

# Simultaneous Reconstruction of Attenuation and Activity for non-TOF PET/MR Using MR Prior Information

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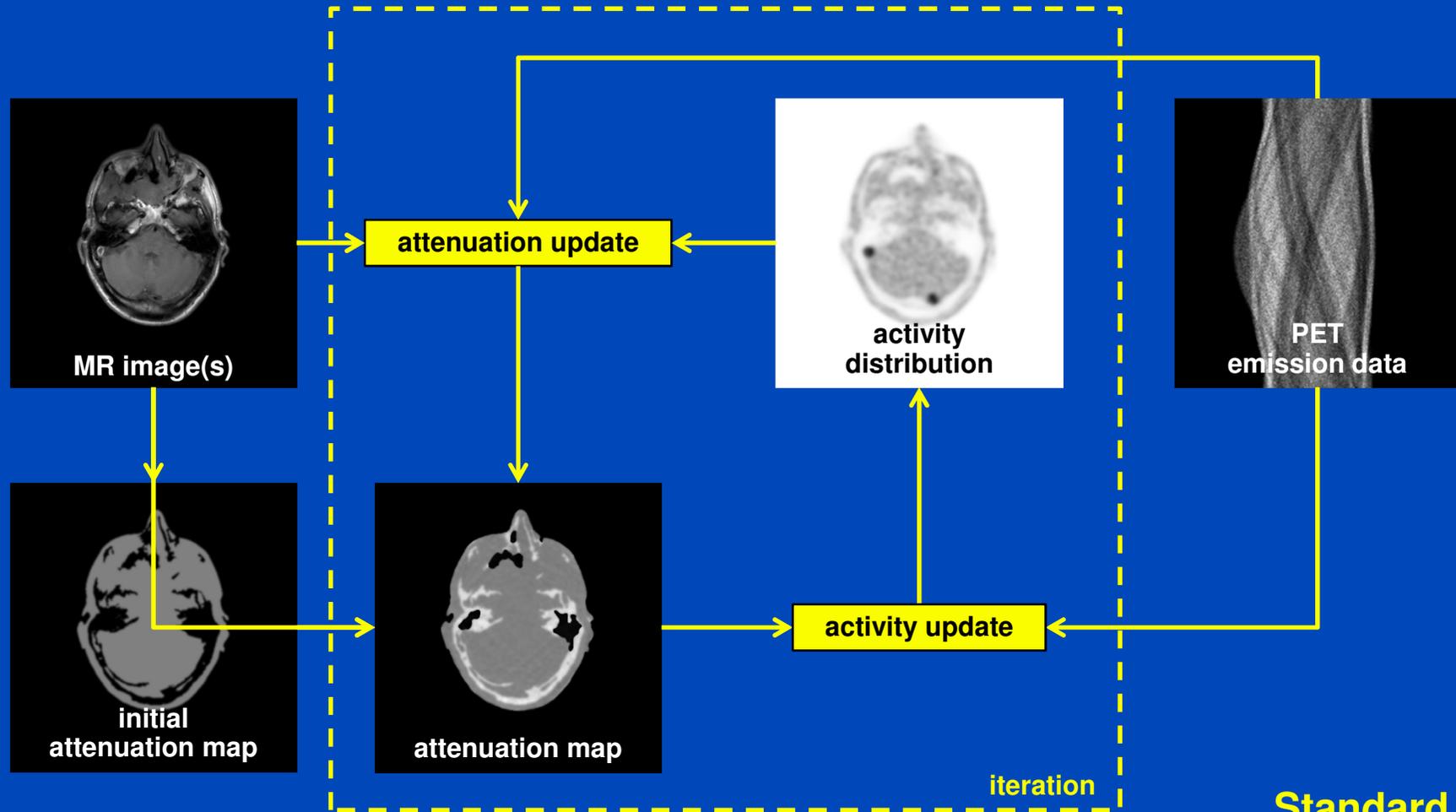


DEUTSCHES  
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IN DER HELMHOLTZ-GEMEINSCHAFT

# Introduction

- **Motivation**
  - Standard MR-based attenuation correction (AC) neglects bone attenuation and thus underestimates the activity distribution.
- **Aim**
  - Improve AC for non-TOF PET/MR by simultaneous reconstruction of attenuation and activity distributions from PET emission data using MR prior information.
- **Proposed algorithm**
  - The presented algorithm is an extension of the maximum-likelihood reconstruction of attenuation and activity (MLAA)<sup>[1]</sup> for non-TOF PET/MR, called **MR-MLAA**.

# Workflow



Standard  
MR-based AAC

# Prior Information

- Cost function

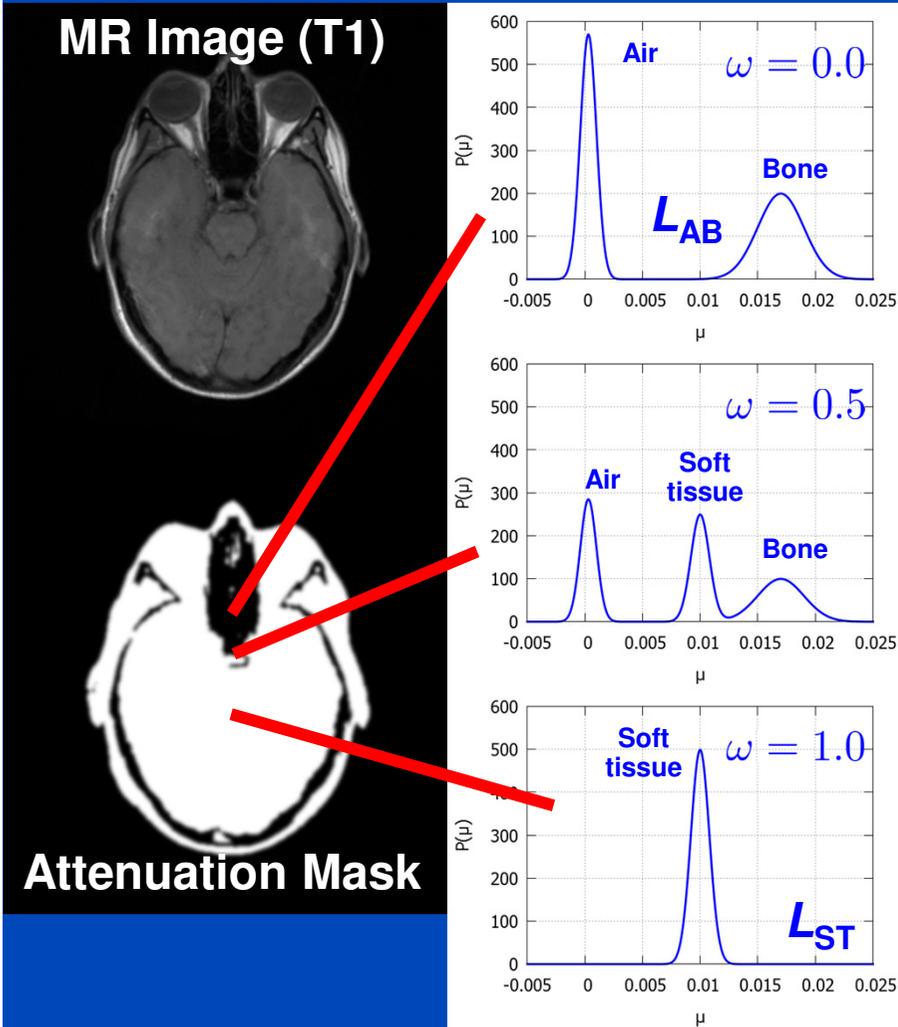
$$C(\lambda, \mu) = L(\lambda, \mu) + L_S(\mu) + L_I(\mu)$$

$\lambda$  Activity

$\mu$  Attenuation

- Log-likelihood  $L$ 
  - Probability for acquiring the measured data given  $\lambda$  and  $\mu$ .
- Smoothing prior  $L_S$ 
  - Favors smooth attenuation map.
- Intensity prior  $L_I$ 
  - **Voxel-dependent** Gaussian-like probability distribution of pre-defined attenuation coefficients, e.g., for soft tissue, air, bone, etc.

# Intensity Prior $L_I$



- Use the MR image to create a mask defining air/bone and soft tissue.
- Smooth mask.
- Define intensity prior  $L_I$  as linear combination of air/bone intensity prior  $L_{AB}$  and soft tissue intensity prior  $L_{ST}$ :

$$L_I = (1 - \omega)\beta_{AB}L_{AB} + \omega\beta_{ST}L_{ST}$$

$\omega$  Voxel-dependent weighting factor, based on attenuation mask

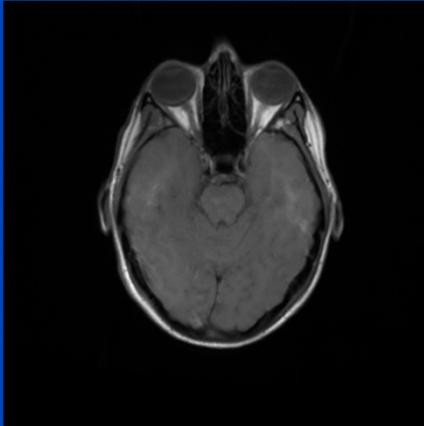
$\beta_{AB}, \beta_{ST}$  Global weighting factors

# Experiments

- Simulate 2D PET emission data accounting for
  - Poisson noise.
  - attenuation.
- Perform reconstructions using
  - the true attenuation for AC (ground truth).
  - standard MR-based AC (MRAC).
  - MR-consistent reconstruction of attenuation and activity (MR-MLAA).
- Quantitative Evaluation
  - Measure **relative mean activity** in ROIs corresponding to simulated lesions.
    - » Lesion 1:  $A_1$
    - » Lesion 2:  $A_2$

# Patient 1

MR Image

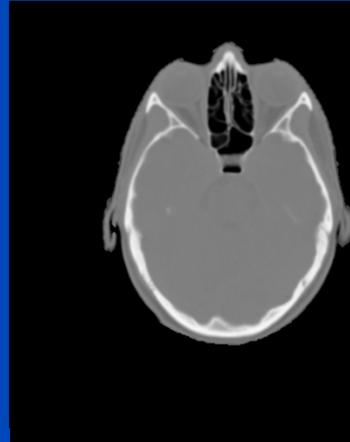


Attenuation Mask



Attenuation

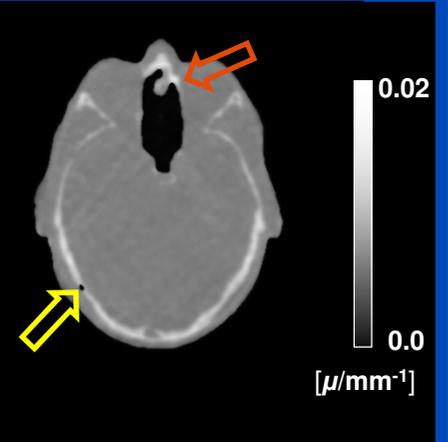
Ground Truth



MRAC

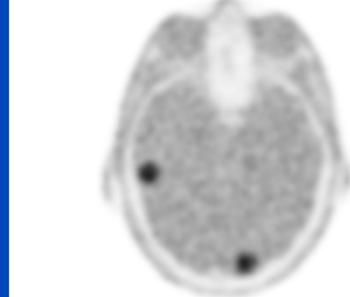


MR-MLAA



Activity

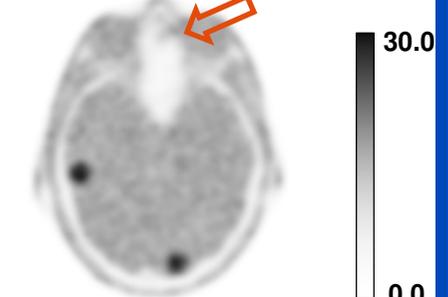
$A_1 = 1.00$



$A_1 = 0.90$



$A_1 = 1.01$



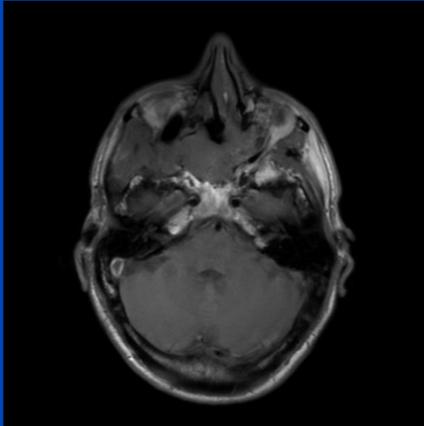
$A_2 = 1.00$

$A_2 = 0.89$

$A_2 = 0.97$

# Patient 2

MR Image

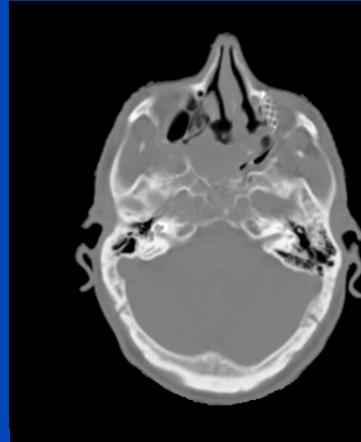


Attenuation Mask



Attenuation

Ground Truth



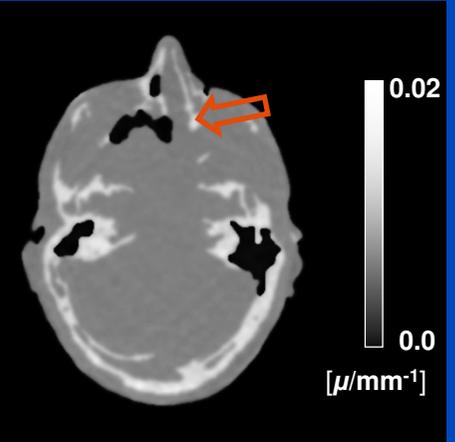
$A_1 = 1.00$

MRAC



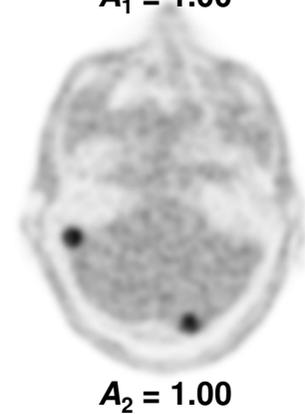
$A_1 = 0.78$

MR-MLAA



$A_1 = 0.91$

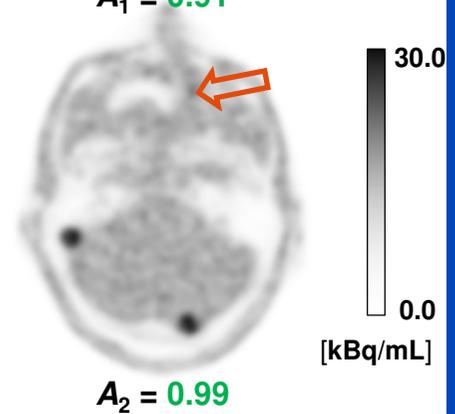
Activity



$A_2 = 1.00$



$A_2 = 0.82$



$A_2 = 0.99$

# Conclusion

- **Underestimation of activity in the lesions can be significantly reduced using MR-MLAA compared to standard MR-based AC.**
- **Some misclassifications**
  - Bone instead of soft tissue or air.
  - Air instead of bone.
- **Potential improvements**
  - Sophisticated segmentation technique to create attenuation mask from MR image(s).
  - Additional prior information, e.g., from non attenuation-corrected (NAC) images.
  - ...

# Thank You!



The 4<sup>th</sup> International Conference on  
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Conference Chair

**Marc Kachelrieß**, German Cancer Research Center (DKFZ), Heidelberg, Germany

**This presentation will soon be available at [www.dkfz.de/ct](http://www.dkfz.de/ct).**

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