

# Motion Vector Field Estimation and Motion-Compensated Reconstruction for Flat Detector Cone-Beam CT Scans of Breathing Patients

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presented by Matthias Baer<sup>1,2</sup>

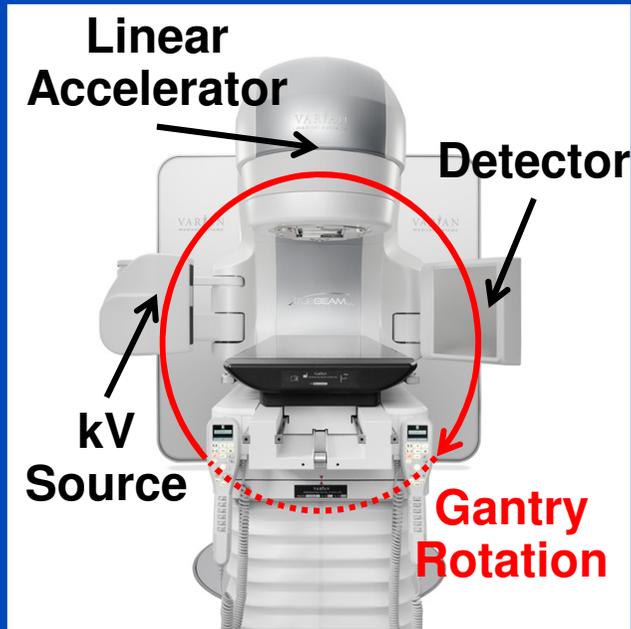
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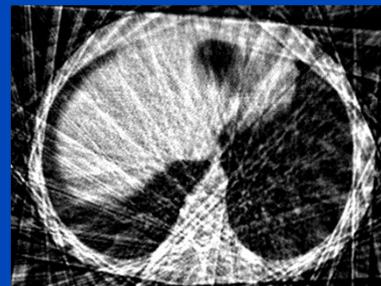
# 4D Cone-Beam CT (4DCBCT) on Slowly Rotating CBCT Devices



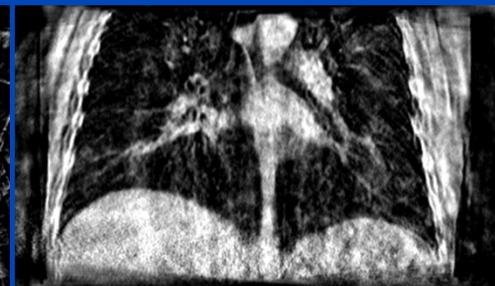
- CBCT imaging unit (kV source and flat panel detector) mounted on the gantry of a linear particle accelerator (LINAC) treatment system
- Comes with a maximum gantry rotation speed of  $6^\circ$  per second
- Much slower than clinical CT devices ( $60\text{ s}/360^\circ$  versus  $0.3\text{ s}/360^\circ$ )
- Cycle of respiratory motion usually in the magnitude of **2 – 5 seconds**, i.e. 10 – 30 respirations per scan
- Artifacts in 3DCBCT and conventional 4DCBCT



3DCBCT  $\Rightarrow$  Motion artifacts



Conventional 4DCBCT  $\Rightarrow$  Angular sampling artifacts



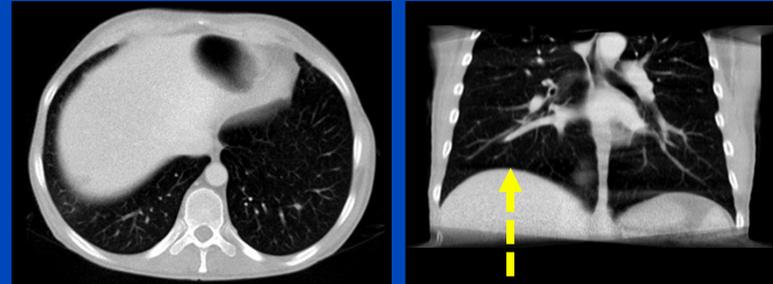
# Aim

**Provide high quality respiratory–correlated 4D volumes from on–board CBCT scans without using dedicated acquisition techniques or knowledge from prior planning scans.**

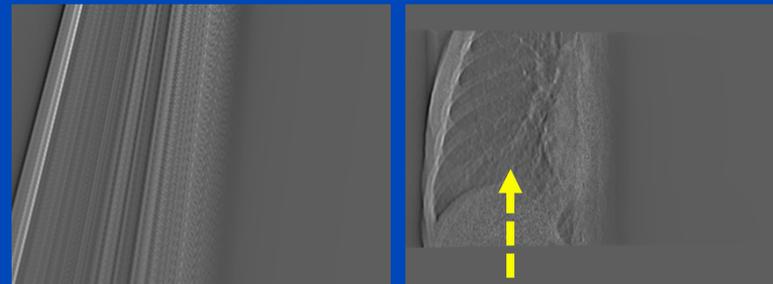
# Motion Compensation (MoCo)

- **Combine benefits**
  - High temporal resolution of conventional 4DCBCT
  - Low noise level from 3DCBCT
- **Use ALL projection data**
  - For each single 3D volume of a 4D data set
  - Compensate for motion using **motion vector fields (MVF)**
  - MVF are estimated based on conventional 4DCBCT images
- **Backproject then warp [1]**
  - Backprojection of projection data along straight lines
  - Then warp with respect to MVF

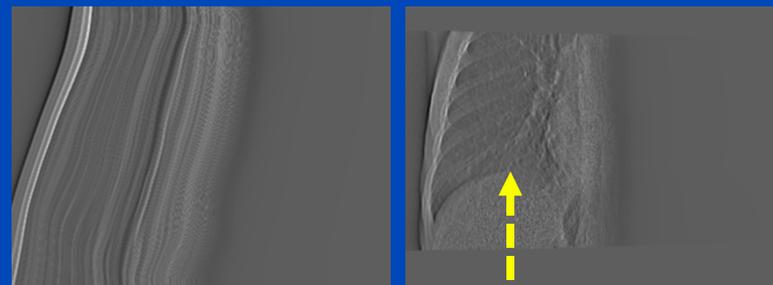
Ground truth in phase 1



Backprojection on (straight) acquisition lines of one projection acquired in phase 2



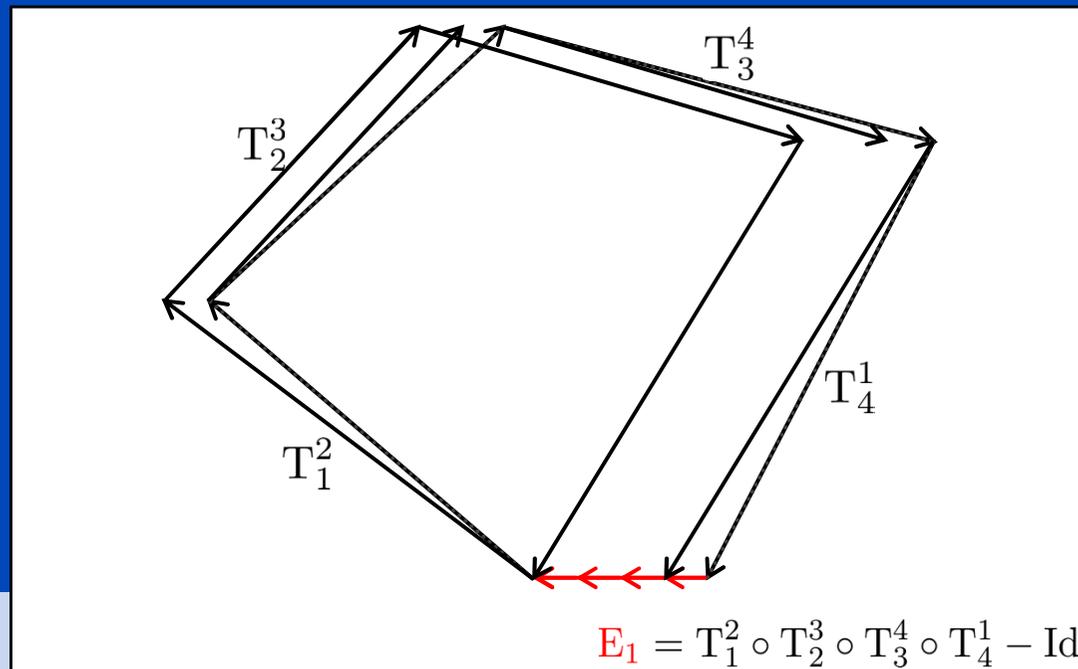
Backprojection warped to phase 1



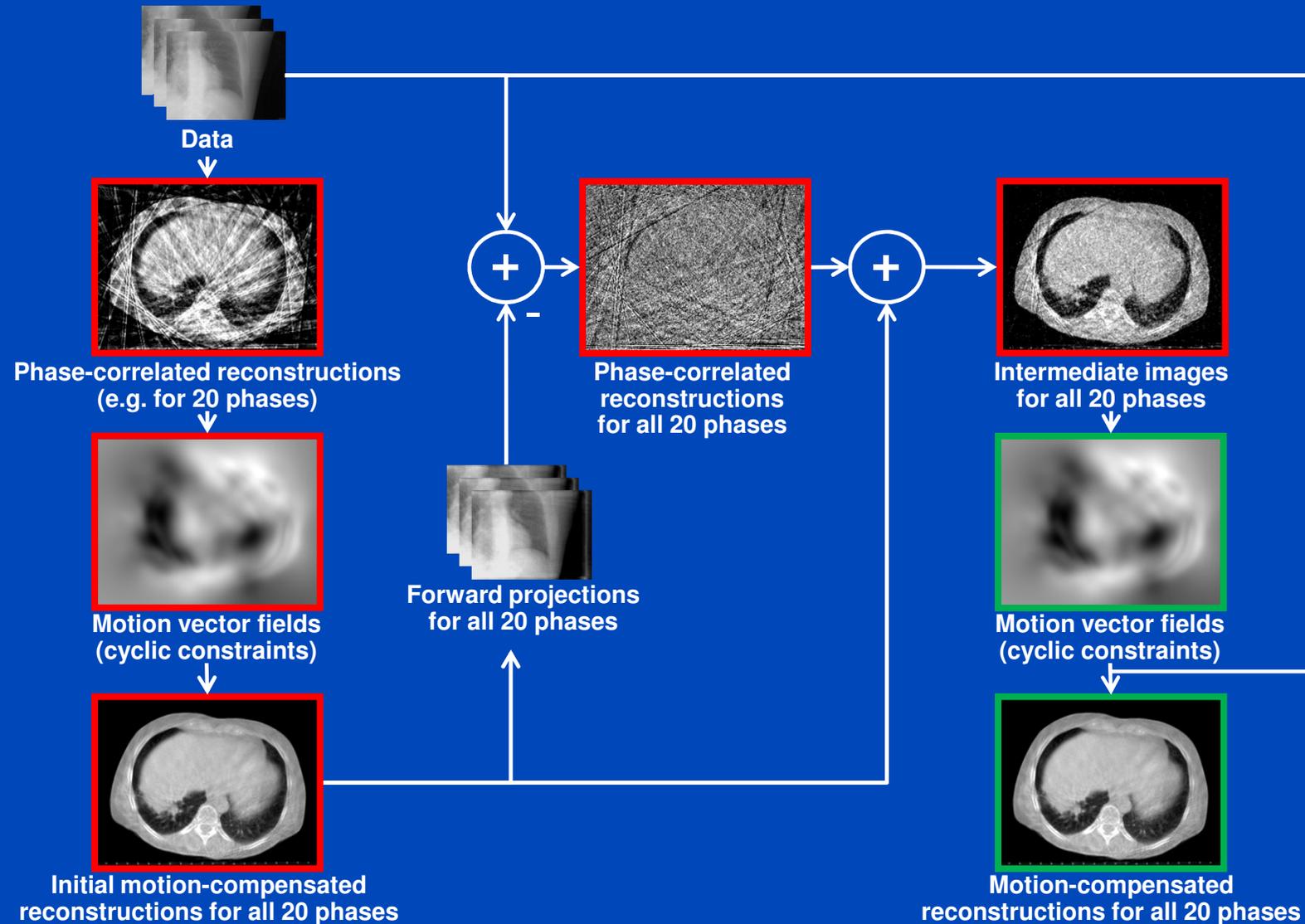
[1] Li et al., "Motion correction for improved target localization with on-board cone-beam computed tomography," Phys. Med. Biol., vol. 51, no. 2, pp. 253–267, Feb. 2006.

# A Cyclic Registration with Temporal Constraints

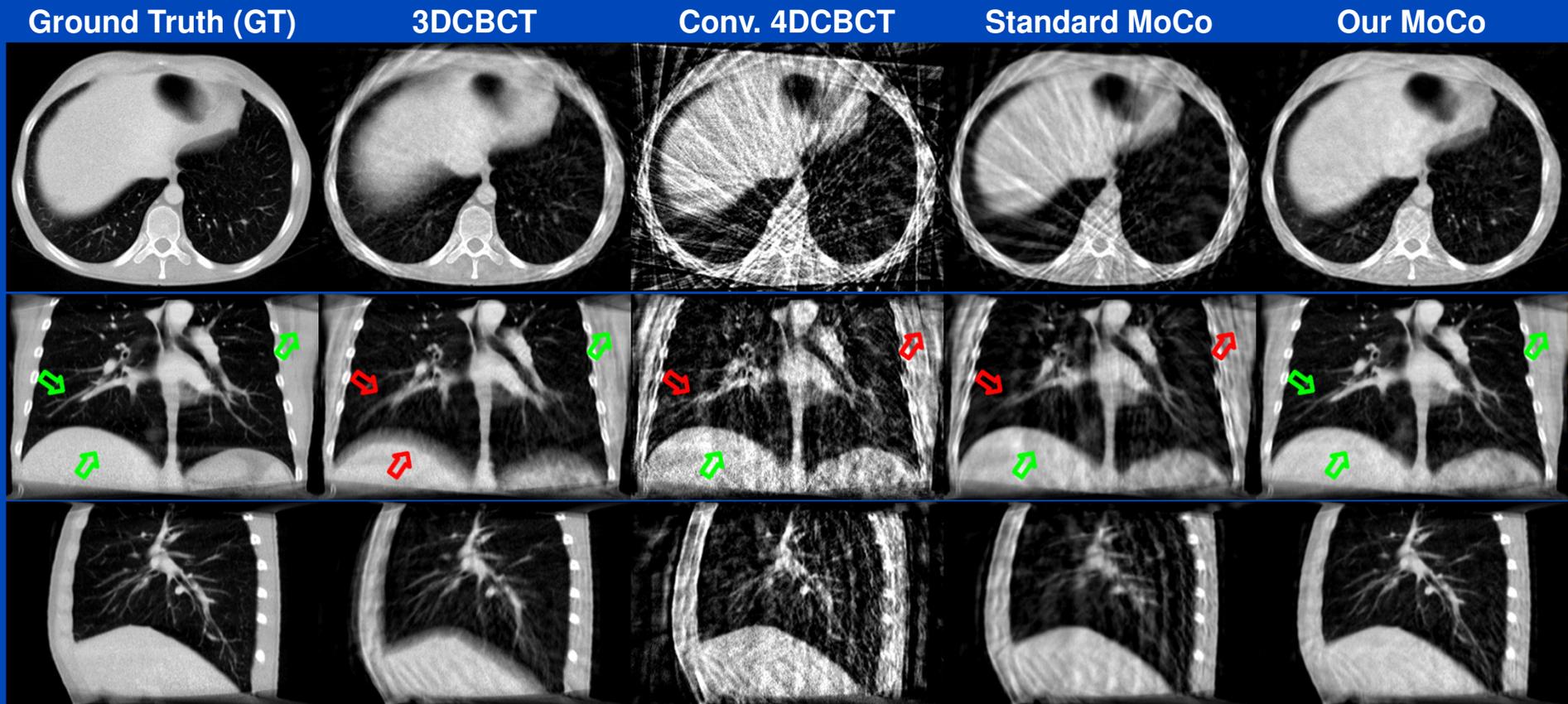
- Initial guess of MVF  $T_j^{j+1}$  between adjacent phases<sup>[1]</sup>
  - Using a spatial registration algorithm
- **Add temporal constraint**
  - Cyclic form of breathing motion patterns  $\Rightarrow$  Error estimate  $E$
  - Minimization by applying the error estimate on the estimated vector fields



# Iterative Motion Estimation



# Results for Simulated Data



- Clinical CT data of a patient thorax deformed with respect to realistic vector fields to simulate breathing

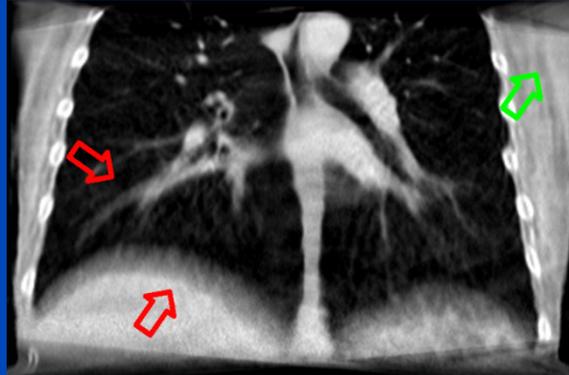
C = -200 HU, W = 1400 HU

# Results for Simulated Data

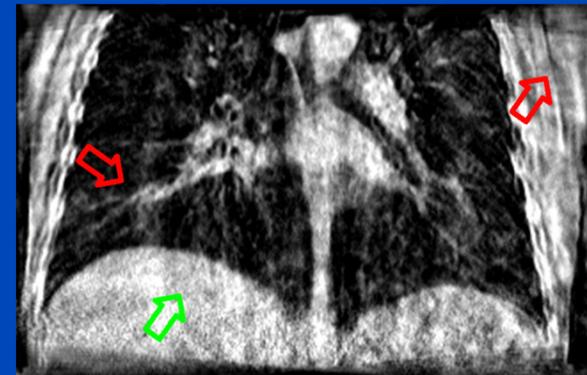
Ground Truth (GT)



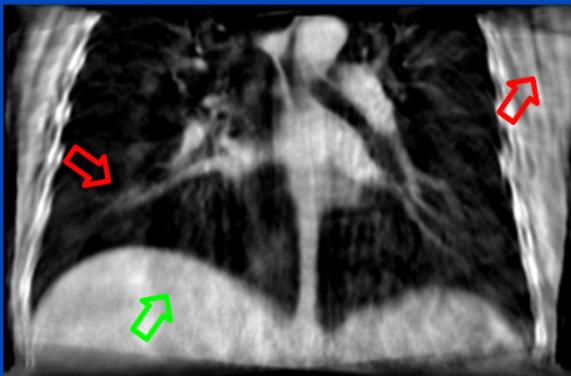
3DCBCT



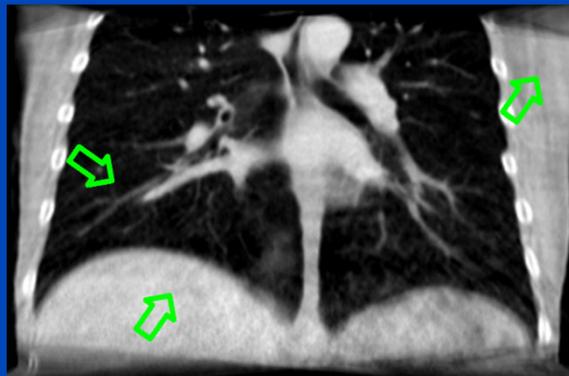
Conventional 4DCBCT



Standard MoCo



Our MoCo



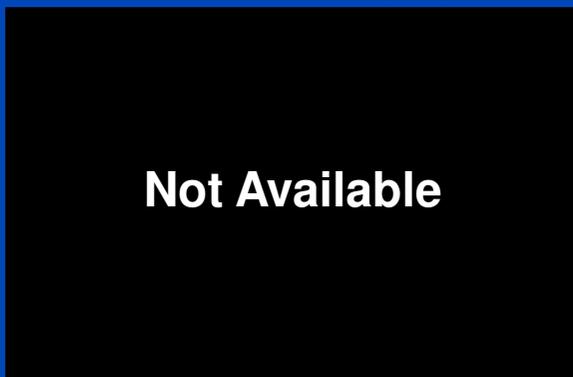
**Our MoCo:**  
Motion-compensated  
image reconstruction  
applying MVFs from our  
iterative motion estimation  
based on a cyclic registration  
with temporal constraints

- High temporal and high spatial resolution
- Low noise level and visibility of lung details

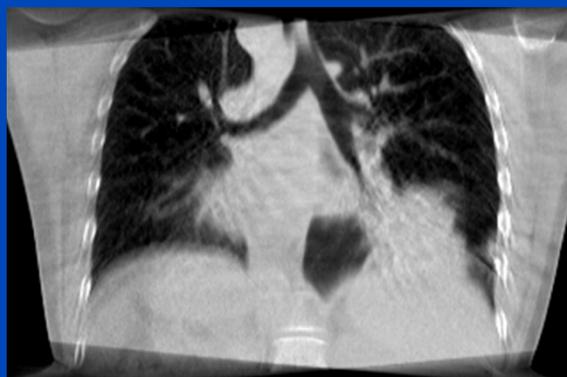
C = -200 HU, W = 1400 HU

# Results for Patient Data

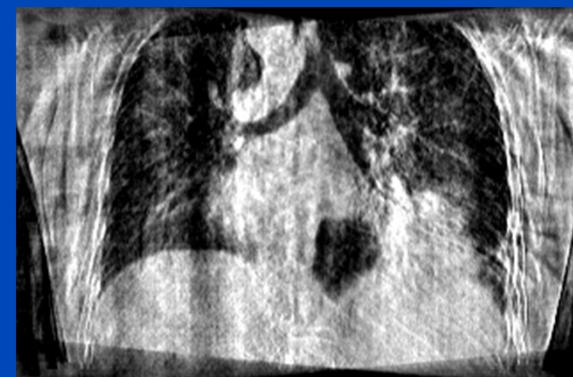
Ground Truth (GT)



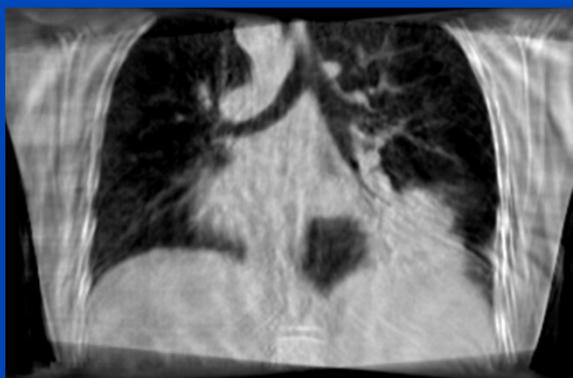
3DCBCT



Conventional 4DCBCT



Standard MoCo



Our MoCo



**Our MoCo:**  
Motion-compensated  
image reconstruction  
applying MVFs from our  
iterative motion estimation  
based on a cyclic registration  
with temporal constraints

- Similar impressions as with the simulated data

C = -200 HU, W = 1400 HU

Acquired with an On-Board Imager®  
Varian Medical Systems, Palo Alto, CA

**dkfz.**

# Summary

- **Iterative motion estimation using a cyclic registration with temporal constraints**
  - Allows for estimation of motion vector fields from conventional 4DCBCT images
  - Decreased sensitivity to angular sampling artifacts
  - No dedicated acquisition technique required
  - No knowledge required from prior scans like planning CTs
- **Motion–compensated image reconstruction applying these motion vector fields**
  - Combine benefits of 3DCBCT and 4DCBCT
    - » High spatial and high temporal resolution
    - » Low image noise
  - Visibility of lung details

# Thank You!

**This study was supported by a grant of Varian Medical Systems, Palo Alto, CA.**

**Parts of the reconstruction software were provided by RayConStruct<sup>®</sup> GmbH, Nürnberg, Germany.**

**This presentation will be soon available at [www.dkfz.de/CT](http://www.dkfz.de/CT)**