

# Synthesizing 4D CBCT Scans from 3D CBCT Phantom Acquisitions

Markus Susenburger<sup>1,2</sup>, Julien Erath<sup>1,2,4</sup>, Pascal Paysan<sup>3</sup>,  
Ricky Salvani<sup>3</sup>, Gernot Echner<sup>1</sup>, and Marc Kachelrieß<sup>1,2</sup>

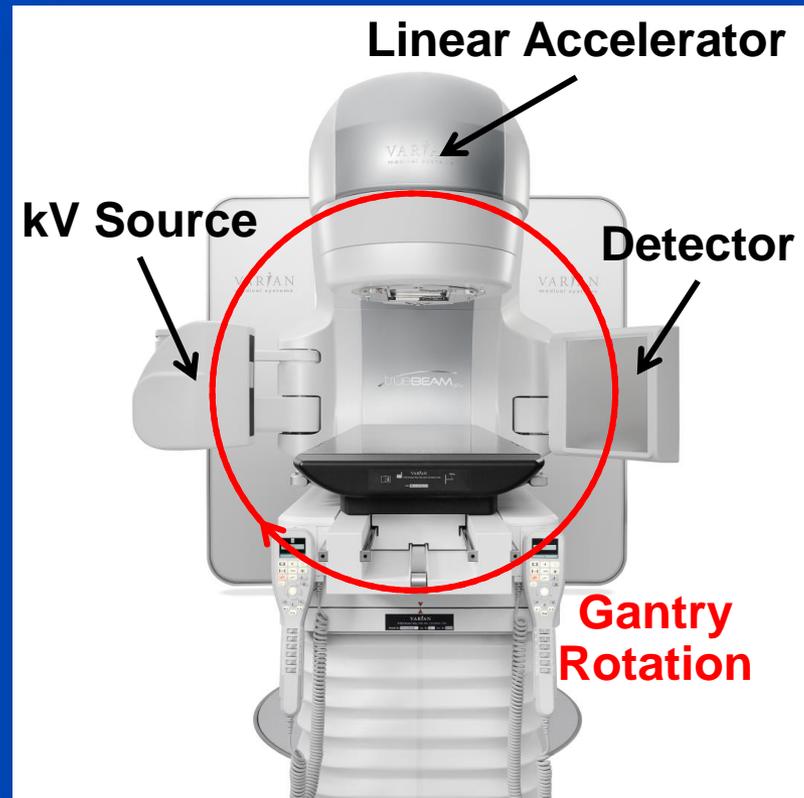
<sup>1</sup>German Cancer Research Center (DKFZ), Heidelberg, Germany

<sup>2</sup>Heidelberg University, Germany

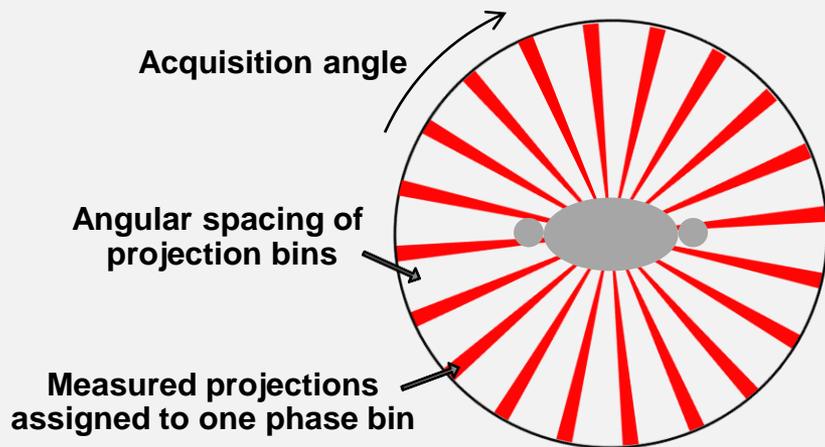
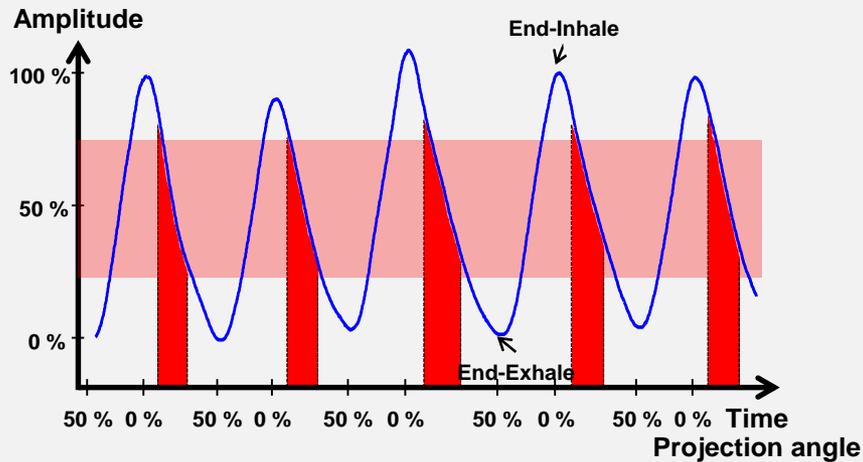
<sup>3</sup>Varian Medical Systems, Dättwil, Switzerland

<sup>4</sup>Siemens Healthineers, Forchheim, Germany

# Cone-Beam CT (CBCT) in Image Guided Radiotherapy



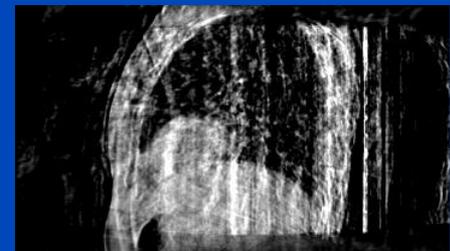
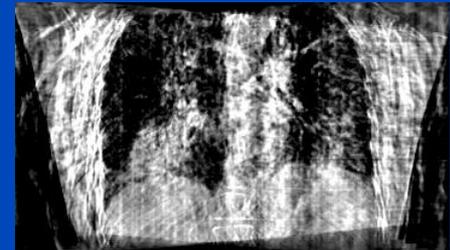
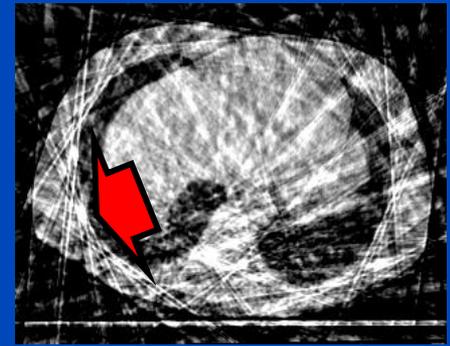
# 4D CBCT Scan with Retrospective Gating



Without gating (3D):  
Motion artifacts



With gating (4D):  
Sparse-view artifacts



# Motivation & Aim

- **Motivation: Ground truth in 4D CBCT is hard to get due to the high patient dose involved for artifact-free images.**
- **Comparing 4D CBCT reconstructions algorithms without a ground truth is cumbersome.**
- **A measured ground truth is of advantage to compare different scanners or tumor positions.**
- **Aim: Provide patient-realistic 4D CBCT ground truth without artifacts.**

# Materials

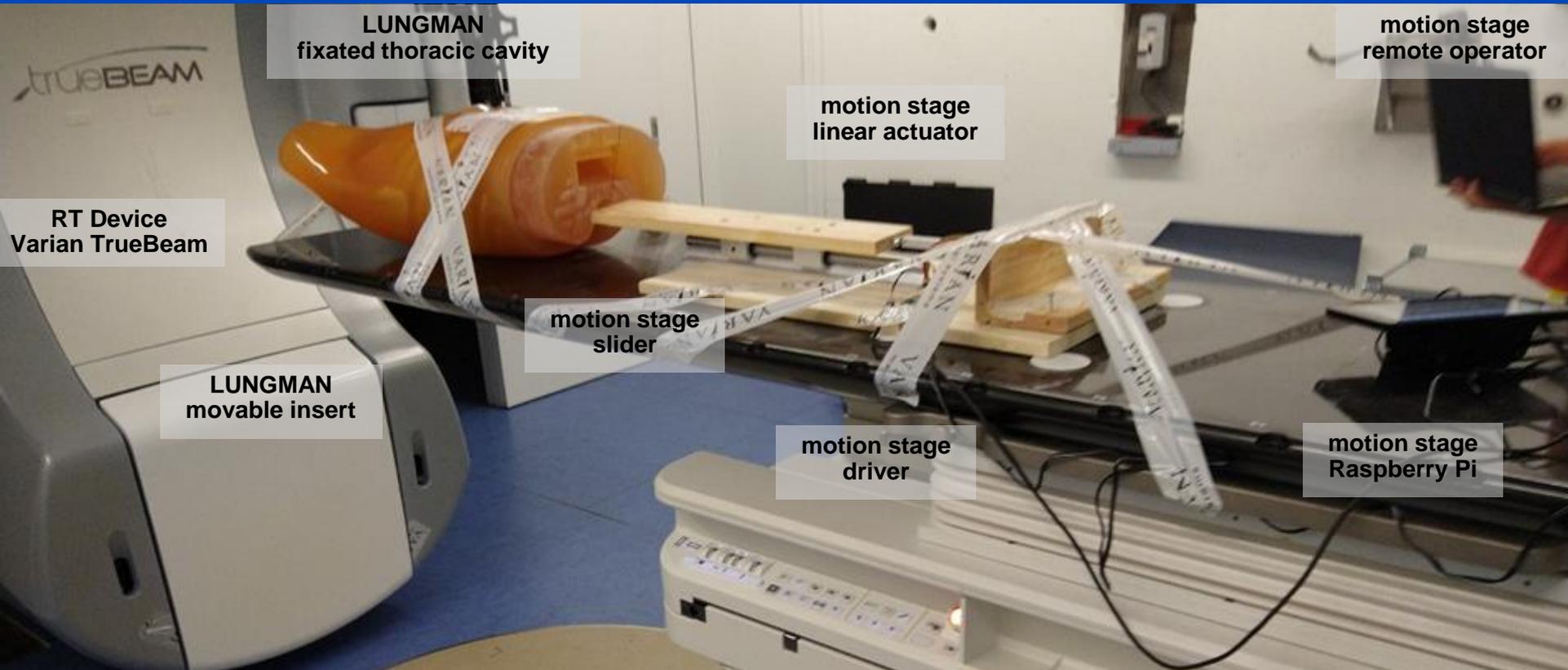
- Perform several consecutive scans with a LUNGMAN phantom at different penetration depths of the abdomen/lung block.
- 51 stop-motion measurements every 1 mm for 50 mm.
- Tube voltages 100 kV & 125 kV



..... field of measurement

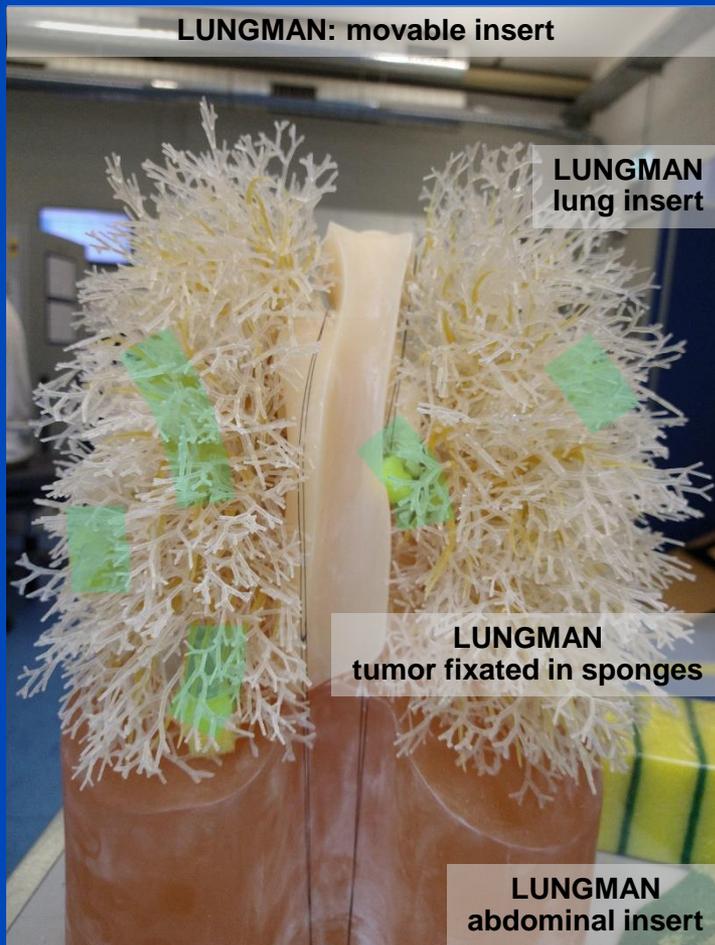
..... MoCo reconstruction

# Experimental Setup



- **LUNGMAN** outer cavity fixated on patient's couch
- Penetration depths of **LUNGMAN** inner cavity can be controlled with a linear actuator on a simple motion stage, controllable from the control room. During the scan, the phantom is not moving.

# LUNGMAN Inner Cavity Setup



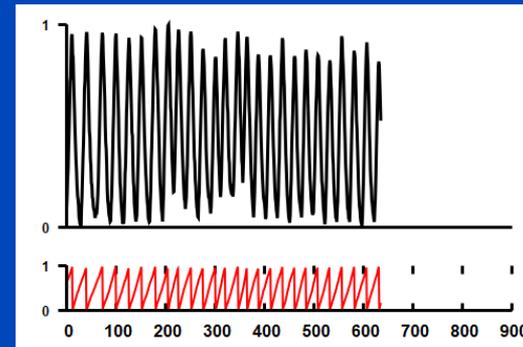
- LUNGMAN inner cavity consisting of abdomen and lung insert.
- 3D printed tumors from the LIDC-IDRI dataset provide realistic tumor shapes.
- Gold markers inserted for a metal artifact study.

# 4D CBCT Synthesizing Method

- We start with a real (or a simulated) amplitude signal from a CBCT acquisition.

relative amplitude signal

| phase signal



- For each projection angle, we find the amplitude of the respiration and correlate it to the measured 3D scans.
- From that given scan, we select the projection closest to the projection angle.
- Repeat this for all projections in the original signal.

# Reconstruction Methods

- The reconstruction size is  $512 \times 512 \times 210$  voxel at  $1 \times 1 \times 1$  mm<sup>3</sup>.
- The 3D images are reconstructed with FDK<sup>1</sup>.
- The 4D images are gated according to their phase signal and the respiration bins are reconstructed with FDK, 20 overlapping phases of 10% phase width.
- The motion-compensated images are reconstructed by two MoCo algorithms: acMoCo<sup>2,3</sup> and acacMoCo<sup>4</sup>.

<sup>1</sup> L. Feldkamp, L. Davis und J. Kress, „Practical Cone–Beam Algorithm,“ Journal of the Optical Society of America, 1(6), 1984.

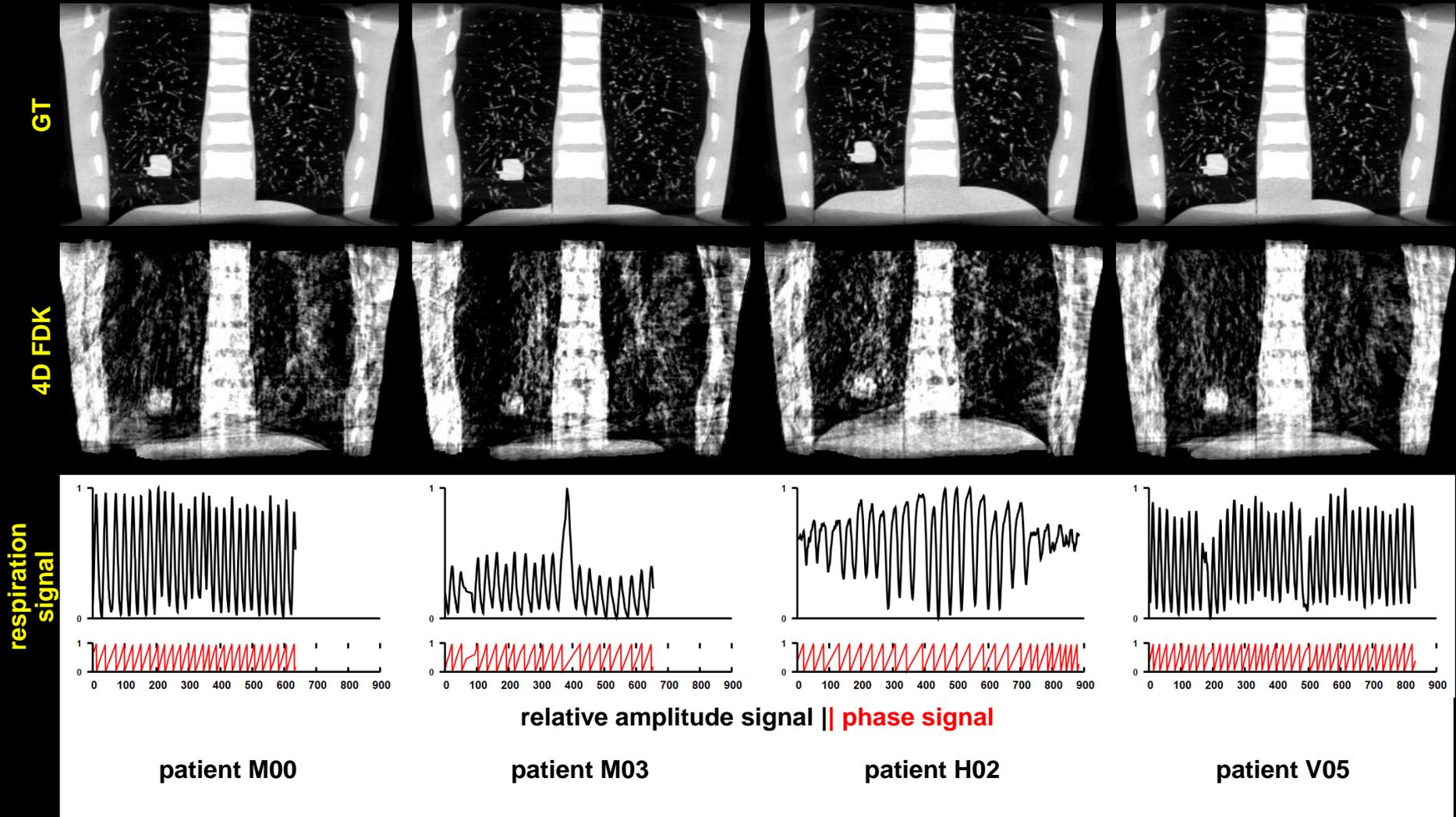
<sup>2</sup> M. Brehm, and M. Kachelrieß, „Self–Adapting Cyclic Registration for Motion–Compensated Cone–Beam CT in Image–Guided Radiation Therapy,“ Med. Phys., 39(12), 2012.

<sup>3</sup> M. Brehm and M. Kachelrieß, „Artifact–Resistant Motion Estimation with a Patient–Specific Artifact Model for Motion–Compensated Cone–Beam CT,“ Med. Phys., 40(10), 2013.

<sup>4</sup> M. Susenburger and M. Kachelrieß, „4D–Segmentation–Based Anatomy–Constrained Motion–Compensated Reconstruction of On–Board 4D CBCT Scans,“ CT Meeting 2020.

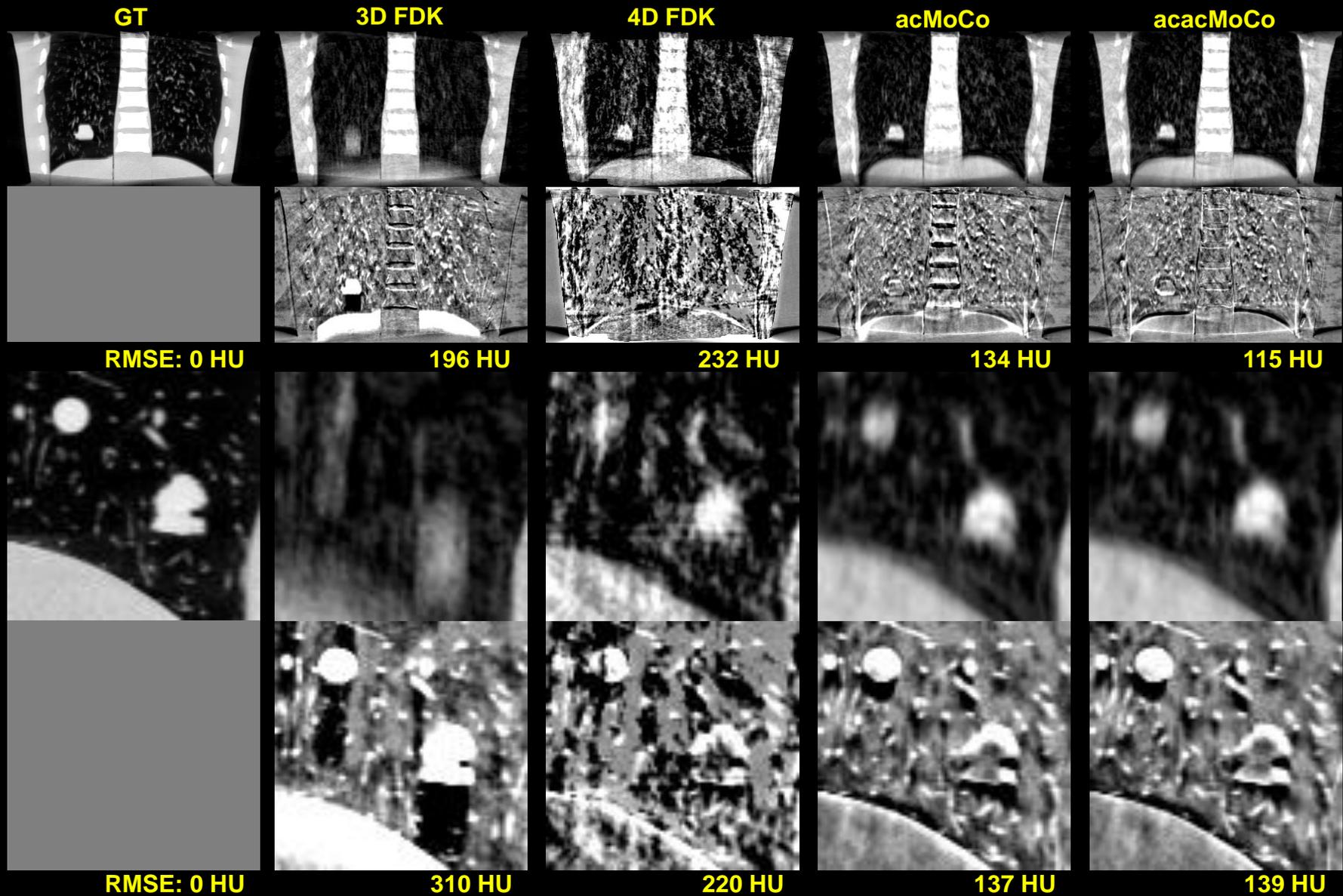
# 4D CBCT Synthesis

## Different Patient Respiration Signals



Images:  $C = -250$  HU,  $W = 1400$  HU

# Tumor Shape Recovery



Images:  $C = -250$  HU  $W = 1400$  HU

Differences:  $C = 0$  HU  $W = 600$  HU

# Conclusions & Limitations

- 4D CBCT synthesis from consecutive 3D scans is suitable for the comparison of 4D reconstruction algorithms.
- The LUNGMAN anatomy is restricted to one specific phantom.
- Motion can only be analyzed in superior-inferior direction.
- Further, the setup is suitable for different scanners and the results can easily be repeated.
- The LUNGMAN phantom as such is often available in many clinics.

# Thank You!

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