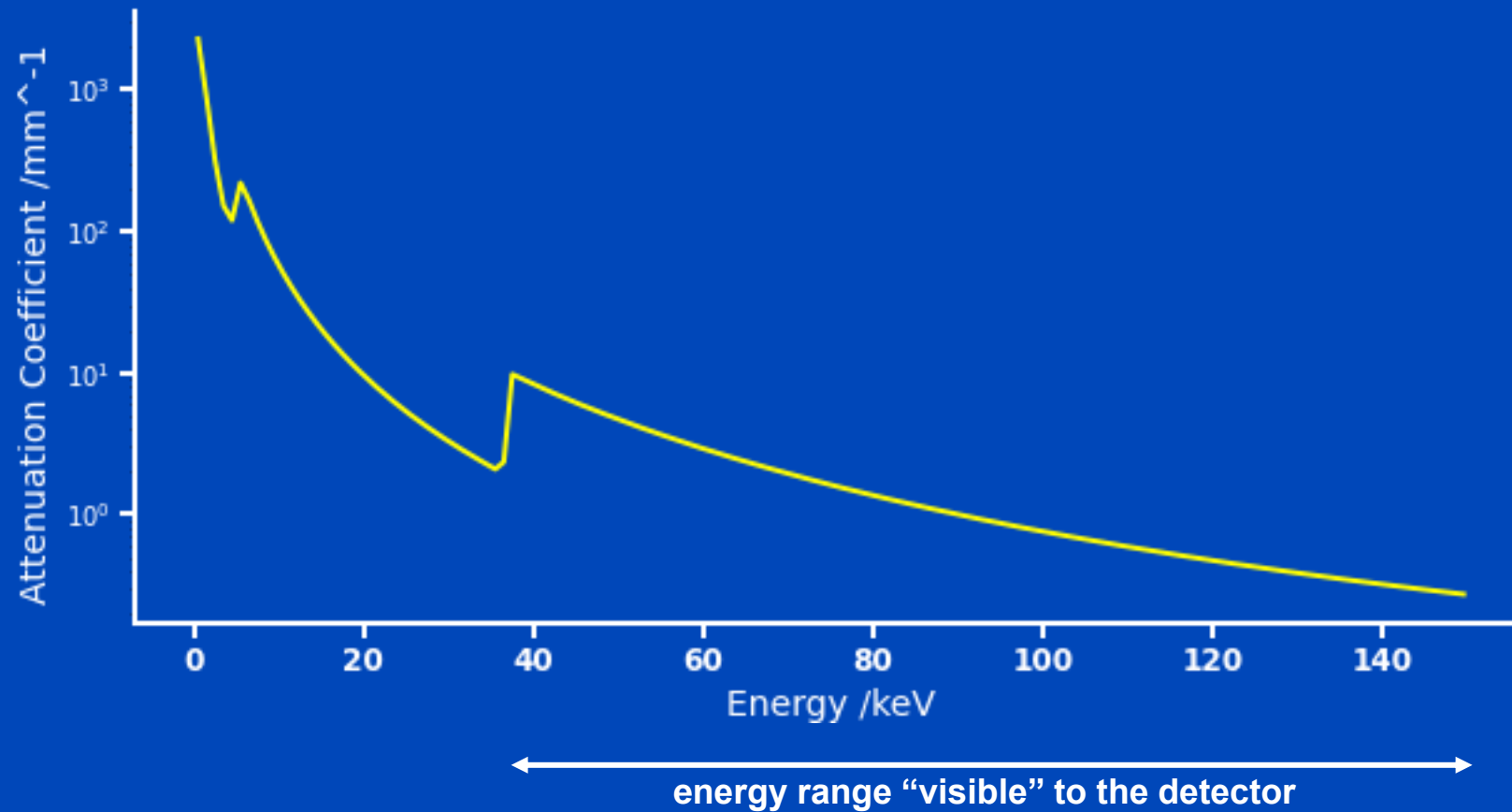
Attenuation Coefficients

Attenuation coefficient of iodine



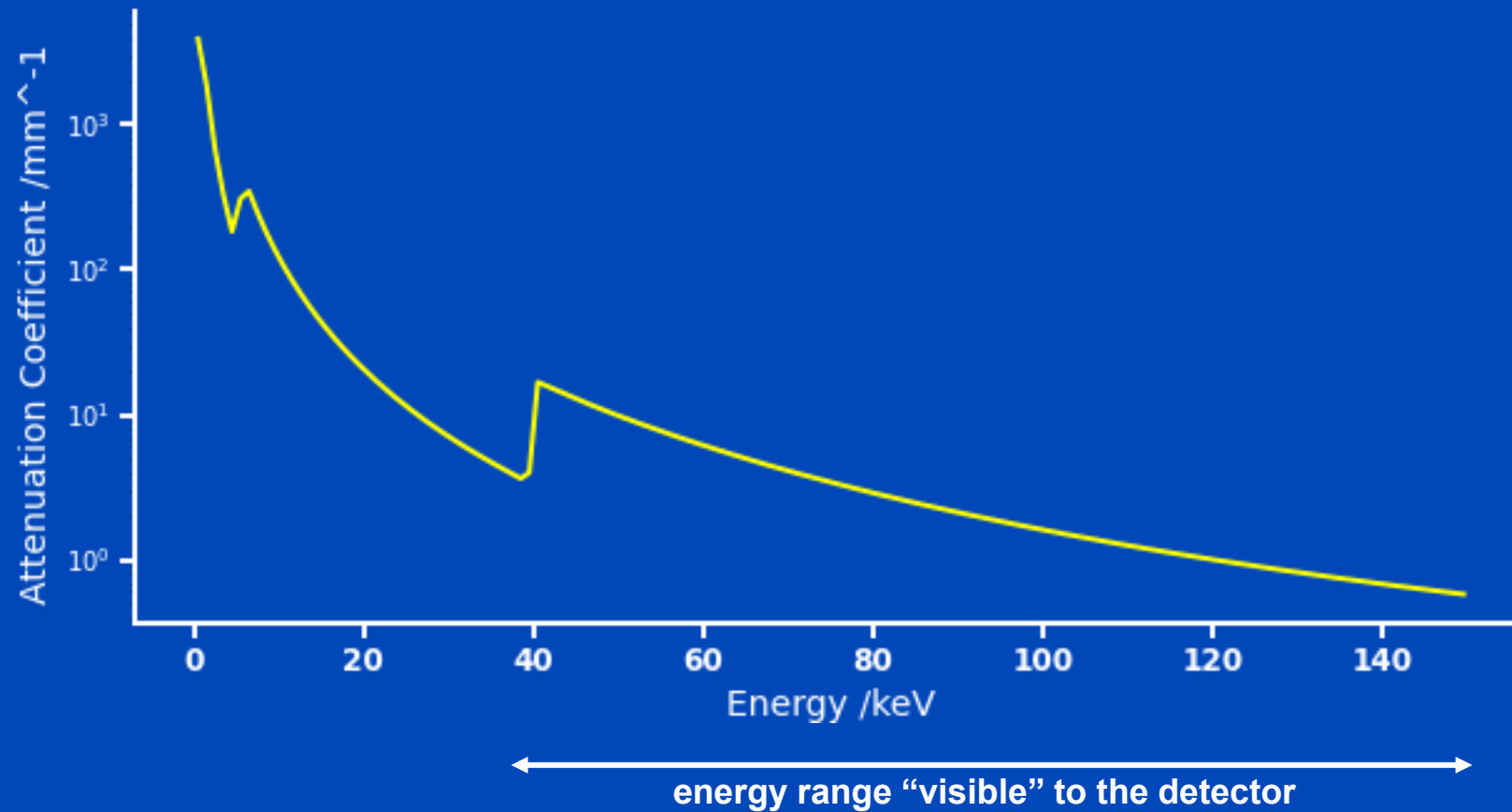
Attenuation Coefficients

Attenuation coefficient of barium



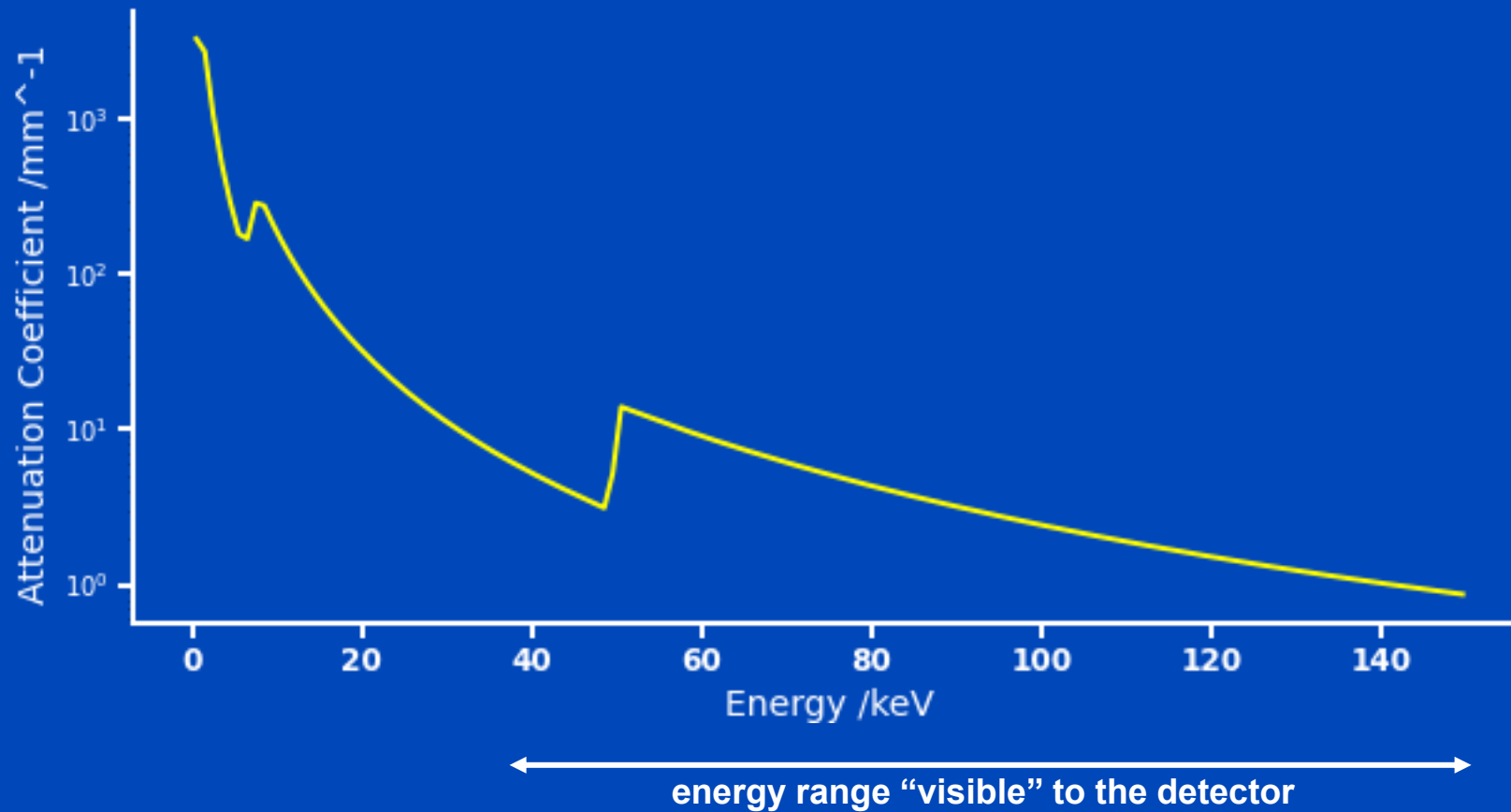
Attenuation Coefficients

Attenuation coefficient of cerium



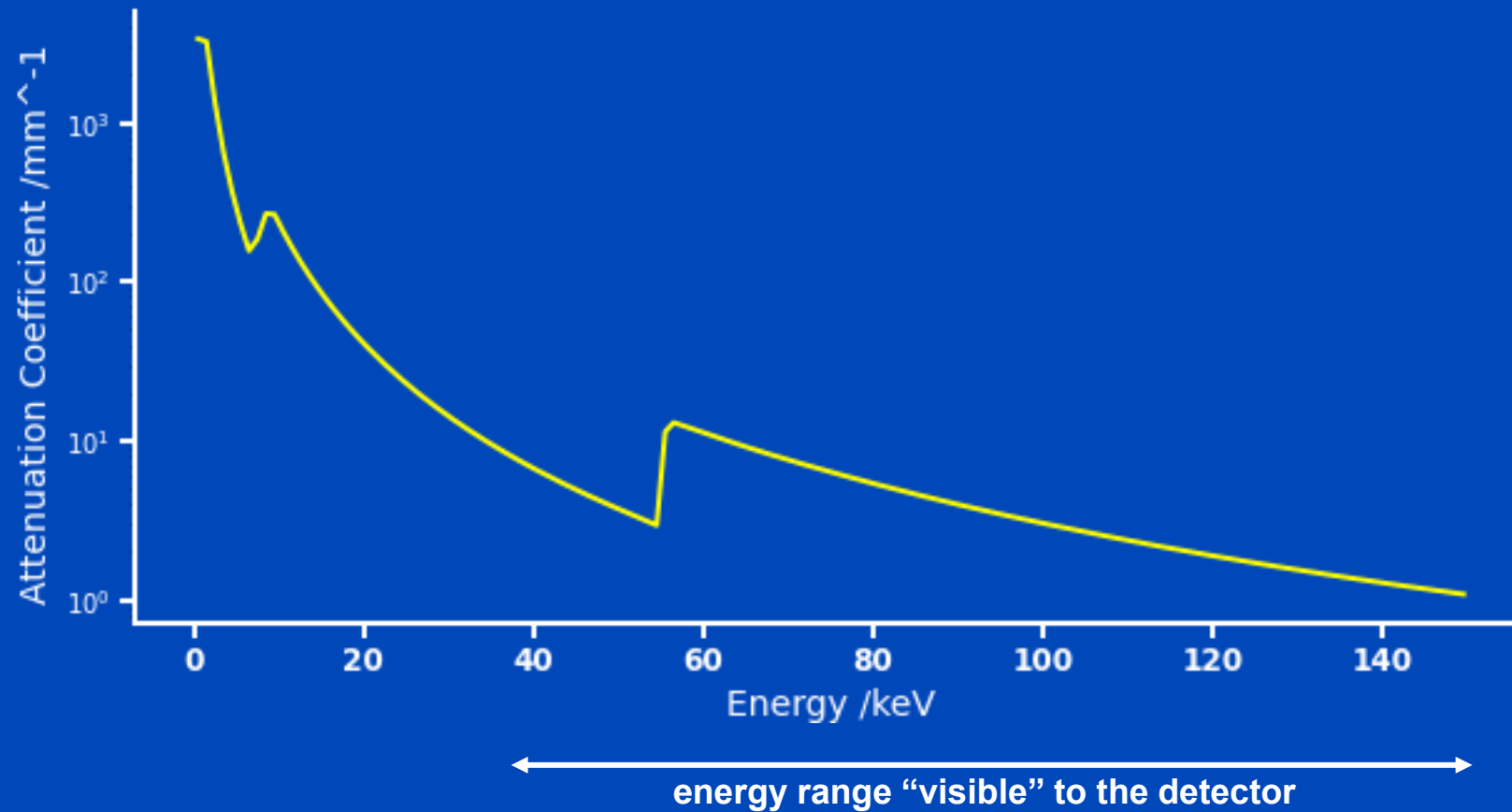
Attenuation Coefficients

Attenuation coefficient of gadolinium



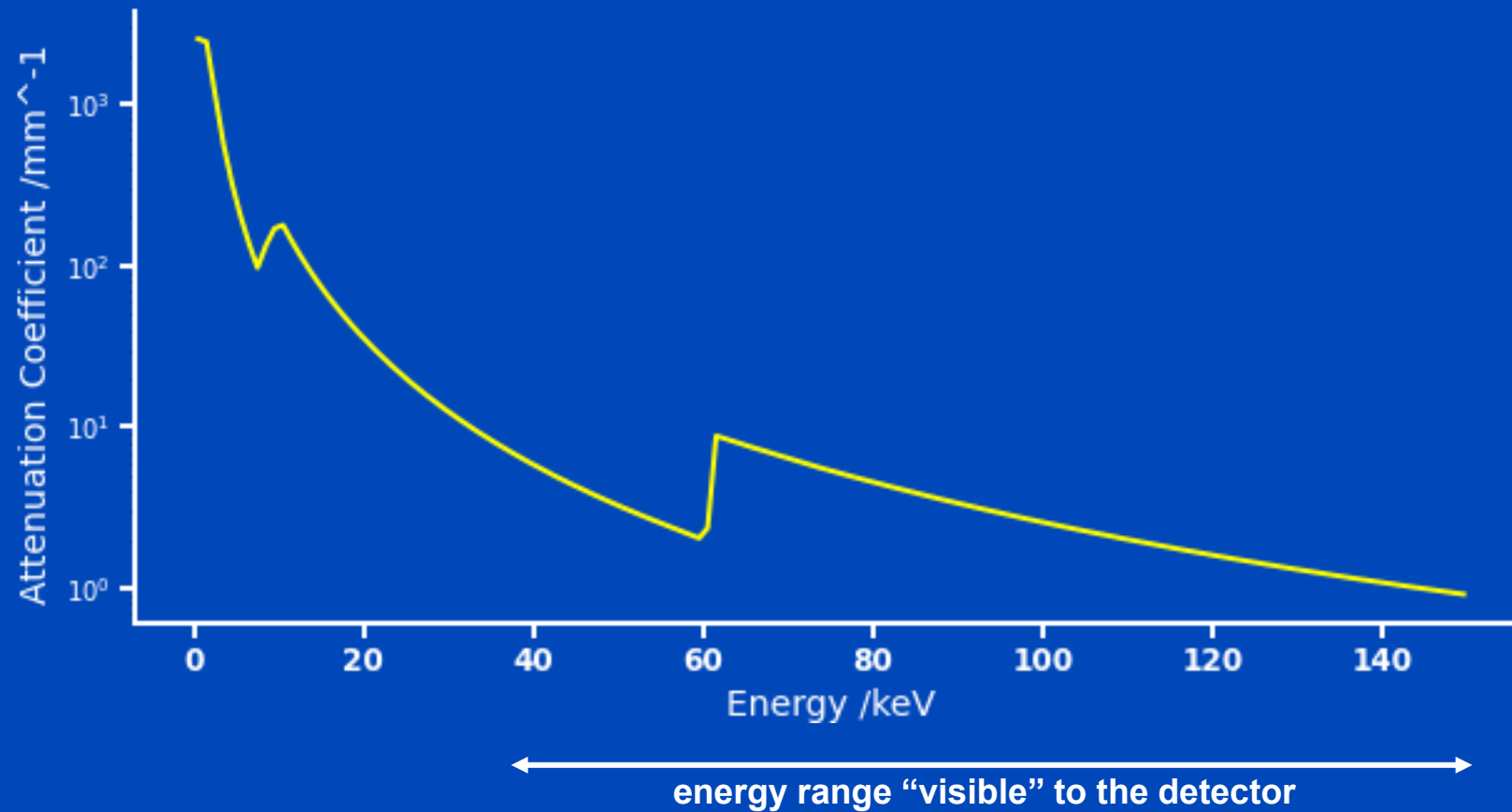
Attenuation Coefficients

Attenuation coefficient of holmium



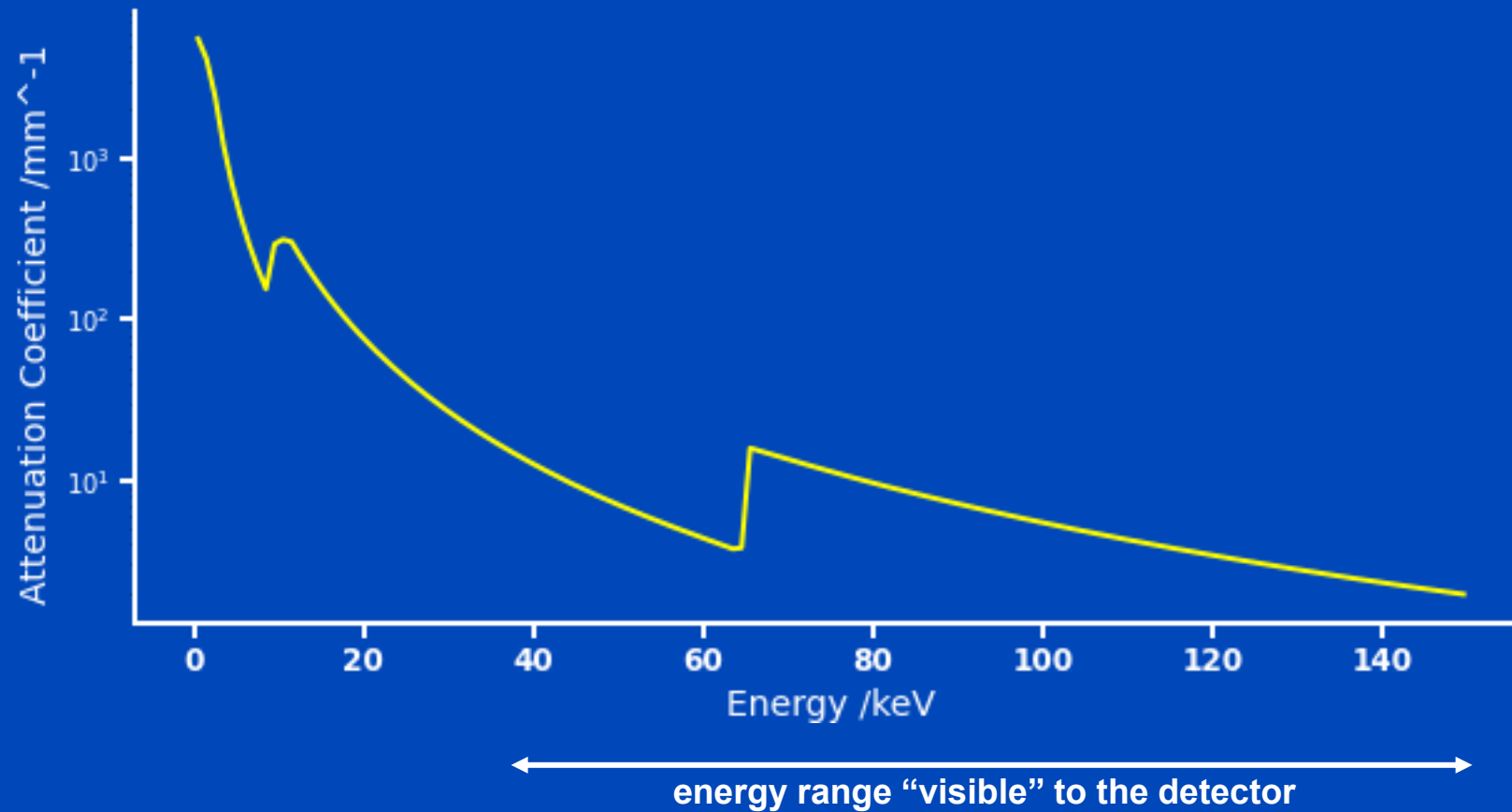
Attenuation Coefficients

Attenuation coefficient of ytterbium



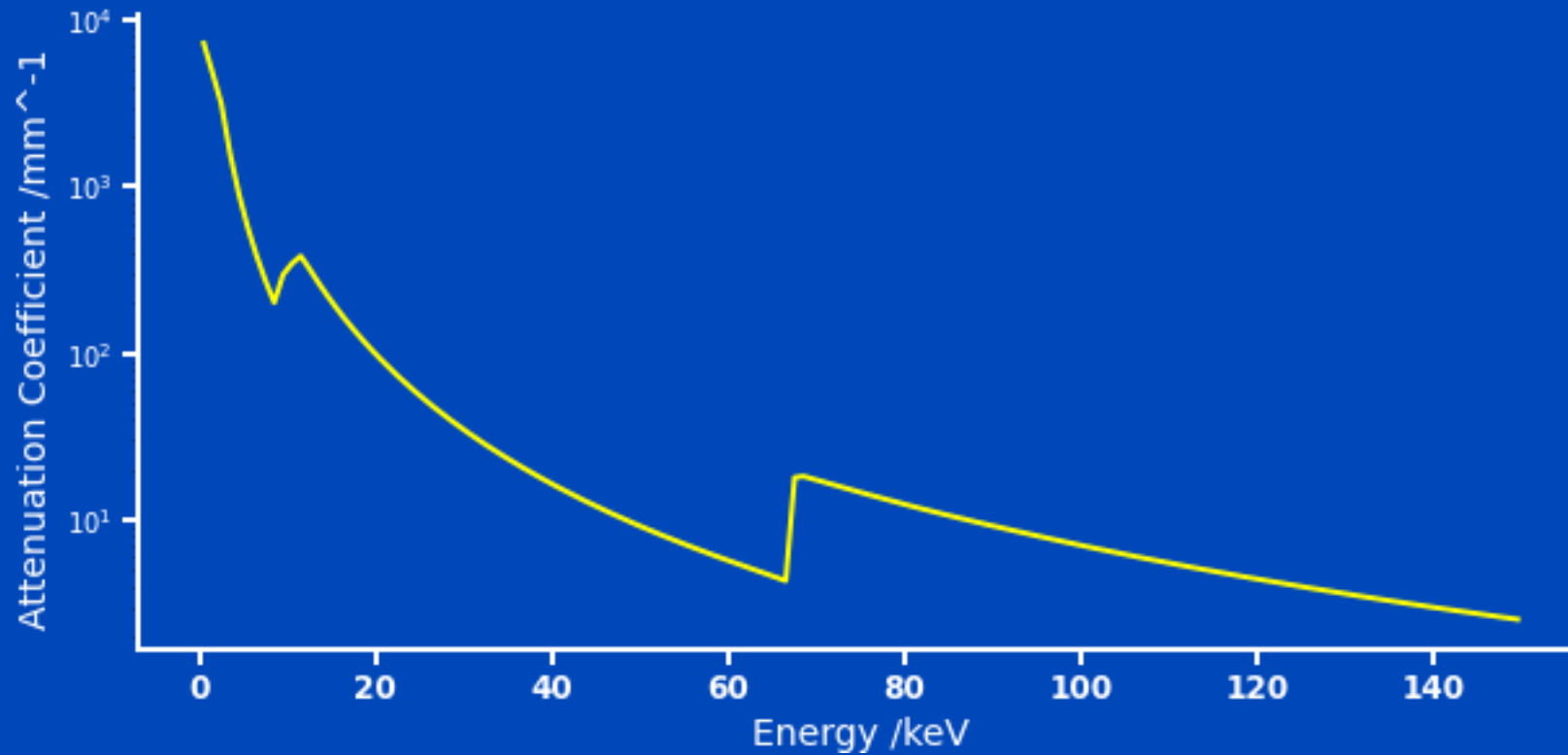
Attenuation Coefficients

Attenuation coefficient of hafnium



Attenuation Coefficients

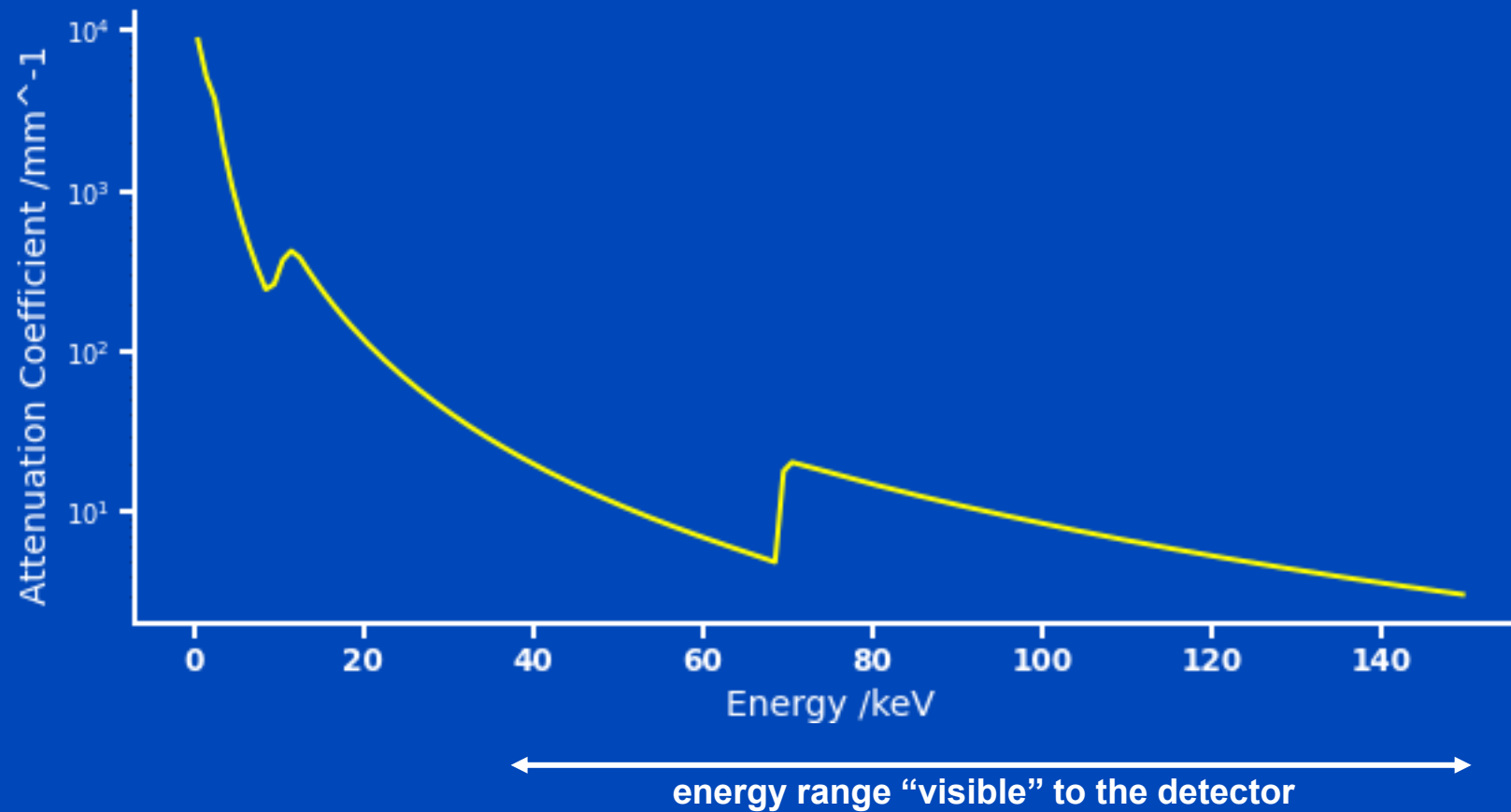
Attenuation coefficient of tantalum



← energy range “visible” to the detector →

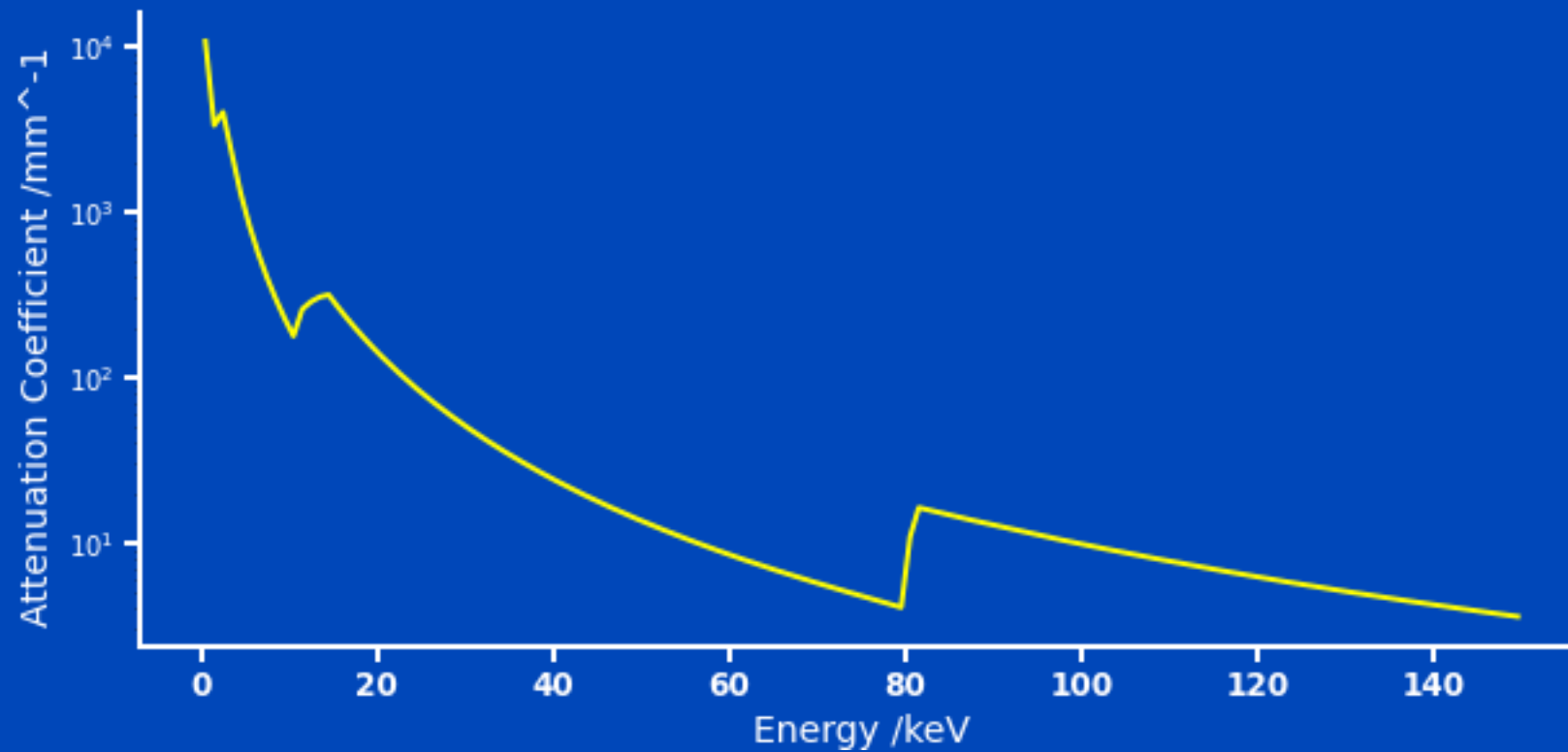
Attenuation Coefficients

Attenuation coefficient of tungsten



Attenuation Coefficients

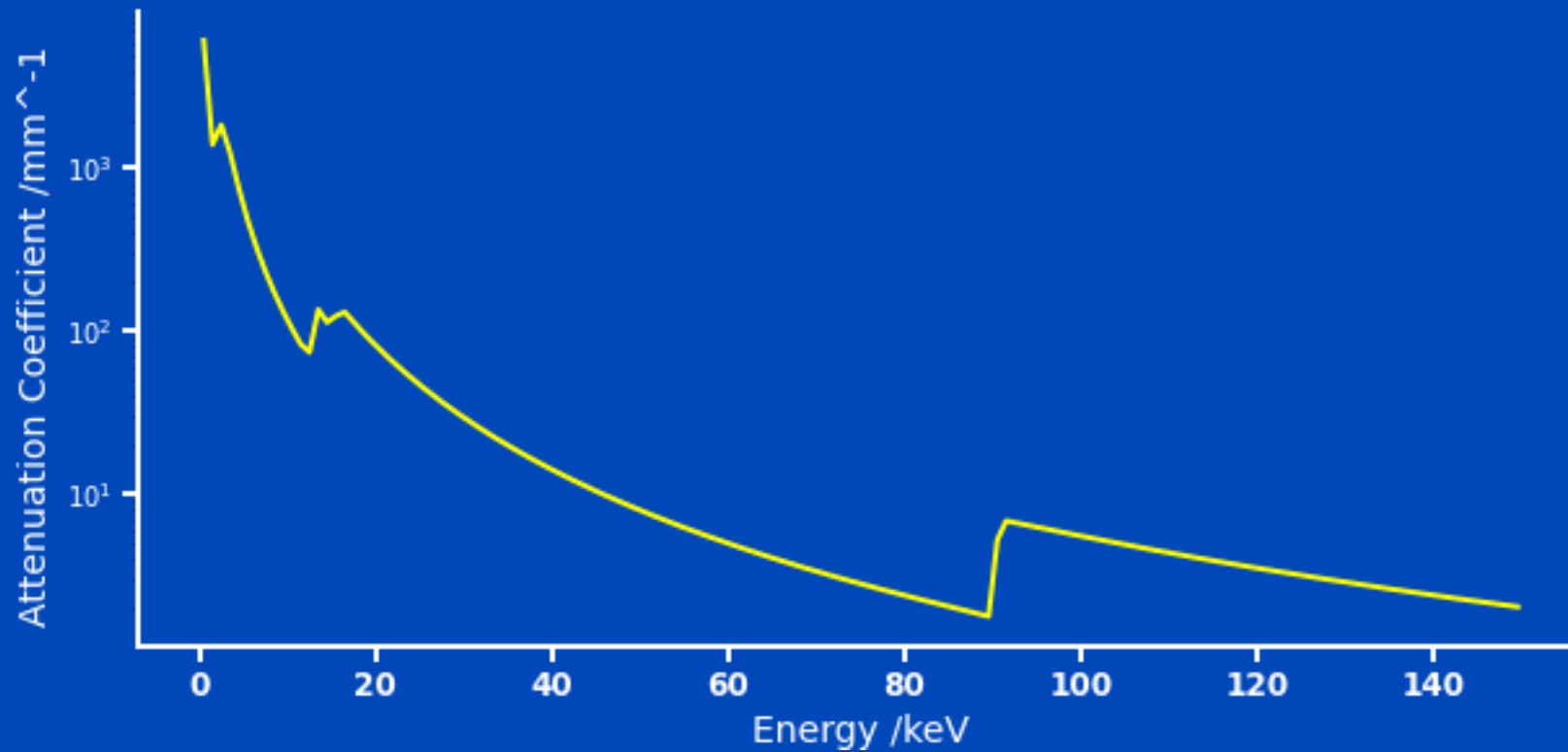
Attenuation coefficient of gold



energy range "visible" to the detector

Attenuation Coefficients

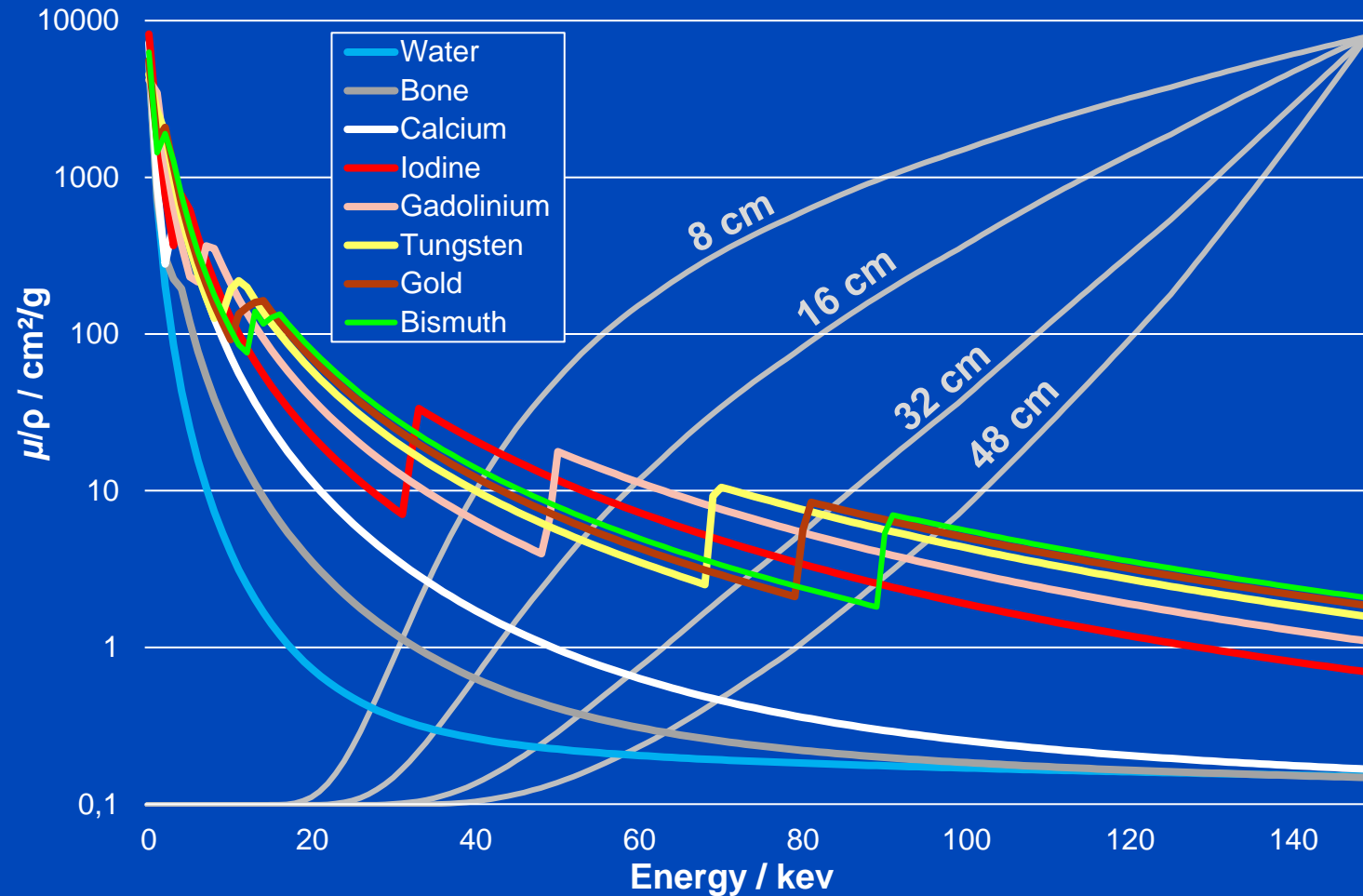
Attenuation coefficient of bismuth



More than Two Materials?

$$\mu(\mathbf{r}, E) = f_1(\mathbf{r})\psi_1(E) + f_2(\mathbf{r})\psi_2(E) + \underbrace{f_3(\mathbf{r})\psi_3(E) + \dots}_{\text{Only, if we inject high } Z \text{ materials!}}$$

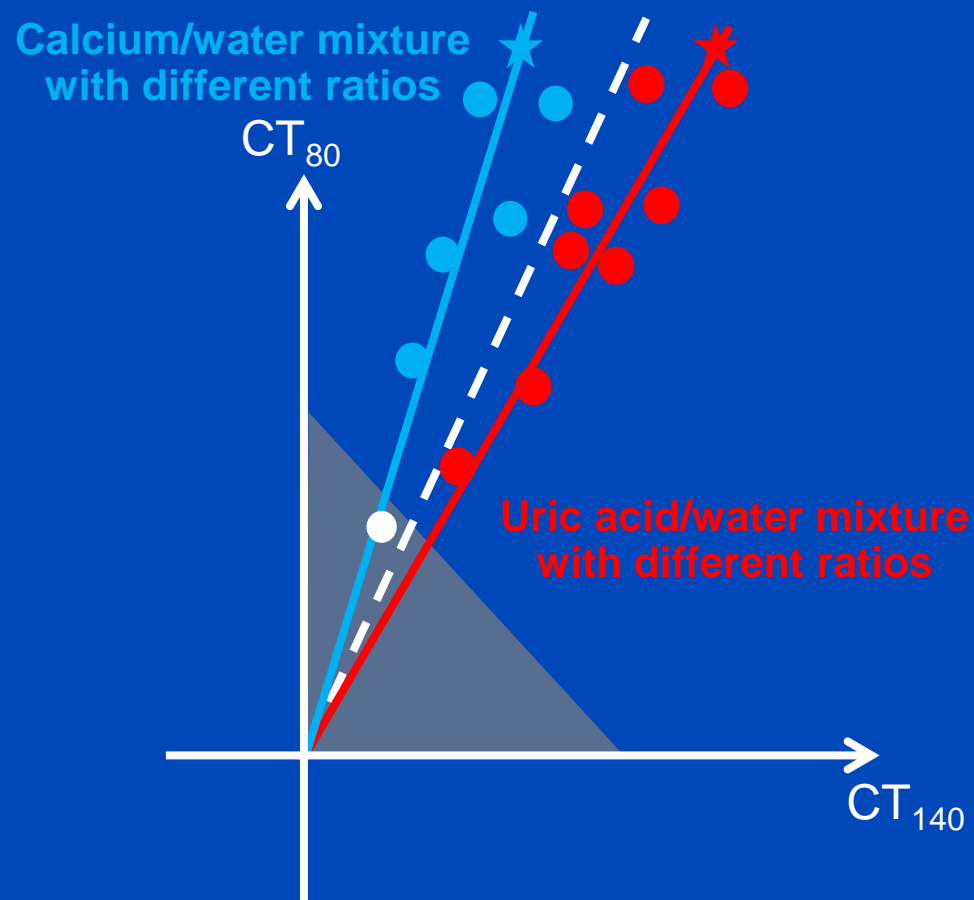
Only, if we inject high Z materials!



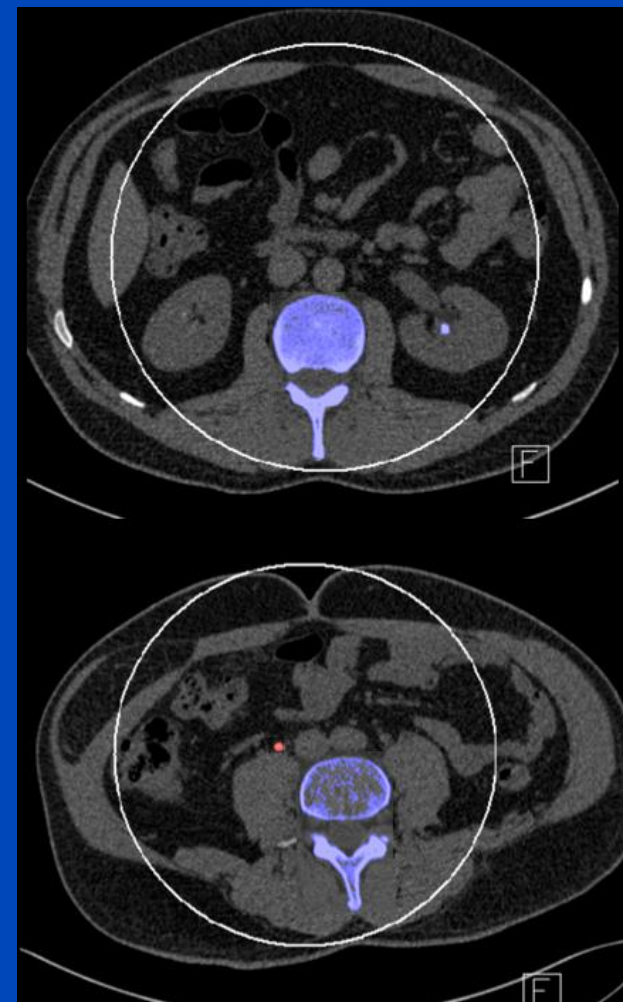
Element	K-edge
O (61%)	< 1 keV
C (23 %)	< 1 keV
H (10%)	< 1 keV
N (2.6%)	< 1 keV
Ca (1.7 %)	4.0 keV
P (1.1%)	2.1 keV
I	33.2 keV
Gd	50.2 keV
W	69.5 keV
Au	80.7 keV
Bi	90.5 keV

Gray curves: 120 kV water transmission on a non-logarithmic ordinate individually normalized to 1 at 140 keV.

What? Only if we inject high Z materials?



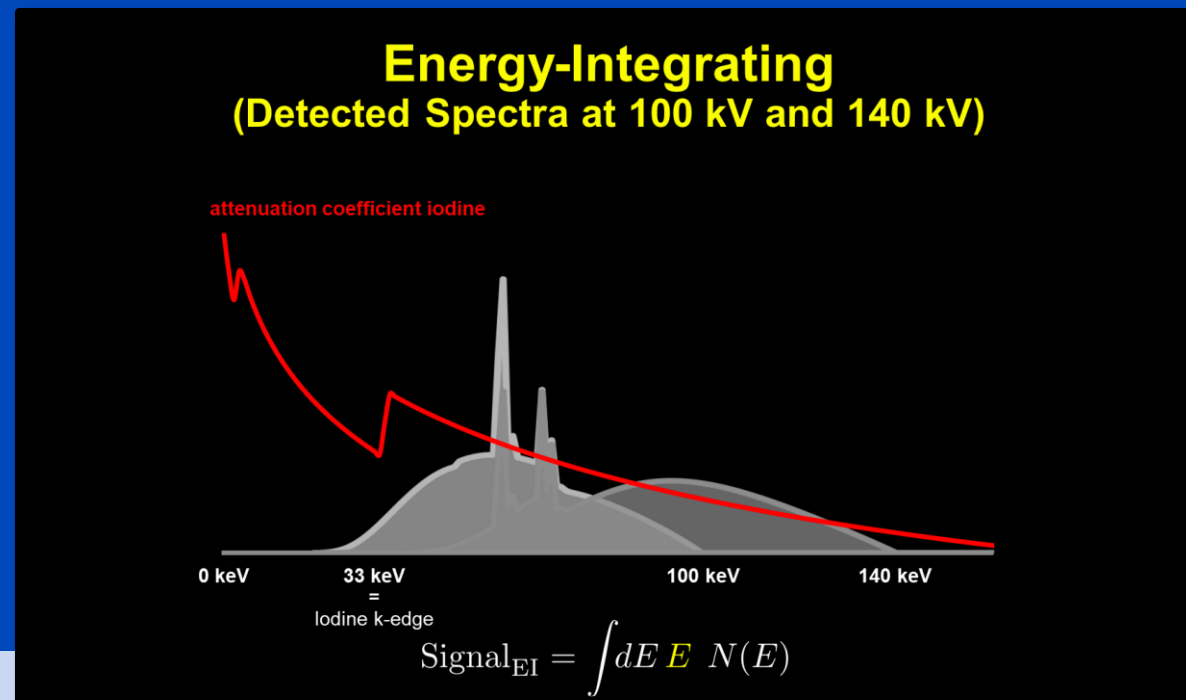
- ★ ★ Pure calcium and pure uric acid
- ● Measured bone and uric acid



Courtesy of Klinikum Großhadern, LMU München and of Siemens Healthineers

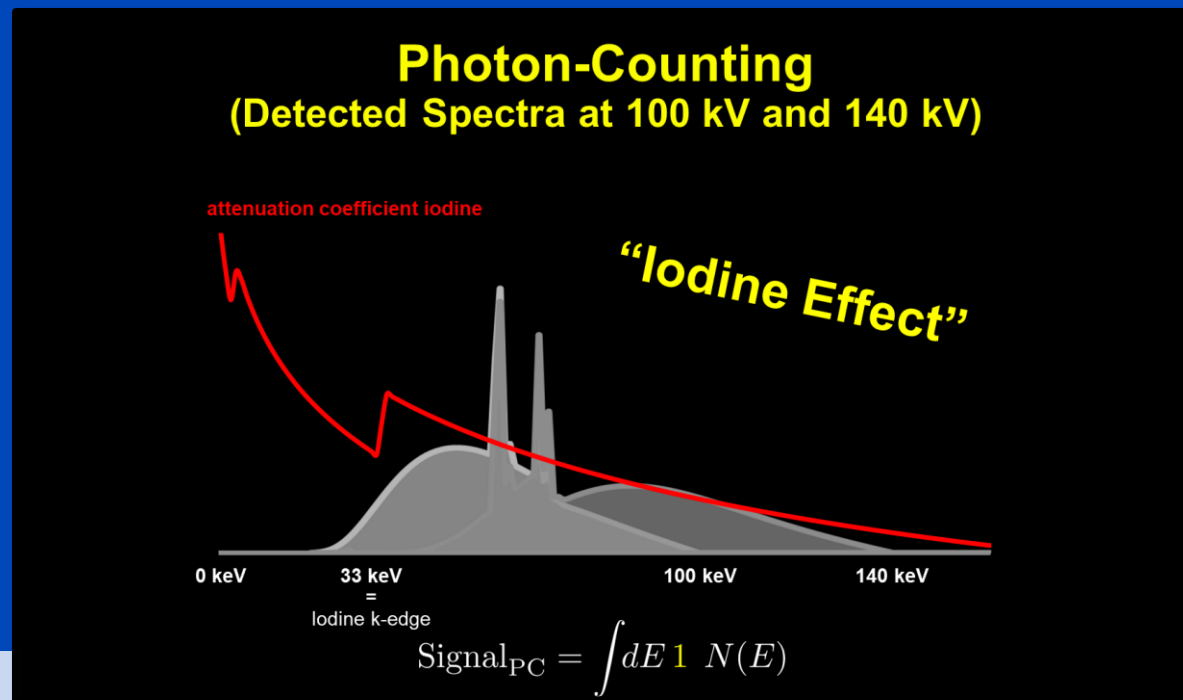
Iodine in Conventional (Non-Spectral CT)

- Is used successfully for decades as the CT contrast agent.
- However:
 - Iodine's k-edge is at 33 keV and forces us to scan with low kV, e.g. 70 kV.
 - Iodine contrast decreases at higher kV, and thus for thicker patients.
- Contrast agents (CAs) with higher k-edges may thus have an advantage
 - Unclear, how great this advantage is. We are doing very well with iodine for decades!



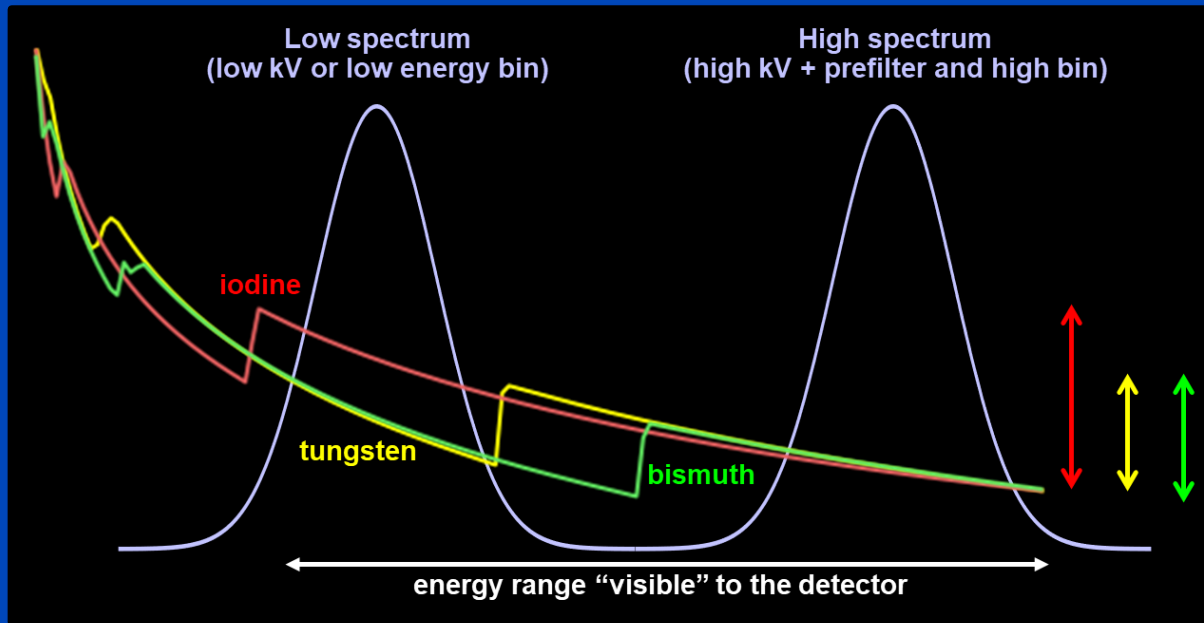
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Iodine in Spectral CT

- Is the best contrast for VNC + CA map material decomposition
 - High contrast at the low end and low contrast at the high end of the photon energies.
 - Spectra (incl. PCCT thresholds) can be best selected to probe those extremes.



Element	Z	K-edge	$\frac{\mu_{\max} - \mu_{\min}}{\mu_{\min}}$
Iodine	53	33.2 keV	30.6
Barium	56	37.4 keV	30.3
Cerium	58	40.4 keV	28.0
Gadolinium	64	50.2 keV	15.1
Hafnium	72	65.4 keV	7.1
Tungsten	74	69.5 keV	5.7
Bismuth	83	90.5 keV	7.2

Values μ_{\min} and μ_{\max} determined in [40, 150] keV.

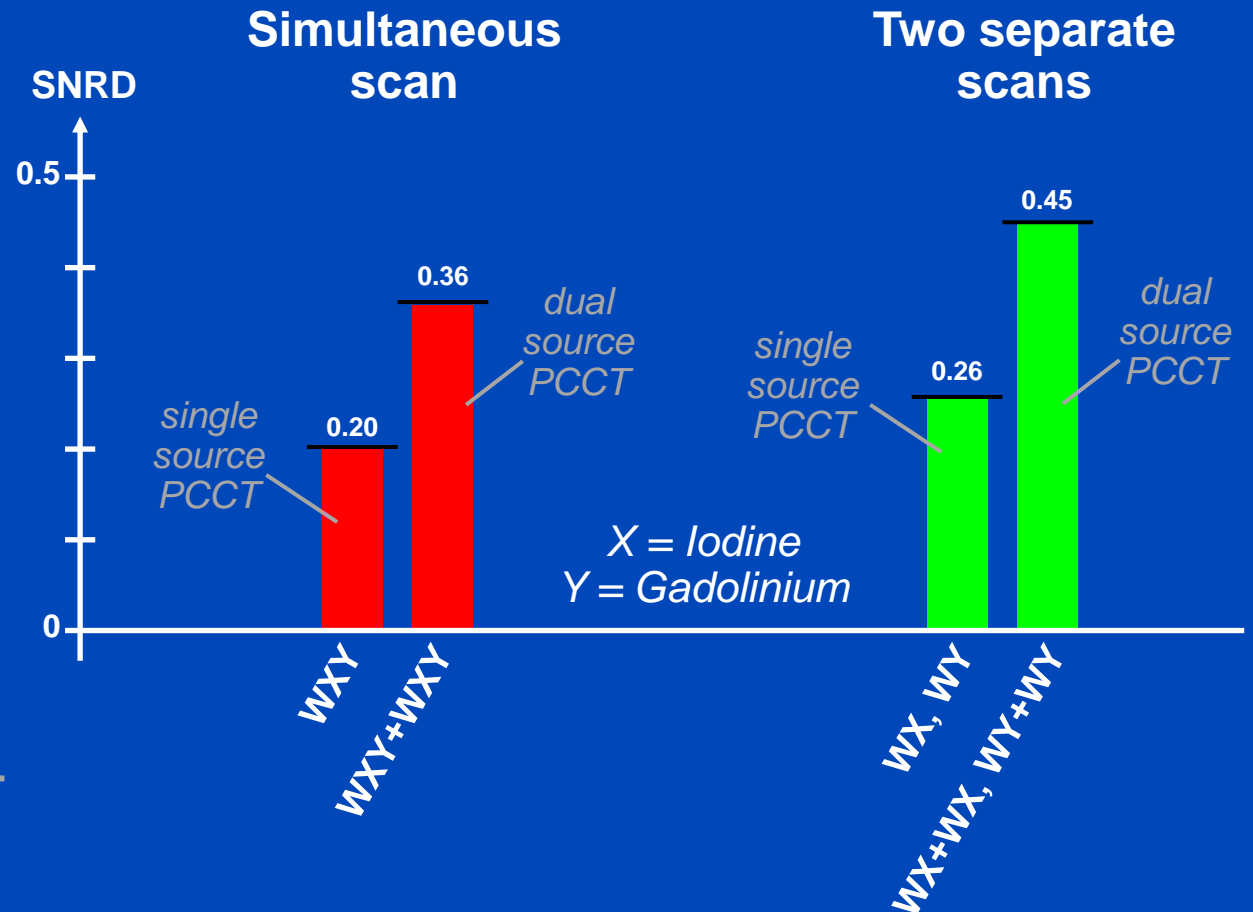
- Scanning with two different contrast agents, X and Y, say, simultaneously, does this make sense?

Proposals to Simultaneously use More than One Contrast Agent, X and Y

1. J. Schlomka, E. Roessler, R. Dorscheid, S. Dill, G. Martens, T. Istel, C. Baumer, C. Herrmann, R. Steadman, G. Zeitler, A. Livne, and R. Proksa. Experimental Feasibility of Multi-Energy Photon-Counting K-Edge Imaging in Pre-Clinical Computed Tomography. *Phys. Med. Biol.* 53, 4031-4047 (2008).
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3. J. Mongan, S. Rathnayake, Y. Fu, R. Wang, E. F. Jones, D.-W. Gao, and B. M. Yeh. In Vivo Differentiation of Complementary Contrast Media at Dual-Energy CT. *Radiology* 265, 267-272 (2012).
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5. D. P. Clark, K. Ghaghada, E. J. Moding, D. G. Kirsch, and C. T. Badea. In Vivo Characterization of Tumor Vasculature using Iodine and Gold Nanoparticles and Dual Energy Micro-CT. *Phys. Med. Biol.* 58, 1683-1704 (2013).
6. J. R. Ashton, D. P. Clark, E. J. Moding, K. Ghaghada, D. G. Kirsch, J. L. West, and C. T. Badea. Dual-Energy Micro-CT Functional Imaging of Primary Lung Cancer in Mice Using Gold and Iodine Nanoparticle Contrast Agents: A Validation Study. *PLoS ONE* 9, e88129 (2014).
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9. R. Symons, T. E. Cork, M. N. Lakshmanan, R. Evers, C. Davies-Venn, K. A. Rice, M. L. Thomas, C.-Y. Liu, S. Kappler, S. Ulzheimer, V. Sandfort, D. A. Bluemke, and A. Pourmorteza. Dual-Contrast Agent Photon-Counting Computed Tomography of the Heart: Initial Experience. *The International Journal of Cardiovascular Imaging* 33, 1253-1261 (2017).
10. R. Symons, B. Krauss, P. Sahbaee, T. E. Cork, M. N. Lakshmanan, D. A. Bluemke, and A. Pourmorteza. Photon-Counting CT for Simultaneous Imaging of Multiple Contrast Agents in the Abdomen: An in Vivo Study. *Med. Phys.* 44, 5120-5127 (2017).
11. R. Symons, B. Krauss, P. Sahbaee, T. E. Cork, M. N. Lakshmanan, D. A. Bluemke, and A. Pourmorteza. Photon-Counting CT for Simultaneous Imaging of Multiple Contrast Agents in the Abdomen: An in Vivo Study. *Med. Phys.* 44, 5120-5127 (2017).
12. D. Muenzel, D. Bar-Ness, E. Roessler, I. Blevis, M. Bartels, A. A. Fingerle, S. Ruschke, P. Coulon, H. Daerr, F. K. Kopp, B. Brendel, A. Thran, M. Rokni, J. Herzen, L. Bousset, F. Pfeiffer, R. Proksa, E. J. Rummeny, P. Douek, and P. B. Noël. Spectral Photon-Counting CT: Initial Experience with Dual-Contrast Agent K-Edge Colonography. *Radiology* 283, 723-728 (2017).
13. D. Muenzel, H. Daerr, R. Proksa, A. A. Fingerle, F. K. Kopp, P. Douek, J. Herzen, F. Pfeiffer, E. J. Rummeny, and P. B. Noël. Simultaneous Dual-Contrast Multi-Phase Liver Imaging using Spectral Photon-Counting Computed Tomography: a Proof-of-Concept Study. *European Radiology Experimental* 1, 25 (2017).
14. J. Dangelmaier, D. Bar-Ness, H. Daerr, D. Muenzel, S. Si-Mohamed, S. Ehn, A. A. Fingerle, M. A. Kimm, F. K. Kopp, L. Bousset, E. Roessler, F. Pfeiffer, E. J. Rummeny, R. Proksa, P. Douek, and P. B. Noël. Experimental Feasibility of Spectral Photon-Counting Computed Tomography with Two Contrast Agents for the Detection of Endoleaks Following Endovascular Aortic Repair. *European Radiology* 28, 3318-3325 (2018).
15. I. Riederer, D. Bar-Ness, M. A. Kimm, S. Si-Mohamed, P. B. Noël, E. J. Rummeny, P. Douek, and D. Pfeiffer. Liquid Embolic Agents in Spectral X-Ray Photon-Counting Computed Tomography using Tantalum K-Edge Imaging. *Scientific Reports* 9, 5268 (2019).
16. T. C. Soesbe, M. A. Lewis, K. Nasr, L. Ananthakrishnan, and R. E. Lenkinski. Separating High-Z Oral Contrast from Intravascular Iodine Contrast in an Animal Model using Dual-Layer Spectral CT. *Academic Radiology* 26, 1237-1244 (2019).
17. L. Ren, K. Rajendran, J. G. Fletcher, C. H. McCollough, and L. Yu. Simultaneous Dual-Contrast Imaging of Small Bowel with Iodine and Bismuth using Photon-Counting-Detector Computed Tomography: a Feasibility Animal Study. *Investigative Radiology* 55, 688-694 (2020).
18. ... many many more since 2020 ...

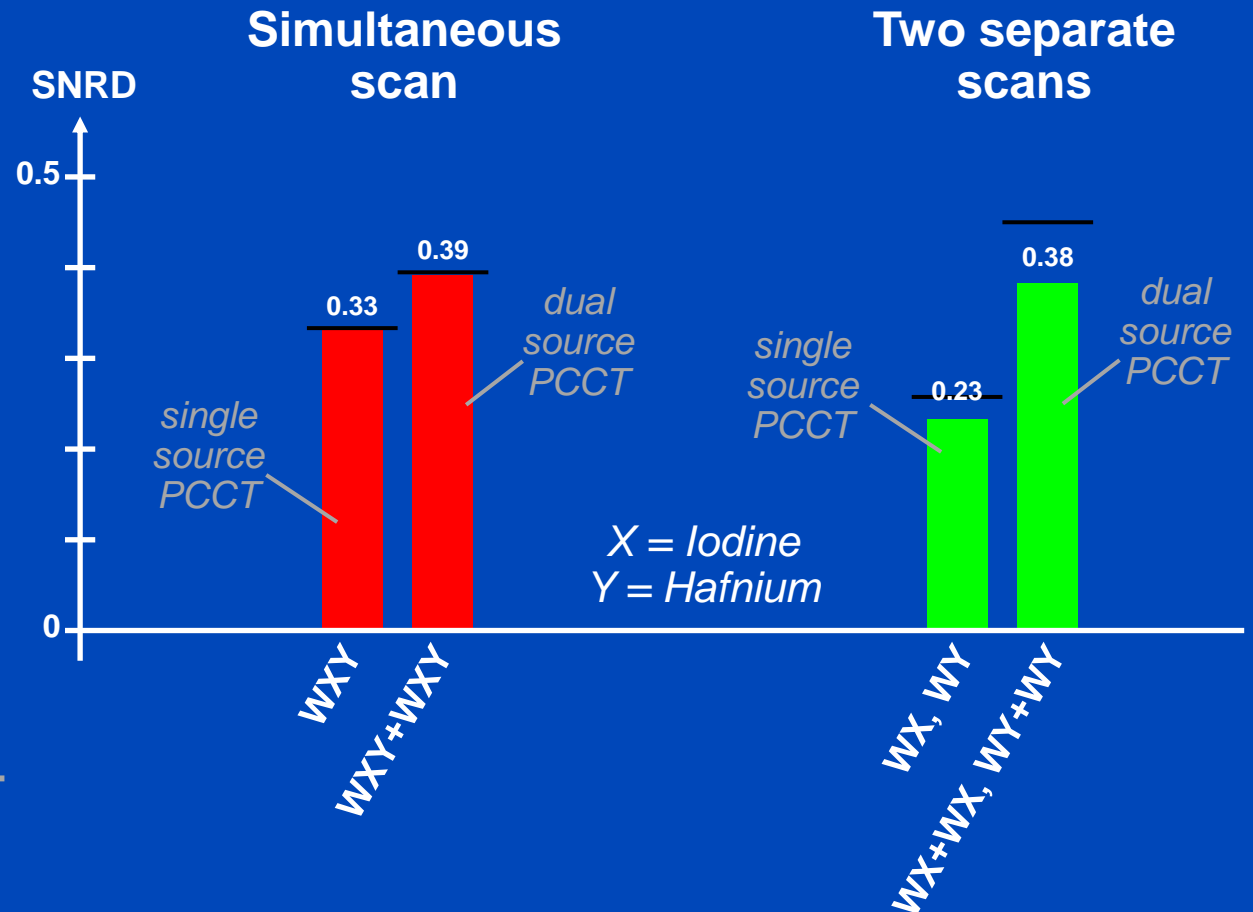
Two Contrast Agents X and Y in the Same Region

- Must have $X \neq Y$ if scanned simultaneously.
- Can have $X = Y$ if scanned separately.
- Separate scans require less dose!
- Good old liver protocols are optimal:
 - $X = Y = \text{iodine (today)}$
 - Two separate scans
 - Only one CA injection required
 - Unenhanced scan not necessary with PCCT



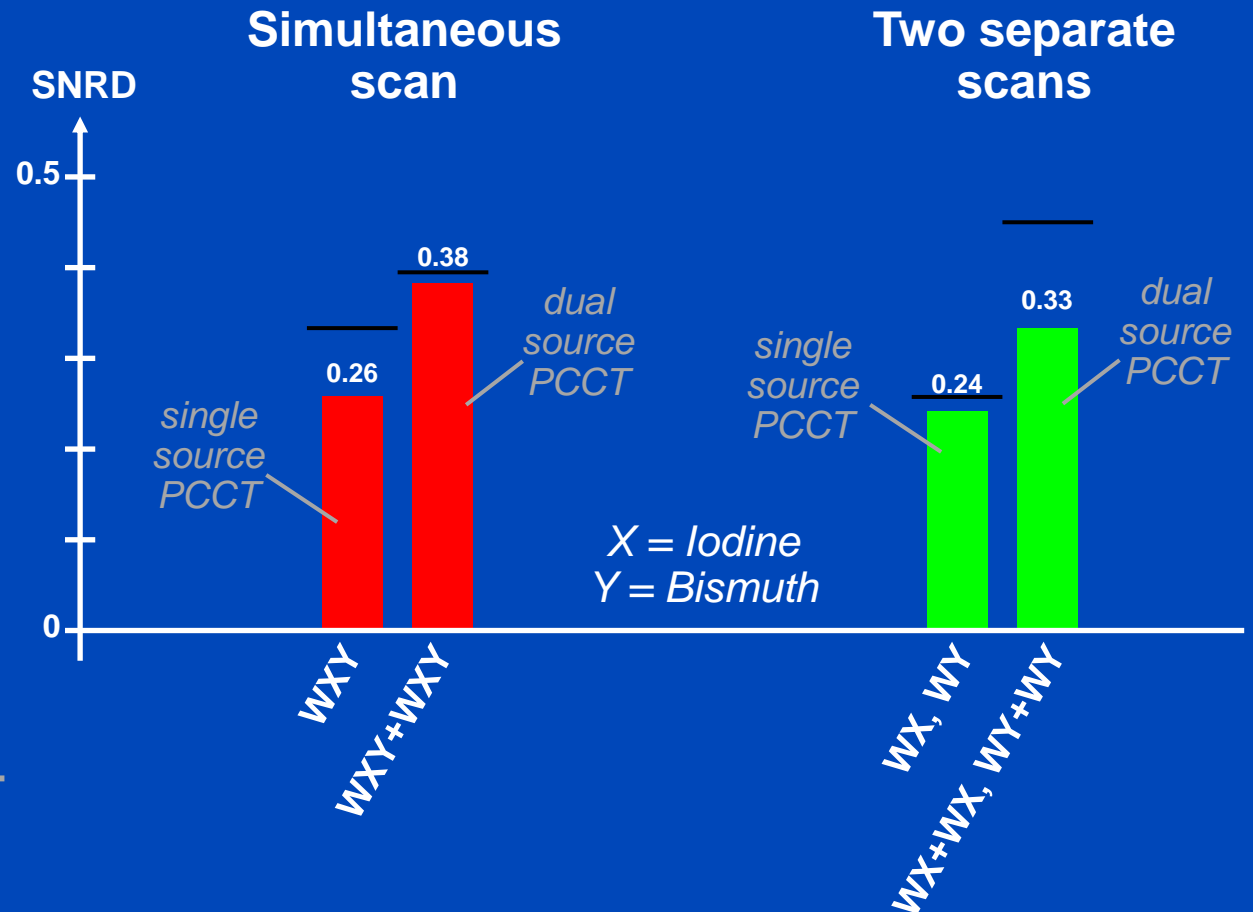
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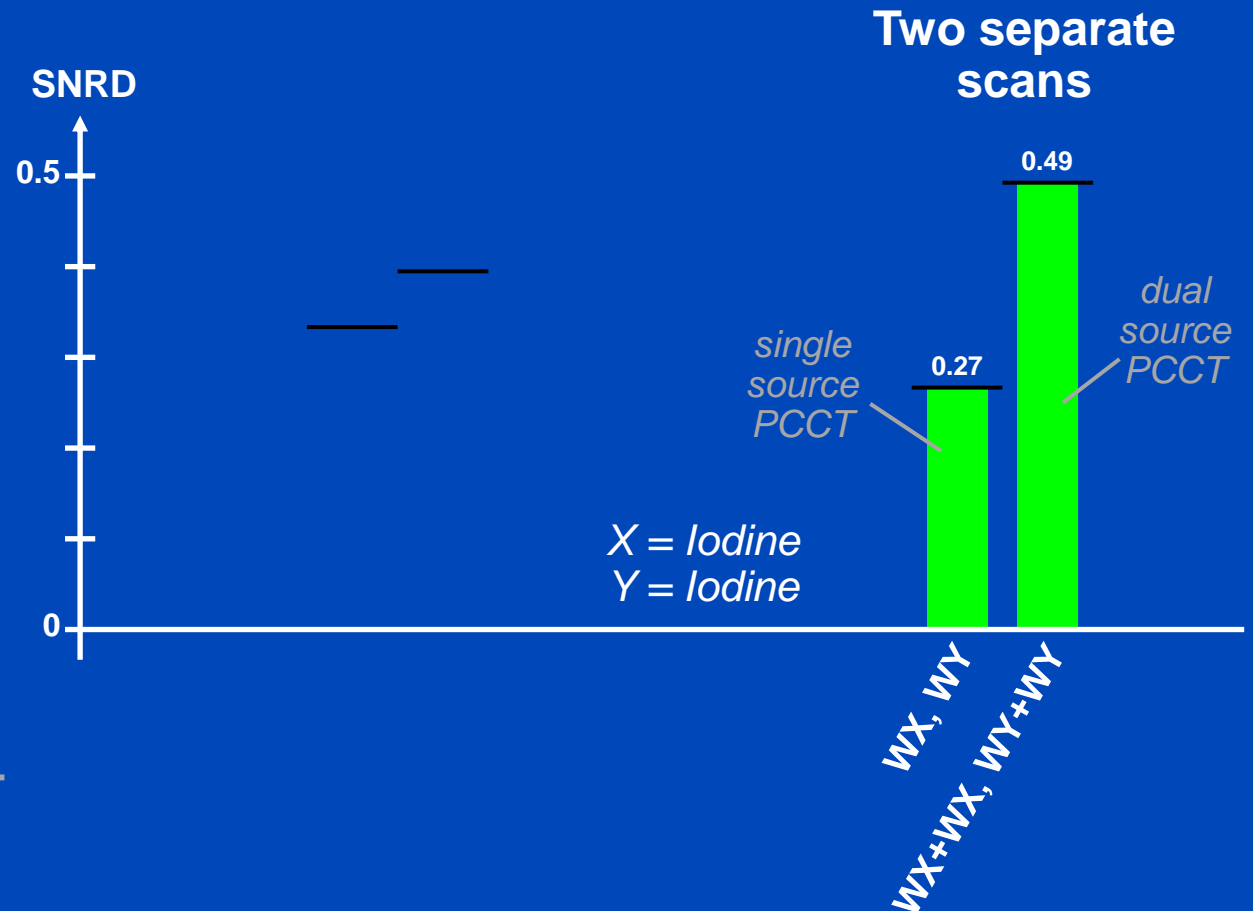
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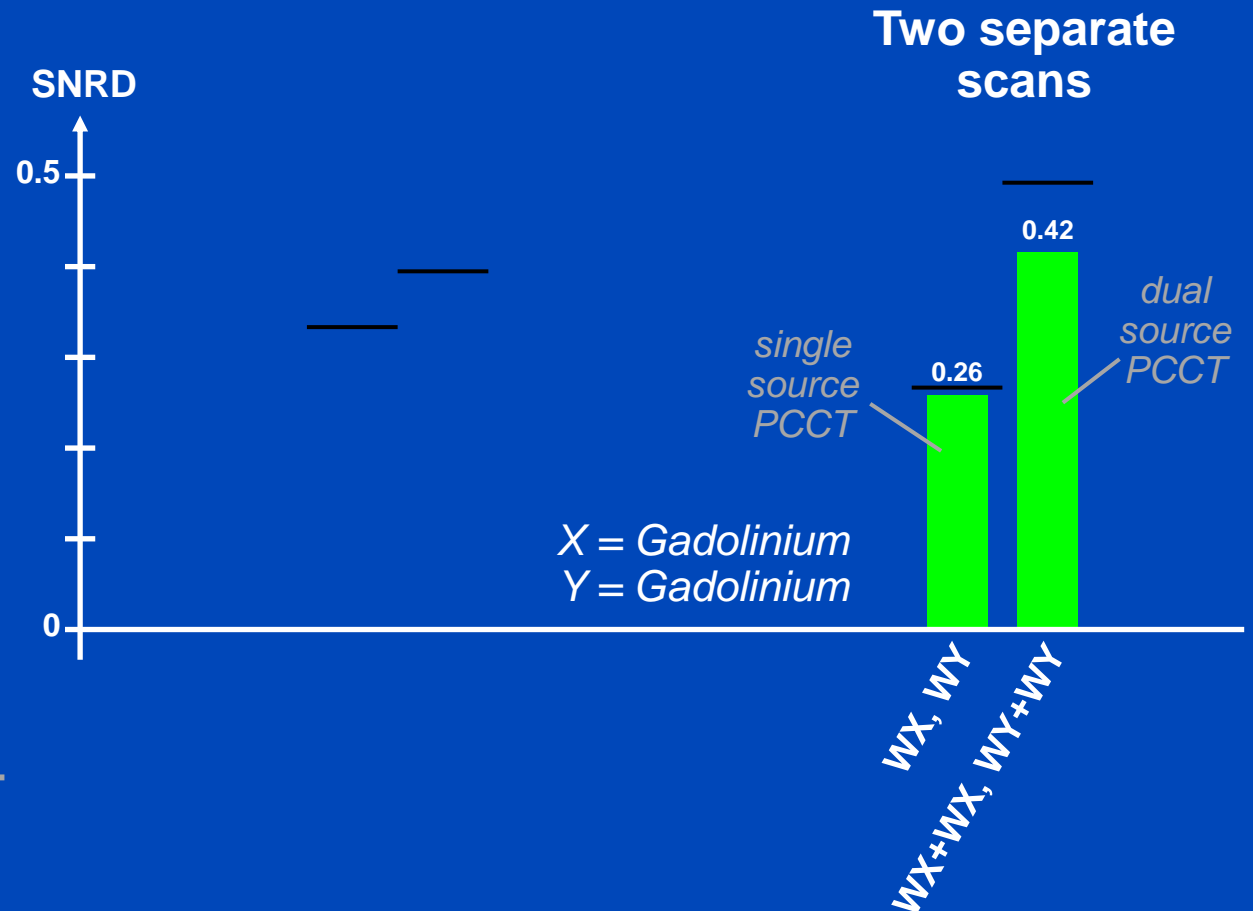
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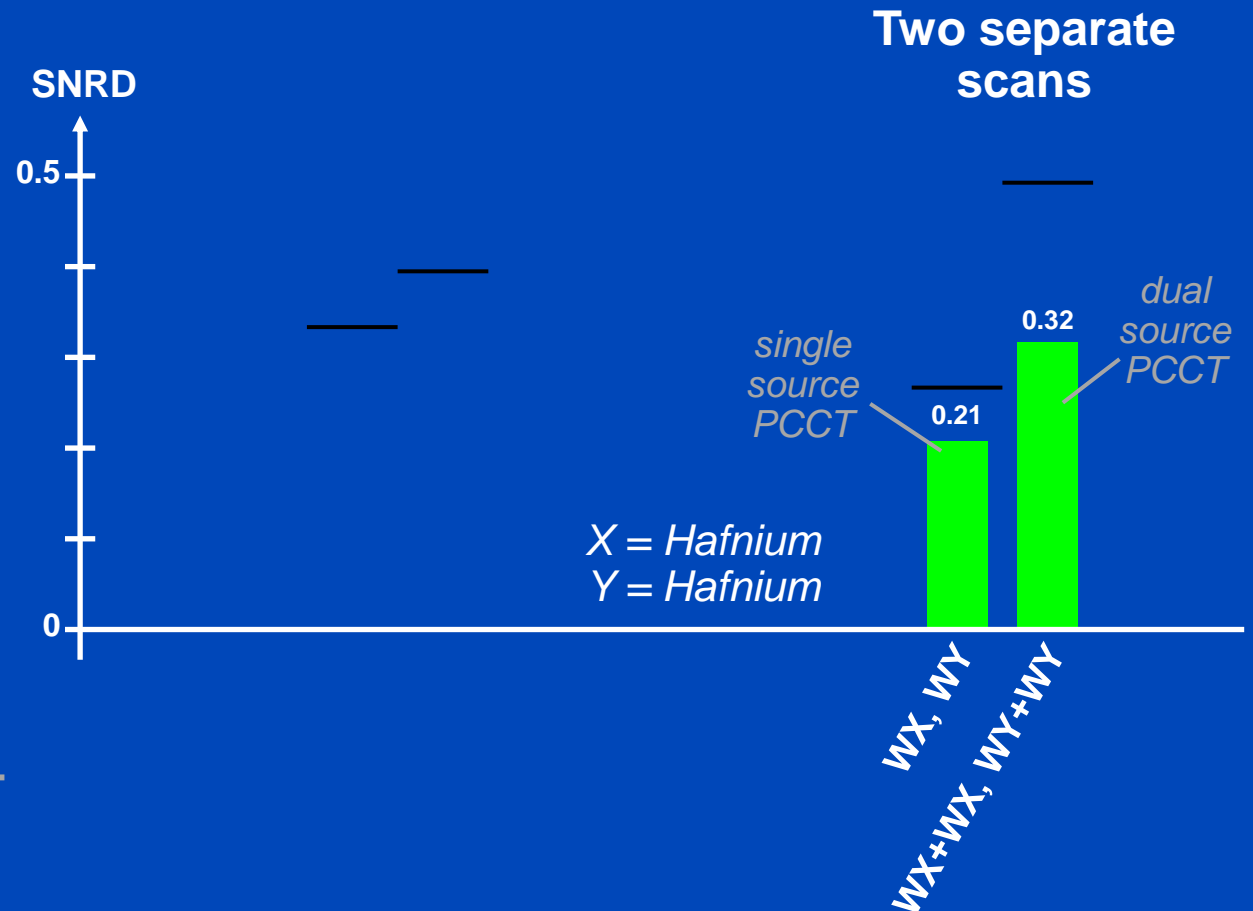
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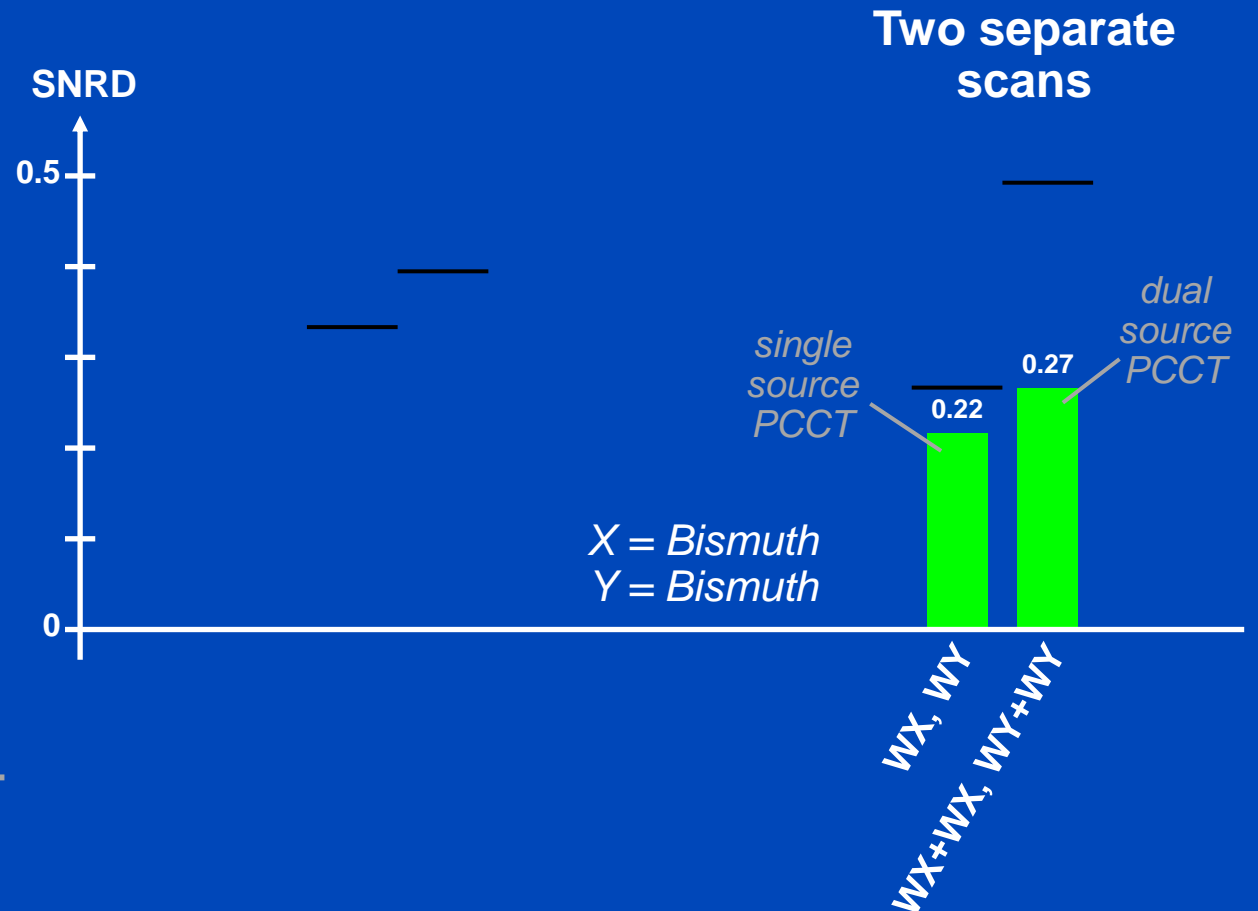
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Two Contrast Agents X and Y in Different Regions

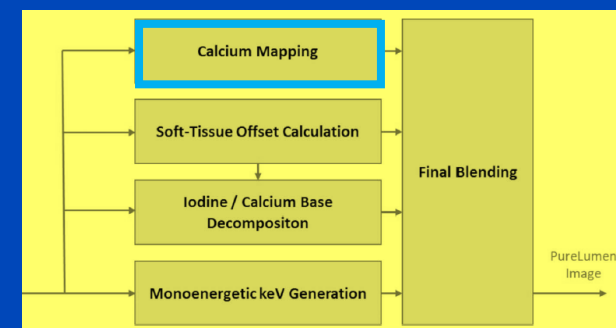
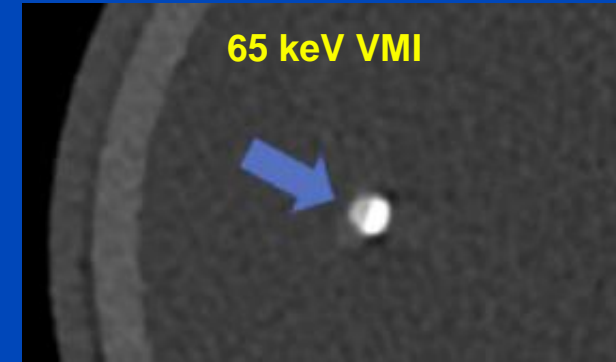
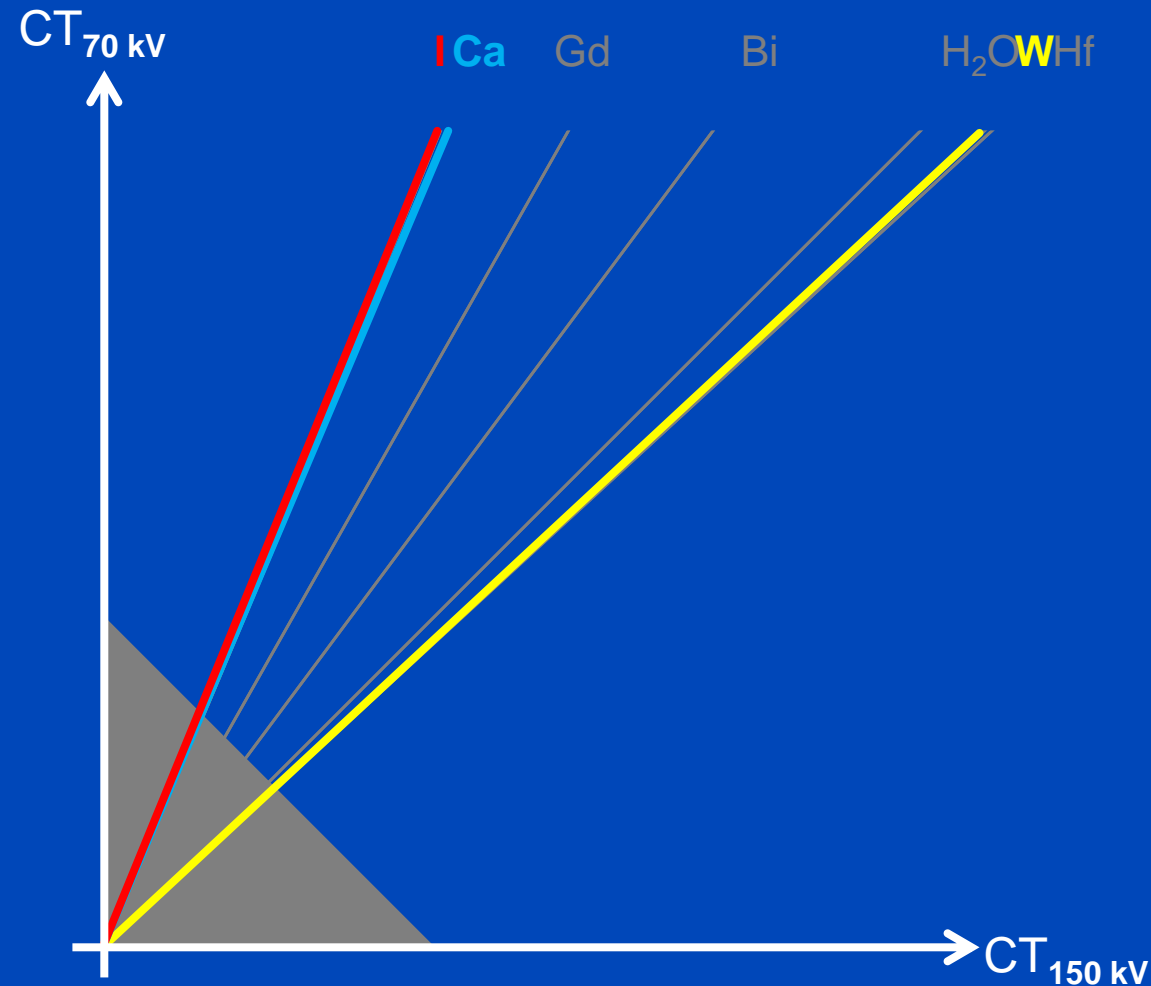
- That's trivial, it's different regions
- Any reason for not using $X=Y$?

Is Iodine Good (or even God)?

- PCCT simulation with tube voltage, prefilter and energy threshold position optimization and optimized linear reconstruction¹.
- CAs diluted to have 200 HU in the center of a 32 cm water phantom when scanned at 120 kV spectrum with only intrinsic filtration.
- Patient sizes 20 cm, 30 cm, 40 cm.
- Scan parameters maximizing SNRD of W and X yield:

200 mm, $B = 3$, real	X=Iodine SNRDs of W, X, tot	X=Gadolinium SNRDs of W, X, tot	X=Hafnium SNRDs of W, X, tot	X=Bismuth SNRDs of W, X, tot
WX	14.7, 3.16, 3.39	12.4, 2.55, 2.74	10.1, 2.30, 2.47	9.91, 2.33, 2.51
WX+WX	21.5, 6.08, 6.45	17.6, 3.89, 4.17	13.2, 2.87, 3.08	17.1, 4.05, 4.35
400 mm, $B = 3$, real	X=Iodine SNRDs of W, X, tot	X=Gadolinium SNRDs of W, X, tot	X=Hafnium SNRDs of W, X, tot	X=Bismuth SNRDs of W, X, tot
WX	2.28, 0.38, 0.41	2.03, 0.36, 0.39	1.62, 0.29, 0.31	1.63, 0.31, 0.34
WX+WX	3.12, 0.69, 0.74	3.00, 0.60, 0.64	2.02, 0.45, 0.48	1.93, 0.38, 0.40

What if We Want to Discriminate Ca from CA?

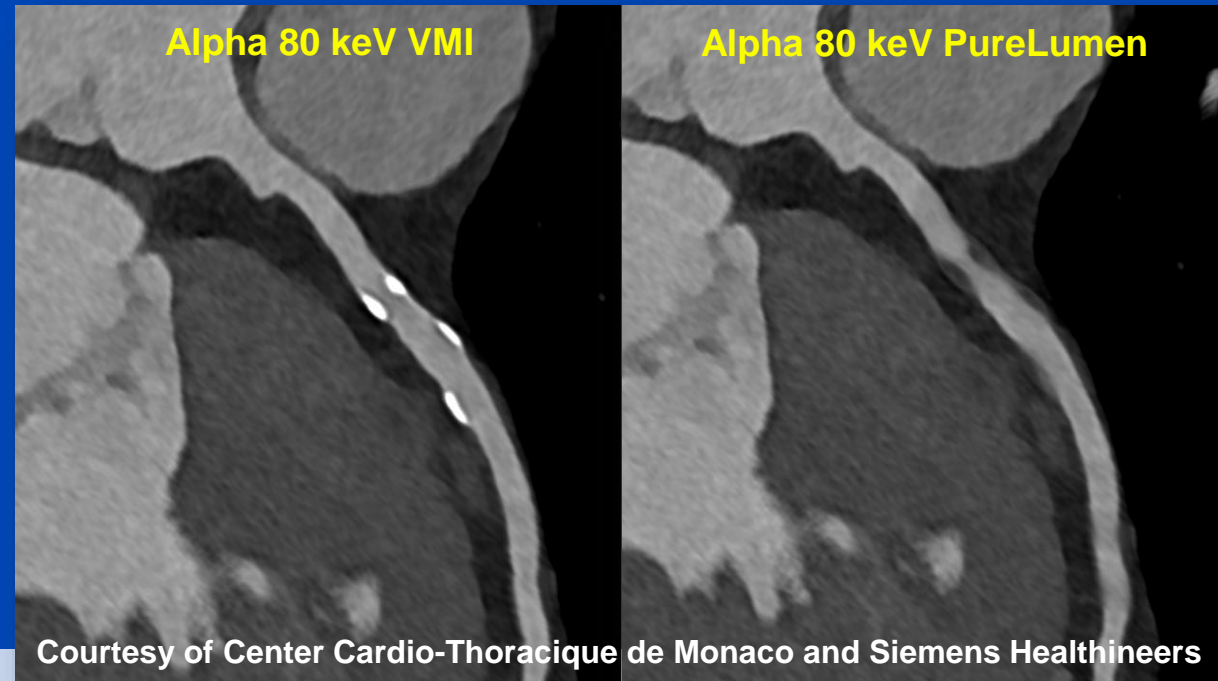


Allmendinger et al., Invest Radiol 57(6), 2022

In the energy range of clinical CT and with objects similar to patients we find that 0.5 mm Ag \approx 0.6 mm Sn \approx 2.0 mm Cu.

Conclusions

- Dual contrast may not make sense. Scan separately and save dose.
- Iodine is great!
- Higher Z may help to better discriminate Ca from CA.
 - In particular a tungsten CA ($Z = 74$) seems good to tell Ca from CA.
 - However, tungsten is not easy to discriminate from soft tissue by spectral means.
 - This means, potential tungsten maps will be of low quality. Adding prior knowledge may help.
 - Special application in coronary arteries?
 - Tungsten could be mixed with iodine!
- It is iodine forever!
- Maybe it will have a little sister.



Thank You!

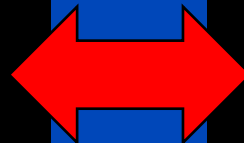
- This presentation will soon be available at www.dkfz.de/ct.
- Job opportunities through marc.kachelriess@dkfz.de or through DKFZ's PhD program.
- Parts of the reconstruction software were provided by RayConStruct® GmbH, Nürnberg, Germany.

EuroSafe Imaging Session EU 13

Assessment of
AI-based image reconstruction

Friday, 9:30 to 11:00

Room M1



Low dose CT benchmark:



github.com/eeulig/ldct-benchmark

E. Eulig, B. Ommer, and M. Kachelrieß. Benchmarking deep learning-based low-dose CT image denoising algorithms. *Med. Phys.* 51(12):8776-8788, December 2024.

Thank You!



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