

RIDL: Row Interpolation with Deep Learning

Fully3D 2021 – Leuven, 22.07.2021

Jan Magonov^{1,2,3}, Marc Kachelrieß¹, Eric Fournié², Karl Stierstorfer², Thorsten Buzug³ and Maik Stille³

¹Division of X-Ray Imaging and CT, German Cancer Research Center (DKFZ), Heidelberg, Germany

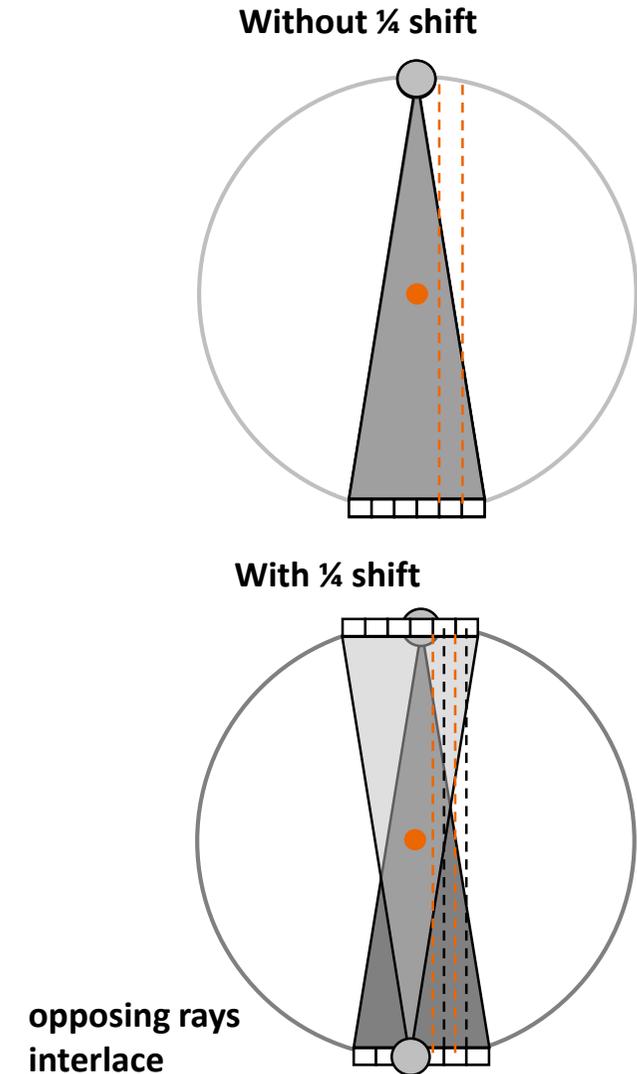
²Siemens Healthcare GmbH, Forchheim, Germany

³Institute of Medical Engineering, University of Lübeck, Lübeck, Germany



Motivation:

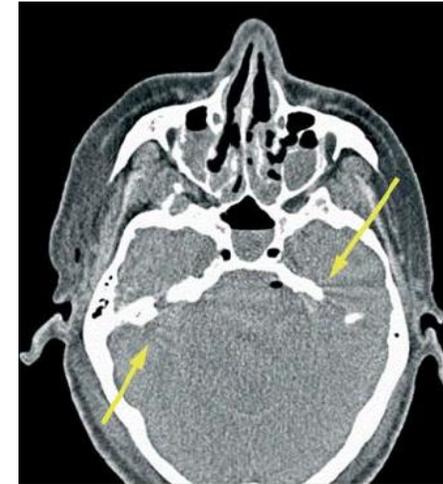
- Correct sampling needs to fulfill the Nyquist theorem: at least two sample points should be recorded per FWHM of the detector point spread function (PSF).
- Requiring at least **two samples per detector pixel**
- This condition is not given in real CT setup, as the spacing of detector sample centers is slightly larger than the active width of the detector pixels.
- Quarter detector offset (QDO) is used to fulfill the Nyquist theorem by mounting the detector array shifted by one quarter of detector sampling distance in x-y-plane.



Motivation:

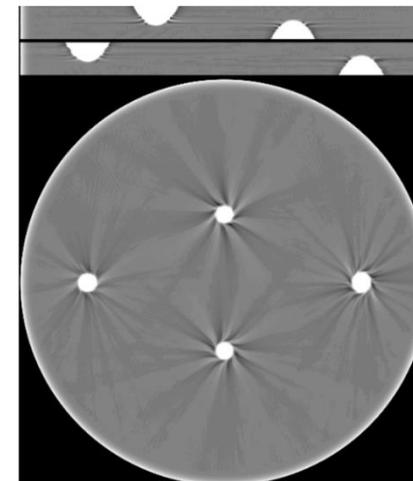
Spiral CT and Windmill Artifacts

- During backprojection in multislice spiral CT, an interpolation is performed between adjacent detector rows.
- Inadequate longitudinal sampling leads to so-called windmill artifacts .
- Characterized by streaks diverging from a focal high-density structure.
- Streaks appear to rotate while scrolling through the affected slices.

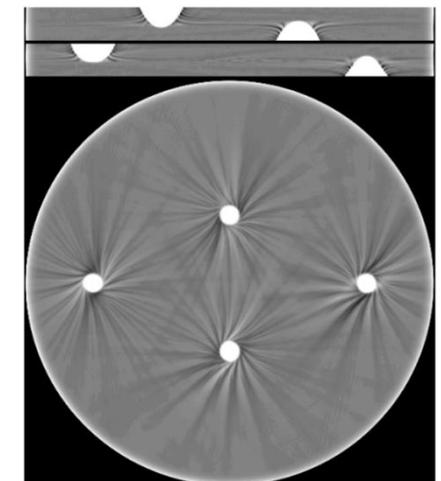


1

Pitch: 0.5



Pitch: 1.0



Motivation: Spiral CT and Windmill Artifacts

Without zFFS

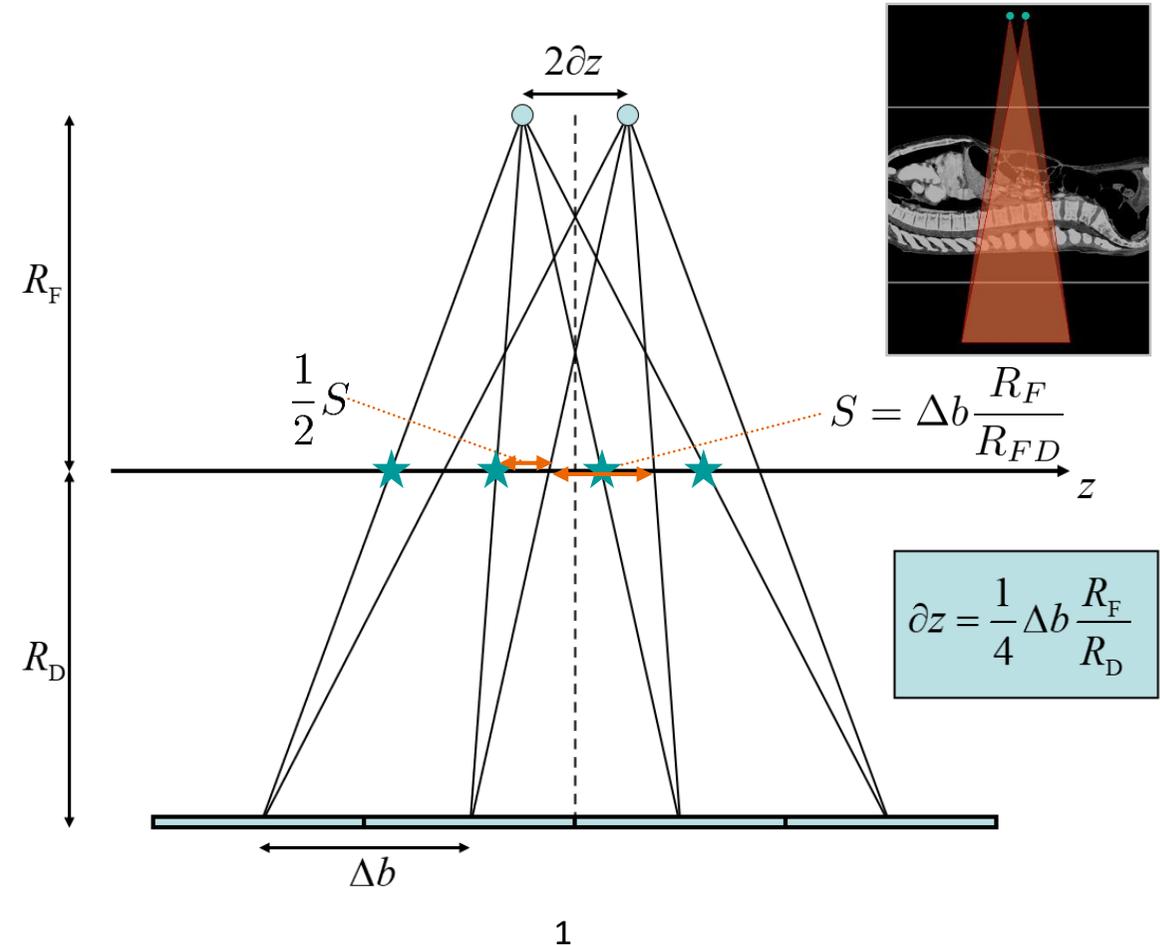
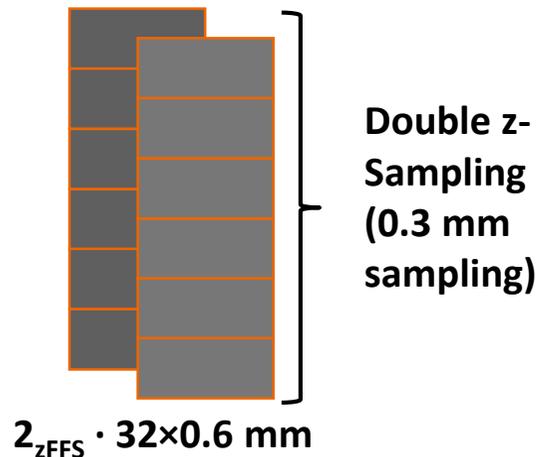


With zFFS



Motivation: Z-Flying Focal Spot (zFFS)

- Z-flying focal spot (zFFS) uses a periodic motion of the focal spot in longitudinal direction.
- Two subsequent readings are slightly shifted in z-direction to achieve a doubled sampling distance in the iso-center.



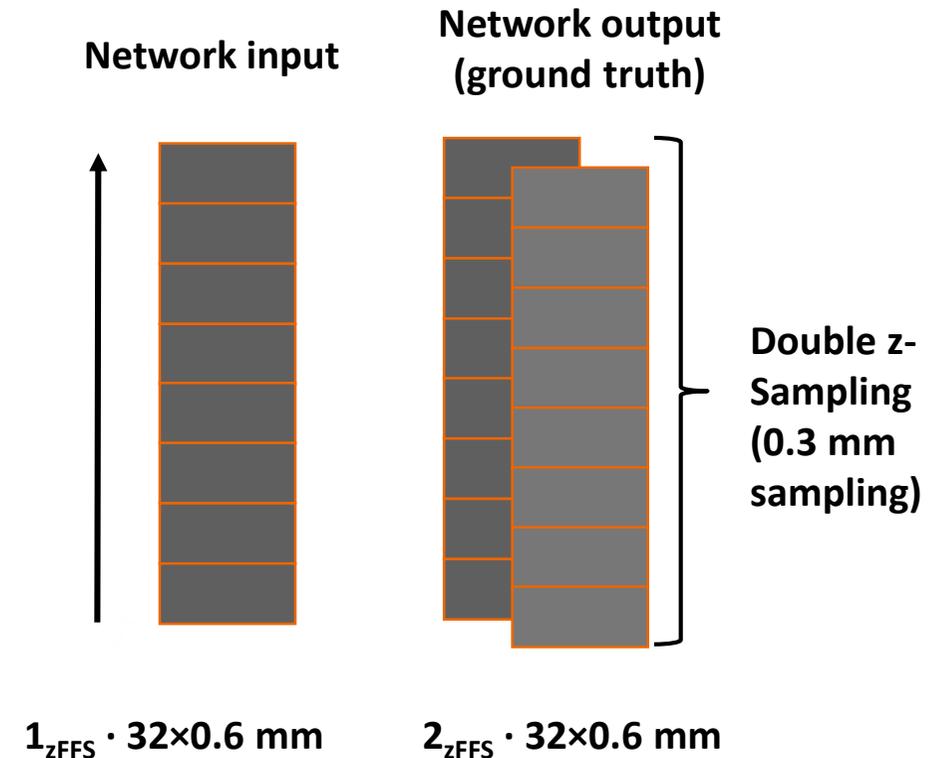
Disadvantages of zFFS:

- High technical effort and therefore expensive.
- No application in CT systems that lack the technical requirements.
- More readings required, which may prevent switching in the fastest scan mode.

- Is a neural network able to interpolate between detector rows in z-direction to achieve a higher sampling?
- Is this approach able to outperform a linear interpolation of the detector rows?

Methods

- Train a neural network that learns to generate interpolated rows by supervised learning.
- Divide projection data (detector readouts) in alternative rows.
- Every second row of a certain projection is used as network input .
- Projection image containing all zFFS-generated rows is set as network ground truth.

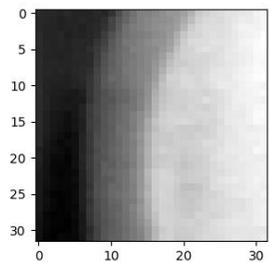


Data Preparation: Training and Testing Data

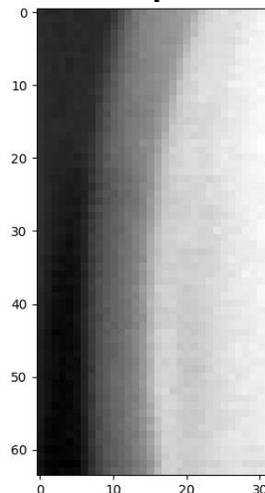


Selecting random
patches

Network input

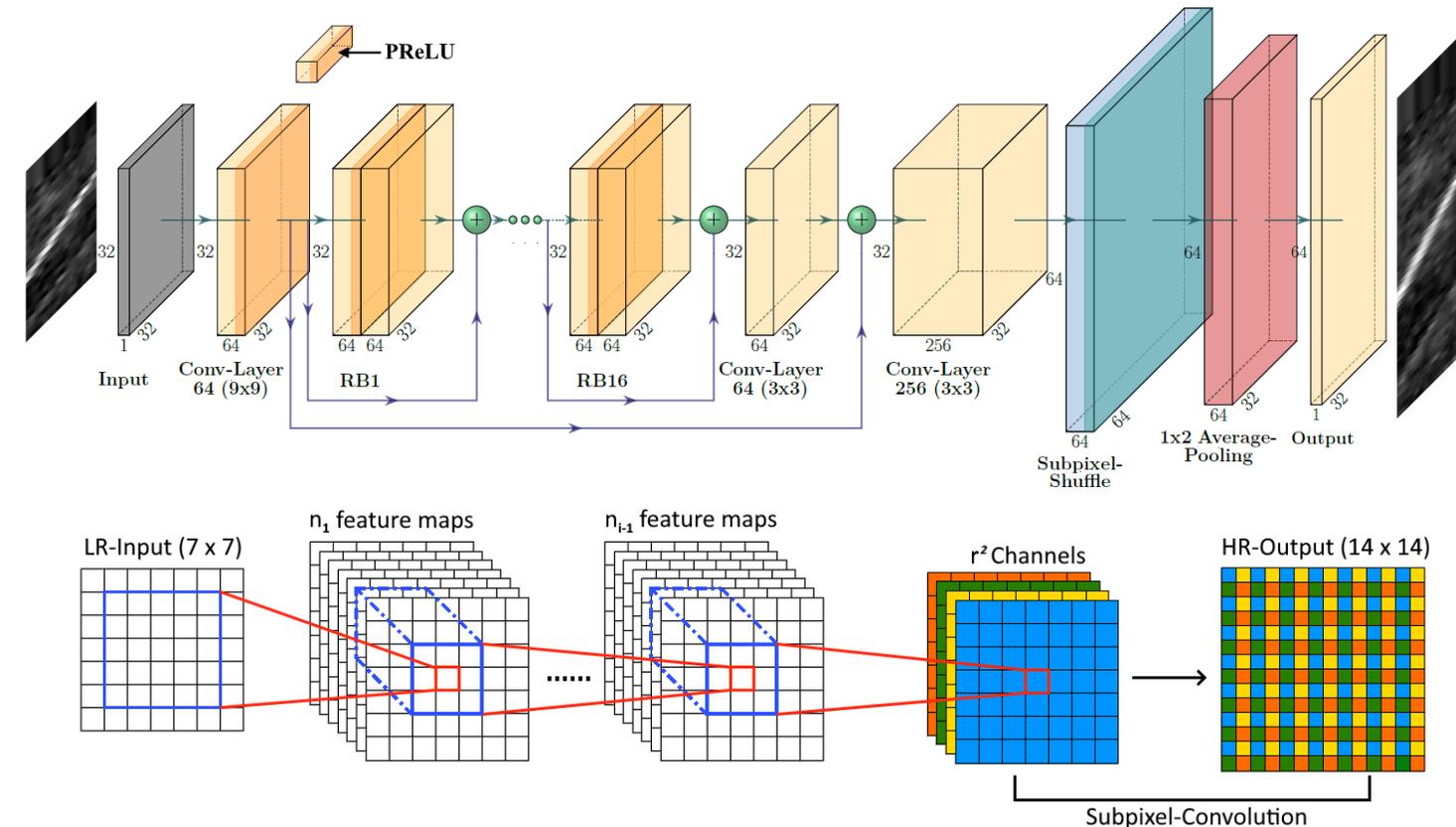


Ground truth &
desired network
output



- 29 clinical CT scans of different body regions from various Siemens CT systems (0.6 mm slice thickness)
- Split into two disjoint subsets: training (23 scans) and testing data (6 scans)
- Projection data acquisition after the rebinning
- Selecting random projection data patches (64×32) and globally normalize value range to [0,1]

Network Architecture: RIDL-SRResNet



2

- Network application in the field of super-resolution (Ledig et al.¹)
- 64×32 patches
- Input: 32×32, Output: 64×32
- 1,377,921 trainable parameters
- Upscaling of the input image LR feature maps by using a subpixel convolution (Shi et al.²)

1: C. Ledig, L. Theis, F. Huszár, et al. “Photo-Realistic Single Image Super-Resolution Using a Generative Adversarial Network”. In: Computer Vision and Pattern Recognition, July 2017, PP. 105–114.

2: W. Shi, J. Caballero, F. Huszár, et al. “Real-Time Single Image and Video Super-Resolution Using an Efficient Sub-Pixel Convolutional Neural Network”. In: 2016 IEEE Conference on Computer Vision and Pattern Recognition (CVPR). 2016, PP. 1874–1883

- Training: 500,000 pairs of patches from training data
- Testing: 125,000 pairs from testing data
- ADAM optimizer; initial learning rate: 1×10^{-5} ; halved once the validation error could not be minimized after 25 epochs; early-stopping regularization after 100 epochs

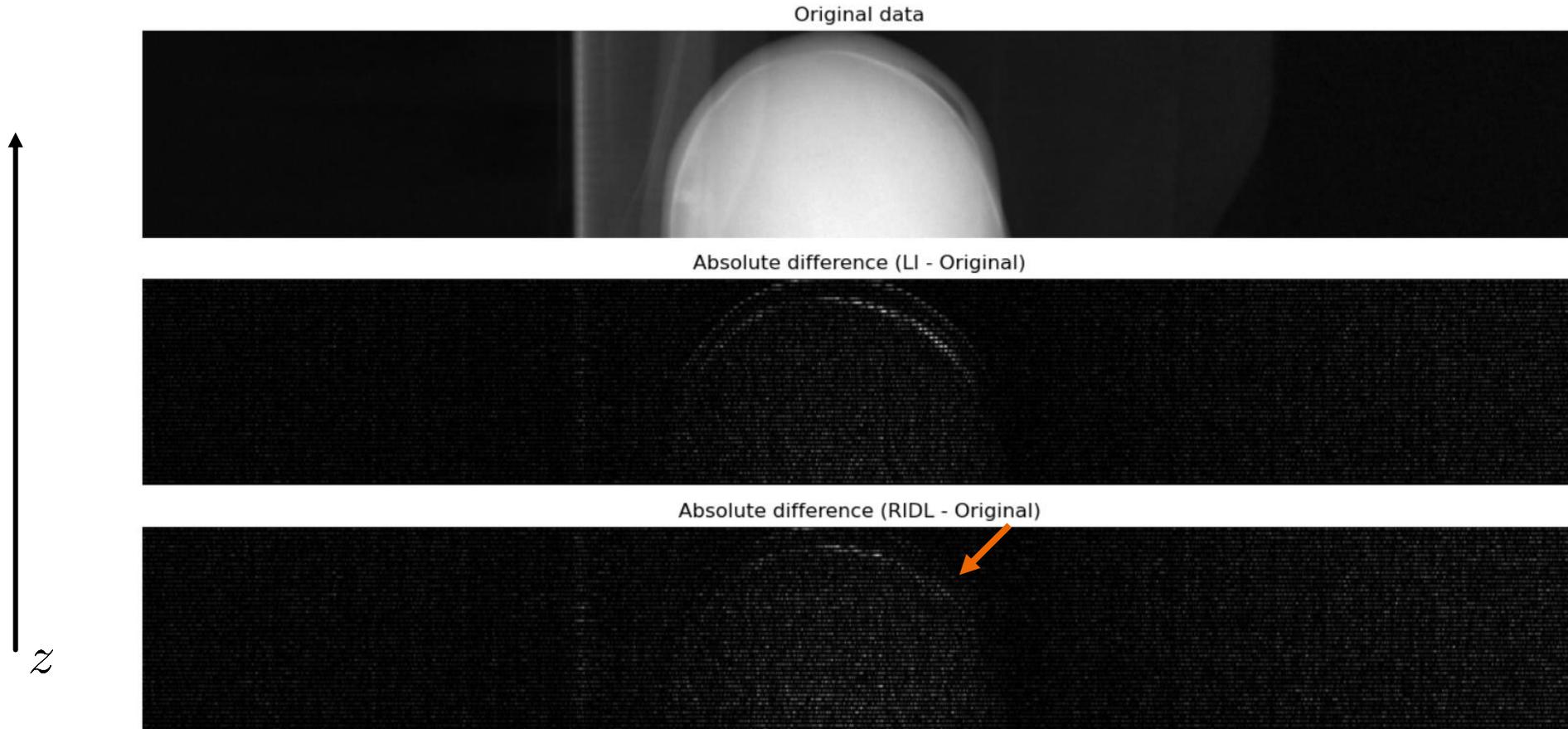
- Loss function proposed in¹:

$$L_{\text{comb}}(y, \hat{y}) = \alpha \cdot (1 - L_{\text{MS-SSIM}}(y, \hat{y})) + (1 - \alpha) \cdot L_{\text{MAE}}(y, \hat{y})$$

- $\alpha = 0.84$, empirically determined

Results

Results in Projection Domain



| ID | Loss function | $MSE(y, \hat{y})$ | $\overline{MSE}(y, \hat{y})$ |
|-------------|---------------|---|---|
| LI | - | $2.352 \cdot 10^{-4}$ | $6.306 \cdot 10^{-4} \pm 5.310 \cdot 10^{-4}$ |
| RIDL | L_{comb} | $1.976 \cdot 10^{-4}$ | $5.626 \cdot 10^{-4} \pm 4.718 \cdot 10^{-4}$ |

Results in Image Domain

Ground truth with zFFS



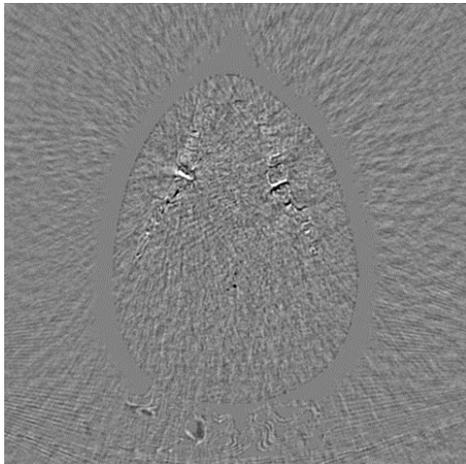
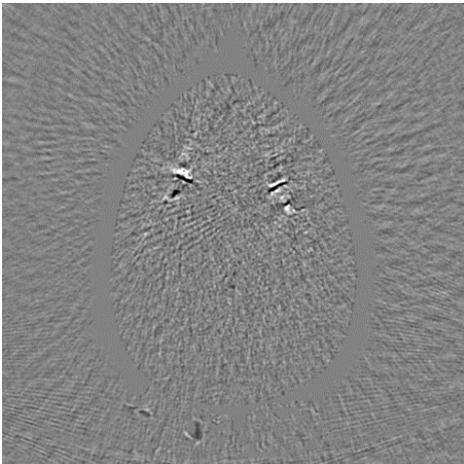
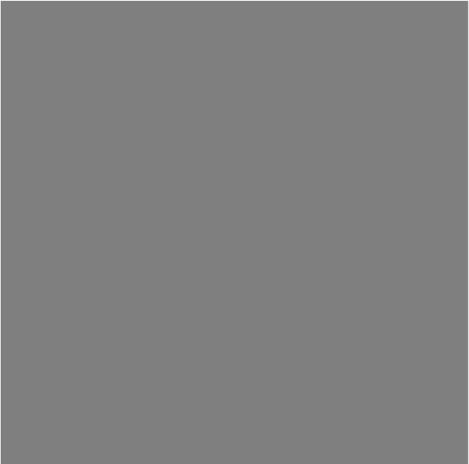
Linear interpolation (LI)



RIDL



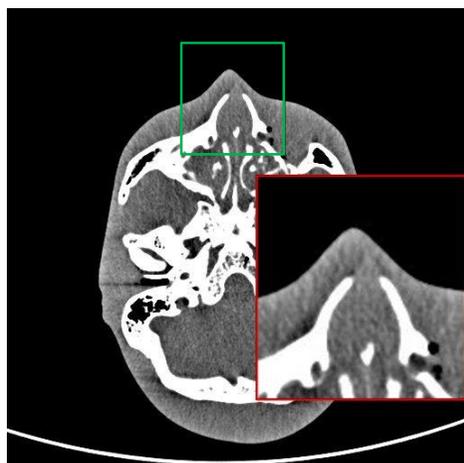
C = 60 HU
W = 360 HU



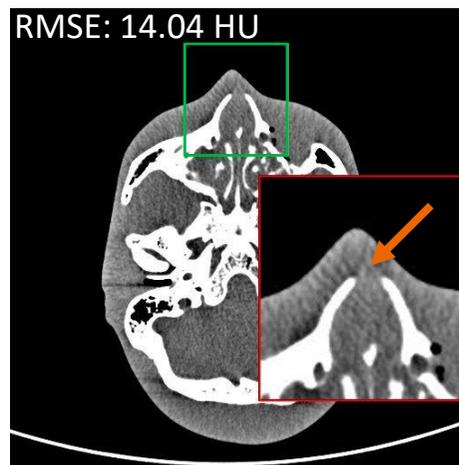
C = 0 HU
W = 150 HU

Results in Image Domain: Slice No. 74

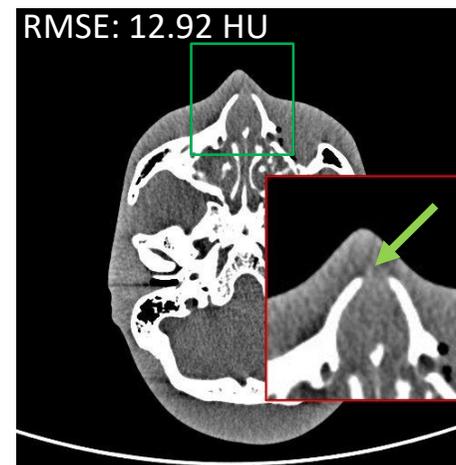
Ground truth with zFFS



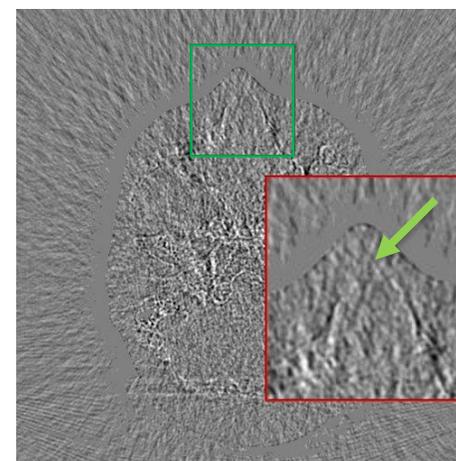
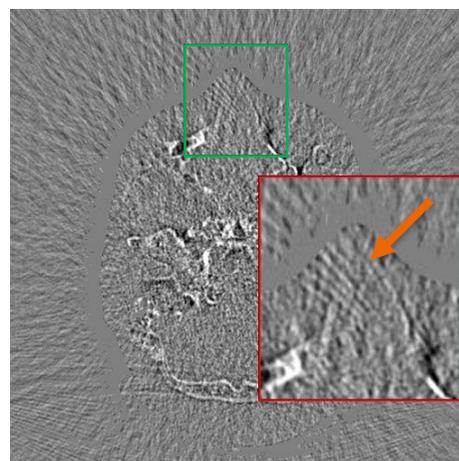
Linear interpolation (LI)



RIDL



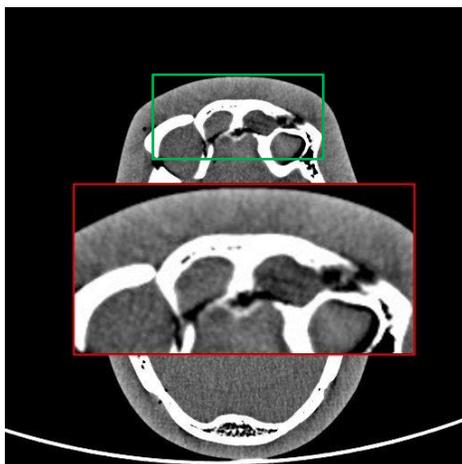
C = 60 HU
W = 360 HU



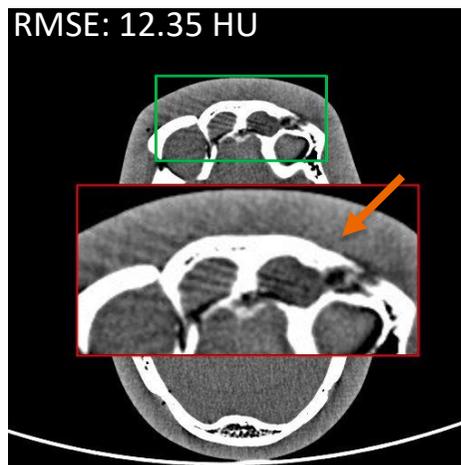
C = 0 HU
W = 150 HU

Results in Image Domain: Slice No. 125

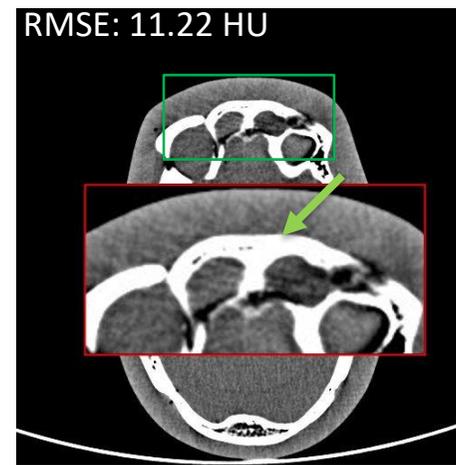
Ground truth with zFFS



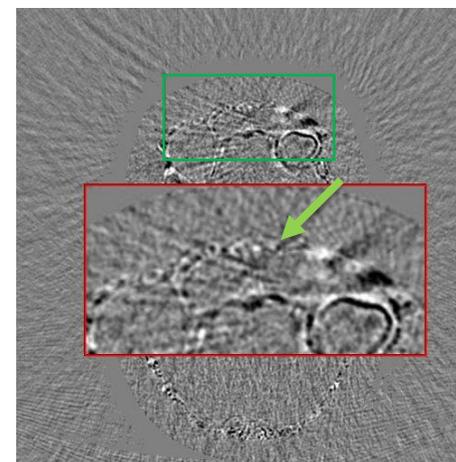
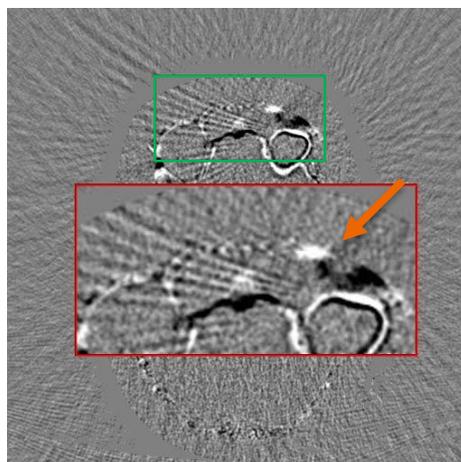
Linear interpolation (LI)



RIDL



C = 60 HU
W = 360 HU



C = 0 HU
W = 150 HU

- **Row interpolation with RIDL network can achieve better results than linear interpolation.**
- **Results can be considered a proof of concept: a neural network can meet the requirements of increasing the sampling of projection data.**
- **Positive impact on the prevention of windmill artifacts in spiral CT reconstruction.**

- **Compare RIDL network results to more advanced interpolation algorithms.**
- **Further adjustment of critical network parameters.**
- **Investigate other architectures and try to simplify the network.**
- **Improvement of training and test data.**

Thank you for your attention!

Siemens Healthineers

Computed Tomography
Siemens Healthcare GmbH
Siemensstr. 3
91301 Forchheim, Germany

Dr. Karl Stierstorfer

Eric Fournié

Jan Magonov

jan.magonov@siemens-healthineers.com

University of Lübeck

Institute of Medical Engineering
Ratzeburger Allee 160
23562 Lübeck, Germany

Prof. Dr. Thorsten M. Buzug

Dr. Maik Stille



UNIVERSITÄT ZU LÜBECK
INSTITUTE OF MEDICAL ENGINEERING

German Cancer Research Center (DKFZ)

Division of X-Ray Imaging and CT
Im Neuenheimer Feld 280
69120 Heidelberg, Germany

Prof. Dr. Marc Kachelrieß



GERMAN
CANCER RESEARCH CENTER
IN THE HELMHOLTZ ASSOCIATION